Molecular imaging of immunotherapy targets in cancer

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Abstract

Immunotherapy has emerged as a promising alternative in the arsenal against cancer by harnessing the power of the immune system to specifically target malignant tissues. As the field of immunotherapy continues to expand, researchers will require newer methods for studying the interactions between the immune system, tumor cells, and immunotherapy agents. Recently, several noninvasive imaging strategies have been employed to map the biodistribution of immune checkpoint molecules, monitor the efficacy and potential toxicities of the treatments, and identify patients who are likely to benefit from immunotherapies. In this review, we outline the current applications of noninvasive techniques for the preclinical imaging of immunotherapy targets, and suggest future pathways for molecular imaging to contribute to this developing field.

Keywords: PD-1; PD-L1; CTLA-4; immune checkpoints; immunotherapy; positron emission tomography (PET); cancer
Introduction

While the field of cancer immunotherapy has undergone tremendous growth during the past decade, the idea of using a person’s own immune system to combat disease can be traced back over a century (1,2). These approaches have immense implications for oncology applications, yet clinical translation of immunotherapy is currently limited. In the past, concerns over potential immune-related adverse effects, as well as limited benefit from traditional vaccination techniques, limited the clinical use of immunotherapies; however, the recent Food and Drug Administration approval of several immune checkpoint inhibitor immunotherapies has led to renewed interest in the field. To date, the three primary targets of checkpoint inhibition include the programmed cell death 1 receptor (PD-1) and its ligand (PD-L1), and the cytotoxic T-lymphocyte associated antigen-4 receptor (CTLA-4). As summarized in Table 1, several antibody-based checkpoint inhibitors have received FDA approval, with many others currently in various stages of clinical trials.

The innate immune system contains a number of checkpoints that ensure immune cells capable of recognizing self-antigens do not destroy healthy tissues. Thus, as tumors are self-derived tissues, they often display these same antigens and avoid immune surveillance (1). By interrupting these immune checkpoints that have been hijacked by tumors, checkpoint blockade therapy allows the immune system to recognize tumor-associated antigens and consequently destroy these malignant cells (2). Interested readers are referred to the review by Buchbinder et al. for further information on the mechanisms of these pathways (3). Blockade of these immune checkpoint pathways has shown incredible efficacy in the treatment of many cancers, including Hodgkin’s lymphoma, non-small cell lung cancer, melanoma, and others. In some instances, a correlation has been found between receptor expression and the efficacy of immune interventions (4); however, this expression seems to be dynamic and heterogeneous and as a result, fixed immunohistochemical analyses may not provide accurate information at the time of treatment (5). Molecular imaging can provide nearly real-time information about receptor expression levels, allowing physicians to predict which patients may benefit from immunotherapy and accounting for response differences between individual patients. In return, these prescreening measures will not only spare
patients ineffective therapy and potential adverse effects, but will also have implications economically as cancer therapy remains costly and time-intensive (6). In addition to patient stratification, molecular imaging of immunotherapy targets may provide insight into the status of the immune system and overall disease progression.

Since $^{18}$F-fluorodeoxyglucose (FDG) positron emission tomography (PET) monitors cellular metabolism and immunotherapy elicits a natural inflammatory response, traditional PET imaging using $^{18}$F-FDG has proven inadequate in examining responses to immunotherapy (7). Nonetheless, immunotherapy patients are still routinely examined with $^{18}$F-FDG, causing disease monitoring to be inherently subjective. To date, no clinical trials have been performed for molecular imaging of immune checkpoint targets. However, several preclinical trials have shown that noninvasive imaging techniques using PET, single photon emission computed tomography (SPECT), and optical imaging are viable platforms for determination of receptor density and hold promise for stratification of patients for future immune therapies. In addition, by tracking the fate of immune cells in vivo, researchers may be able to monitor adverse effects related to the off-target accumulation of antibodies and elucidate the mechanisms that underlie these restrictive toxicities. Molecular imaging techniques thus have nearly limitless potential to revolutionize the emerging field of immunotherapy.

