

Caffeine Occupancy of Human Cerebral A₁ Adenosine Receptors: In Vivo Quantification with ¹⁸F-CPFPX and PET

David Elmenhorst*¹, Philipp T. Meyer*^{1,2}, Andreas Matusch¹, Oliver H. Winz¹, and Andreas Bauer^{1,3}

¹Institute of Neuroscience and Medicine (INM-2), Forschungszentrum Jülich, Jülich, Germany; ²Department of Nuclear Medicine, University Hospital Freiburg, Freiburg, Germany; and ³Department of Neurology, Medical Faculty, Heinrich-Heine-University Düsseldorf, Düsseldorf, Germany

Caffeine is the neuroactive agent in coffee and tea and is a broadly consumed stimulant. It is a nonselective antagonist of the neuro-modulator adenosine and, if applied in commonly consumed doses, evokes its stimulating effects through the blockade of adenosine receptors. ¹⁸F-8-cyclopentyl-3-(3-fluoropropyl)-1-propylxanthine (¹⁸F-CPFPX) has been established as a highly selective and affine PET ligand for the A₁ adenosine receptor (A₁AR). The objective of the present study was to visualize and quantify the in vivo occupancy of the human cerebral A₁AR by caffeine using ¹⁸F-CPFPX and PET. **Methods:** Fifteen subjects (age range, 24–68 y) underwent a 140-min bolus–plus–constant-infusion PET experiment after at least 36 h of caffeine abstinence. Metabolite-corrected blood data were used to calculate steady-state distribution volumes (V_T) during the baseline condition of the scan between 70 and 90 min. Subsequently, subjects received a 10-min infusion of varying concentrations (0.5–4.3 mg/kg of body weight) of caffeine at 90 min. Occupancy V_T of the A₁AR was thereafter estimated using data acquired between 120 and 140 min. Occupancy levels were calculated using the Lassen plot, from which the inhibitory concentrations of 50% were derived. Plasma levels of caffeine were determined at regular intervals. One subject received an intravenous vehicle as a placebo. **Results:** Caffeine displaced 5%–44% of ¹⁸F-CPFPX binding in a concentration-dependent manner. There was no change of radioligand binding after the administration of placebo. Half-maximal displacement was achieved at a plasma caffeine concentration of 67 μM, which corresponds to 450 mg in a 70-kg subject or approximately 4.5 cups of coffee. **Conclusion:** Given a biologic half-life of about 5 h, caffeine might therefore occupy up to 50% of the cerebral A₁AR when caffeinated beverages are repeatedly consumed during a day. Furthermore, the present study provides evidence that ¹⁸F-CPFPX PET is suitable for studying the cerebral actions of caffeine, the most popular neurostimulant worldwide.

Key Words: caffeine; adenosine A₁ receptor; CPFPX; positron emission tomography; human; brain

J Nucl Med 2012; 53:1–7

DOI: 10.2967/jnumed.112.105114

Caffeine is the most commonly consumed psychoactive substance worldwide and an active ingredient in innumerable beverages and foods. Its neurobiologic effects comprise mainly stimulatory actions on alertness, attention (1), cognitive performance (2,3), and cerebral perfusion (4). It is known to reduce sleepiness, to prolong sleep latency, and to enhance wake periods after sleep onset (5,6).

The consumption of approximately 3 cups of coffee corresponds to an oral uptake of 5–8 mg of caffeine per kilogram of bodyweight (7), leading to plasma peak levels of 8–10 mg/L (8,9). The plasma-to-cerebrospinal fluid (CSF) ratio was reported to be 1 for caffeine (10) at equilibrium conditions. CSF concentrations of caffeine will therefore amount to approximately 50 μM (molar weight of caffeine, 194.19 g/mol) after intake of the aforementioned dose of caffeine, which is frequently consumed on a daily basis.

The biologic actions of caffeine are generally assigned to its antagonizing effects at cerebral adenosine receptors. There are 4 different subtypes of adenosine receptors, of which the A₁ adenosine receptor (A₁AR) has the most abundant distribution and highest concentration in the human brain.

Genetic constitutional knockout animals for the different adenosine receptors suggest that the psychostimulant and arousal effects are mainly mediated by the A_{2A} adenosine receptor (11–13). However, these data cannot readily be extrapolated to the human condition because there are substantial interspecies differences with regard to the cerebral distribution and concentration of adenosine receptor subtypes. In the human brain, the A₁AR is the most abundant adenosine receptor. It is highly concentrated in human neocortical areas and shows an area- and layer-specific distribution pattern (14) that is strikingly different from its distribution in rodents (15).