**Programmed Cell Death 1 (PD-1)**

PD-1 is expressed on the surface of T-cells, B-cells, and natural killer cells and acts as a negative regulator of T-cell activity (8). PD-1 expression was also recently reported in certain subpopulations of melanoma cells (9). PD-1 may interact with one of its two endogenous ligands, known as PD-L1 or PD-L2, which are found on the surface of antigen-presenting cells or tumor cells. Upon PD-1 interaction, a kinase signaling pathway that normally results in T-cell activation is inhibited; thus, immunotherapy strategies that interfere with the PD-1 checkpoint have shown enhanced anticancer activity in the clinic. There are currently two FDA-approved antibodies targeting PD-1: pembrolizumab (Keytruda®, Merck & Company, Inc.) and nivolumab (Opdivo®, Bristol-Myers Squibb) (10). While these two antibodies have
the same biological target, their binding affinities and production source are different. The binding affinity of pembrolizumab (<100 pM) for PD-1 is nearly 10-fold higher than that of nivolumab (3 nM). The source of production also differs, as pembrolizumab is a humanized murine antibody while nivolumab is a fully human antibody. Despite these differences, the objective response rates in advanced melanoma were similar between pembrolizumab (26-38%) and nivolumab (31-40%) (10), suggesting that the therapeutic dosages may be saturating the receptor in therapy. PD-1 targeted treatments have shown fewer adverse effects than those employing the CTLA-4 pathway; however, significant immune-mediated responses were still reported during clinical trials (11,12).

Imaging techniques targeting PD-1 are unique because, in most cases, they do not allow visualization of the primary tumor; rather, PD-1-targeted probes allow for imaging of PD-1 expressed on immune cells. For example, Natarajan et al. developed a PET tracer to image PD-1-expressing tumor-infiltrating lymphocytes (TILs) (13). The murine anti-PD-1 monoclonal antibody was prepared with 1,4,7,10-tetraazacyclododecane-1,4,7,10-tetraacetic acid (DOTA) for radiolabeling with 64Cu (half-life (t1/2): 12.7 h). The biodistribution of the tracer was mapped in a transgenic mouse model of melanoma. The tracer effectively accumulated in the tumor with 7.4 ± 0.71 percent injected dose per gram (%ID/g) at 48 h post-injection (p.i.), resulting in a tumor-to-muscle ratio of approximately 11 (Fig. 1A). Blocking studies using excess antibody decreased tumor uptake to 4.51 ± 0.26 %ID/g at 48 h p.i. (Fig. 1A), which further validated the tracer’s high specificity for PD-1. Additionally, bioluminescent imaging of luciferase-transfected TILs confirmed that the tumor uptake was due to lymphocyte infiltration of the tumor (Fig. 1B), showing that PET may be used for the noninvasive imaging and determination of PD-1 expression in vivo.

In another study, Hettich et al. developed novel radiotracers for PET imaging of both PD-1 and PD-L1 (14). Melanoma tumor-bearing mice were locally irradiated to induce TIL infiltration into the tumor, most of which are CD8+ effector cytotoxic lymphocytes uniformly expressing PD-1. The researchers employed a 64Cu-labeled anti-PD-1 tracer for PET imaging, and found that the tracer had increased uptake in the tumor, consistent with higher CD8+ TIL levels. Uptake could also be reduced by blocking
the antigen (Fig. 1C). Furthermore, the authors employed a PD-L1 imaging tracer that will be discussed in the PD-L1 section.

The clinically-approved antibody pembrolizumab was also recently evaluated in a number of murine models, including mice engrafted with human peripheral blood mononuclear cells (15). The $^{89}$Zr-labeled tracer was found to co-localize with human T-cells, allowing direct visualization of their distribution in vivo.

Programmed Death Ligand 1 (PD-L1)

In contrast to PD-1, PD-L1 is naturally expressed on a number of tissues, including some tumor cells, vascular endothelium, hepatocytes, mesenchymal stem cells, T and B cells, macrophages, and mast cells (16). Immune-privileged tissues such as the eye and placenta also display high levels of PD-L1. The blockade of PD-L1 leads to enhanced T-cell activity and inhibition of immune-mediated tumor evasion (16,17). As PD-L1 is often expressed on the actual tumor cells, models for imaging this target have proven to be more attainable than those for targets that are only expressed on immune cells. PD-L1 expression is often heterogeneous even within a given cancer subtype, and immunohistochemistry techniques are susceptible to errors as a result (5). Of note, treatment with pembrolizumab requires >1% of NSCLC cells to be PD-L1 positive, so a PD-L1 tracer may also find application in the planning of these treatments. Consequently, several anti-PD-L1 imaging agents have been developed to quantify PD-L1 expression in preclinical settings.

Maute et al. engineered a high-affinity PD-1 non-antibody variant for both immunoPET imaging and immunotherapy in a colon cancer model (18). Rather than an agent that behaves like PD-L1 and binds to PD-1, the group utilized directed evolution by yeast-surface display to create a high affinity (110 pM) competitive antagonist of human PD-L1. Genetically engineered CT26 colon cancer models that were either PD-L1 negative or PD-L1 positive were employed for tumor treatment studies, where the PD-L1 antagonist was shown to decrease tumor growth out to two weeks. Additionally, conjugation of the antagonist with $^{64}$Cu-DOTA allowed for PET visualization of distribution in both xenografts, with a nearly
two-fold increase in signal for the positive tumors over negative as seen in Fig. 2A. Thus, this agent shows significant promise in theranostics for PD-L1-expressing cancers.

Using the mouse and human cross-reactive antibody MPDL3280A, Chatterjee et al. developed a multimodality SPECT and near-infrared imaging agent for visualizing PD-L1-expressing tumors (19). Previously, MPDL3280A was proven effective in clinical trials for non-small cell lung cancer, bladder cancer, melanoma, renal cell carcinoma, and others (20), prompting researchers to utilize this antibody for imaging of PD-L1 expression. Specifically, Chinese hamster ovary tumor xenografts with and without constitutive stable PD-L1 expression were studied using the $^{111}$In-labeled antibody ($t_{1/2}$: 2.8 days), as well as the dye-labeled version. Both studies indicated that relative PD-L1 expression could be determined (Fig. 2B). Also, predosing with cold antibody was found to improve tumor uptake through saturation of receptors on splenocytes and increased blood circulation time. Triple-negative breast cancer xenografts, where PD-L1 expression was not genetically engineered, were also evaluated in this study, with higher reported values of PD-L1 expression corresponding to higher %ID/g values. These studies indicate that clinically employed antibodies may be modified with imaging agents to determine their biodistribution prior to the administration of therapeutic levels, and patients could ultimately be selected for particular therapies based upon these results.

Similarly, Heskamp et al. radiolabeled an anti-PD-L1 antibody with Indium-111 for SPECT imaging. The biodistribution of the tracer was mapped in mice bearing subcutaneously-implanted breast cancer cells with varying PD-L1 expression levels (21). MDA-MB-231 was found to express PD-L1 in over 90% of cells, while MCF-7 exhibited only minimal expression (0.1%). Tracer uptake values were found to correlate with PD-L1 expression levels; thus, this tracer was able to distinguish PD-L1 expression levels within cell lines of the same cancer type.

As previously discussed, Hettich et al. designed two new PET tracers for targeting PD-1 and PD-L1 (14). Mice were subcutaneously implanted with PD-L1 positive and PD-L1 knockout cells on opposing
flanks. Both *in vivo* imaging and *ex vivo* analysis confirmed that uptake of the anti-PD-L1 tracer was specific for PD-L1-expressing melanoma tissue, while the PD-L1 knockout tumors showed minimal uptake of the tracer (Fig. 2C). Interestingly, the authors noted increased uptake of the PD-L1 tracer in brown adipose tissue, suggesting that this tissue may be immunologically relevant.

In another study, Josefsson *et al.* developed an $^{111}$In-labeled murine anti-PD-L1 antibody for SPECT biodistribution studies and potential radioimmunotherapy application (22). Imaging in mice bearing NT2.5 murine mammary xenografts revealed high uptake in the tumor, as well as the spleen, liver, and thymus. However, spleen uptake was greatly reduced upon predosing with cold antibody, from nearly 60 %ID/g with pure tracer to 11 %ID/g with the administration of 100-fold excess antibody. While this predosing strategy allowed for researchers to clearly visualize the tumors, this also resulted in the administration of high doses of antibody prior to imaging, a non-ideal situation clinically. However, the authors note that radioimmunotherapy may be performed in conjunction with the traditional antibody-based therapy, and it is in this situation that predosing becomes valuable. Theoretical dosimetry calculations using uptake data from pure tracer injections indicate therapeutic absorbed doses to the tumor using both $^{90}$Y ($t_{1/2}$: 64.1 h) and $^{177}$Lu ($t_{1/2}$: 6.65 days), but also high spleen doses that may be toxic. Further evaluation of the proposed radioimmunotherapy with this anti-PD-L1 agent is therefore warranted.

**Cytotoxic T-lymphocyte associated antigen 4 (CTLA-4)**

CTLA-4 is a transmembrane inhibitory receptor expressed on activated T lymphocytes, including activated T-cells, memory T-cells, and Treg-cells (23). In addition, it was recently discovered that CTLA-4 may be expressed by many tumor types (24). The interaction between CD80/CD86 and CTLA-4 expressed on antigen-presenting cells offsets CD28-mediated costimulatory signals, which effectively downregulates T-cell activation through several mechanisms including raising of the T-cell activation threshold and attenuation of clonal expansion (23). CTLA-4 blockade with antibodies effectively limits this interaction, resulting in enhanced T-cell proliferation and the generation of effector T-cells; thus, CTLA-4-targeted antibodies have shown efficacy in the treatment of many cancers. While targeting of CTLA-4
provides therapeutic benefits, anti-CTLA-4 therapies can lead to severe adverse effects. Clinical trials have been performed with two anti-CTLA-4 agents, ipilimumab (Yervoy®, Bristol-Myers Squibb) (25) and tremelimumab (AstraZeneca) (26), in which tumor response rates for the drugs as monotherapy were approximately 10%. These therapies have been shown to be extremely effective in this subpopulation of patients; thus, molecular imaging may assist in prescreening patients to identify individuals more likely to respond to anti-CTLA-4 immunotherapy.

Recently, PET imaging was employed to determine levels of CTLA-4-positive TILs in CT26 colon cancer-bearing mice (27). Here, Higashikawa et al. developed a $^{64}$Cu-labeled anti-mouse CTLA-4 antibody to study subcutaneously-implanted xenografts in mice (27). The antibody was constructed to recognize the extracellular domain of CTLA-4, similar to the behavior of the FDA-approved antibody ipilimumab. Through this study, the authors verified that CTLA-4 expression on TILs, not the tumor cells themselves, was the cause of tracer uptake as minimal levels of CTLA-4 were detected in cell culture or tumors implanted into immunodeficient mice (Fig. 3A). Only when mice were immunocompetent were high CTLA-4 expression levels observed in Western analysis of ex vivo tumors. PET imaging evaluation of the antibody indicated slightly higher uptake of the anti-CTLA-4 antibody with respect to a control IgG in immunocompetent models (7.5 %ID/g vs. 5.8 %ID/g at 48 h p.i.), as seen in Fig. 3B. While the anti-CTLA-4 antibody provided enhanced uptake in comparison to the nonspecific antibody, the agent has yet to be evaluated in models where varying levels of CTLA-4 expression are present. However, this first study successfully demonstrated the use of a $^{64}$Cu-labeled anti-CTLA-4 antibody to noninvasively image CTLA-4 levels on TILs in cancer models.

**Challenges and Future Directions**

Visualizing the complex interactions between the immune system and tumor cells can provide vital insight into biomarkers that may be excellent candidates for future immunotherapies. Immunotherapy blockade strategies are becoming more common in the management of several types of cancer; thus, the field is expected to grow exponentially during the next decade. As immune checkpoint inhibitors rely upon
adequate receptor expression levels, noninvasive imaging to detect PD-1/PD-L1 or CTLA-4 may allow for enhanced patient identification, stratification, and the early assessment of therapeutic response. As many novel immune checkpoints for therapeutic targeting are investigated (1), imaging strategies for prescreening patients will be crucial to the success of these treatments. Additional methods not based on antibody platforms are also being explored, including the in vivo tracking of radiolabeled T-cells (28).

Immunotherapy treatments may also benefit from molecular imaging of targets not directly involved in the checkpoint blockade itself. For instance, CD3 imaging agents may be able to probe the T-cell infiltration occurring during immunotherapy, such as the anti-CTLA-4 therapy studied by Larimer et al. (29). Similarly, Tavare et al. imaged CD8+ TILs during immune responses to therapy (30,31). These investigations may provide a more universal approach to monitoring of immunotherapies, as they are not restricted to single immune checkpoint targets.

As the studies to date in this area have been preclinical, a few steps will be critical for clinical translation. Most of the agents outlined herein are murine antibodies and may not display specificity for human receptors; thus, human or humanized antibodies will need to be created for clinical translation. In addition, humanized or transgenic models used in preclinical research fall short of mimicking the conditions found in human patients. Imaging of these immune checkpoint pathways may also be limited by external conditions, including therapeutic intervention and certain bacterial or viral infections that may modify the immune system (32). As such, it has yet to be seen whether or not these imaging biomarkers will quantitatively represent the receptor densities.

Many preclinical studies utilize a pre-dosing strategy with non-labeled antibody to increase the tracer uptake in targeted tissues of interest (33). While this certainly provides greater visual contrast between background and malignant tissues, this need for saturating receptor binding points to one of the critical pitfalls of immunotherapy. While most biomarkers targeted for imaging are found solely on tumor cells, these immune checkpoint pathway receptors are heterogeneously expressed throughout the entire
body, complicating potential imaging strategies. Thus, molecular imaging of immunotherapy targets requires creative approaches that may extend beyond traditional tracer development, as does the generation of adequate preclinical animal models.

A number of researchers have proposed that immunotherapy and external radiotherapy may act in synergy to increase the therapeutic indices of these treatments (34,35). Thus, agents which perform well in imaging settings may also be modified in the future with therapeutic nuclides, such as $^{90}$Y or $^{177}$Lu, for combined immunotherapy and targeted radiotherapy, further extending the reach of nuclear medicine into this emerging field.

Conclusion

Cancer immunotherapy blockade interventions have the potential to revolutionize cancer management strategies, and are already doing so today. The causes of considerable immune-related adverse effects and limited success rates may be elucidated through the use of noninvasive, neoadjuvant imaging. Molecular imaging of immunotherapy targets such as PD-1, PD-L1, and CTLA-4 has shown promise in preclinical studies, and successful application to the clinic will provide great strides in the fight against cancer. In the future, molecular imaging of immunotherapy targets may enhance patient stratification and provide insight for development of novel immunotherapy targets.

Disclosure

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References


FIGURE 1. Molecular imaging of PD-1-expressing tumor infiltrating lymphocytes (TILs). (A) Subcutaneous melanoma xenografts could be visualized upon injection of a $^{64}$Cu-labeled anti-PD-1 antibody. The specificity of the tracer was confirmed through a blocking study. Adapted from (13). (B) Bioluminescence imaging of luciferase-transfected PD-1-expressing T$_{reg}$-cells validated the binding and tumor infiltration of T lymphocytes. Adapted from (13). (C) PET imaging of melanoma tumor-bearing mice 24 h after injection with a $^{64}$Cu-NOTA-PD-1 antibody. For the blocking study, mice were injected with cold antibody 24 h before tracer injection. Sp: spleen; Tu: tumor. Adapted from (14).
FIGURE 2. Noninvasive imaging of PD-L1 in vivo. (A) A $^{64}\text{Cu}$-labeled PD-L1 antagonist allows for distinction between tumors with high and low expression levels of PD-L1 at 1 h post-injection. Adapted from (18). (B) Near-infrared images acquired in the 800 nm channel show significant differences in uptake of PD-L1-antibody between PD-L1 positive and negative tumors. Adapted from (19). (C) PET imaging of mice subcutaneously implanted with PD-L1 positive (WT) or PD-L1 knockout (KO) tumor cells was performed 24 h after mice were injected with $^{64}\text{Cu}$-NOTA-PD-L1 antibody. Sp: spleen; Tu WT: wild-type tumor; Tu KO: PD-L1 KO tumor; cLN: cervical lymph node; aLN: axillary lymph node; BAT: brown adipose tissue. Adapted from (14).
FIGURE 3. PET imaging of colon cancer with a $^{64}$Cu-labeled anti-CTLA-4 antibody. (A) CTLA-4 expression was low in normal colon tissue and completely absent in CT26 tumors implanted in immunodeficient mice. However, CTLA-4 expression was high in tumors implanted into immunocompetent mice. (B) At 48 h p.i., the $^{64}$Cu-labeled antibody showed higher uptake in CT26 tumors in comparison to the nonspecific antibody control ($^{64}$Cu-DOTA-IgG). Adapted from (27).
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TABLE 1. Several immune checkpoint inhibitors have been FDA-approved for the treatment of cancer, with many others in clinical trials.