The compound 8-cyclopentyl-3-(3-fluoropropyl)-1-propylxanthine (CPFPX) (14,16) shows a high affinity for the A₁AR (dissociation constant, 1.26 nM in cloned human receptors) and a high selectivity (A_{2A} adenosine receptor affinity, 940 nM). It has been applied in autoradiographic in

Received Feb. 27, 2012; revision accepted May 31, 2012.
For correspondence or reprints contact: David Elmenhorst, Institute of Neuroscience and Medicine (INM-2), Forschungszentrum Jülich, 52425 Jülich, Germany.
E-mail: d.elmenhorst@fz-juelich.de
*Contributed equally to this work.
Published online ■■■■.
COPYRIGHT © 2012 by the Society of Nuclear Medicine and Molecular Imaging, Inc.

vitro binding experiments in its tritiated form (^3H -CPFPX) and in PET experiments as a radiofluorinated compound (^{18}F -CPFPX) to determine $A_1\text{AR}$ densities in human, non-human primate, and rodent brain tissue. Another PET ligand that has been successfully implemented and has been extensively characterized in humans is the xanthine derivative ^{11}C -MPDX (17). Because ^{18}F has a longer half-life than ^{11}C , ^{18}F -CPFPX is especially suited for bolus-plus-constant-infusion studies with long scan durations.

Various pharmacokinetic modeling approaches have been validated (14,18), and the feasibility of in vivo displacement of ^{18}F -CPFPX has been shown by an occupancy study with unlabeled CPFPX (19). The proposed models for quantification have a high test-retest reliability and stability (20).

In a recent in vitro study, we measured the concentration of caffeine that displaces 50% of the binding (inhibitory concentration of 50%, or IC_{50}) of ^3H -CPFPX to $A_1\text{AR}$ s in human postmortem brain tissue (21). The respective IC_{50} values were in the range of 113–170 μM , implying that the aforementioned commonly consumed doses of caffeine led to an $A_1\text{AR}$ occupancy that was accessible in vivo using ^{18}F -CPFPX and PET. A preliminary PET study with rats served as a proof of principle (22).

The objective of the present study was, therefore, to quantify the in vivo occupancy of $A_1\text{AR}$ by caffeine in the human brain with a bolus-plus-constant-infusion paradigm using ^{18}F -CPFPX and PET.

MATERIALS AND METHODS

Subjects

All procedures were approved by the Ethics Committee of the Medical Faculty of the University of Duesseldorf, Germany, and the German Federal Office for Radiation Protection. Male volunteers ($n = 15$; mean age, 27.4 ± 3.5 y; age range, 20–34 y) participated in this study after having given written informed consent. One subject was scanned twice; thus, a total of 16 displacement studies were analyzed. Volunteers were screened for a history of neurologic and psychiatric diseases, head injury, and alcohol or substance abuse. With the exception of one subject on thyroxin and a second one on antihistaminic medication (fexofenadine), all subjects were without any acute or chronic medication. Caffeine intake was not allowed for at least 36 h before the subjects underwent PET. The chronic daily caffeine consumption was assessed as a multiple of cups (0.15 L) of coffee per day (1 L of caffeine-containing soft drinks was estimated to be equal to ~ 1.5 cups of coffee (23)).

MRI Acquisition

To exclude structural brain abnormalities and to define regions of interest, individual high-resolution MRI datasets were acquired (Magnetom Vision, 1.5 T; Siemens) using a 3-dimensional T1-weighted magnetization-prepared rapid-acquisition gradient-echo sequence (voxel size, $1 \times 1 \times 1$ mm).

PET Acquisition

PET measurements were performed in 3-dimensional mode on an ECAT EXACT HR+ scanner (Siemens-CTI) equipped with a circular lead shield to reduce scatter radiation from outside the field of view (NeuroInsert; Siemens-CTI). Scanning took place

with the subjects supine in quiet ambience. The volunteers' heads were immobilized in the canthomeatal orientation by a vacuum cushion or by customized head shells of polyurethane foam. A 10-min $^{68}\text{Ge}/^{68}\text{Ga}$ transmission scan was acquired to correct for attenuation. Head positions were permanently monitored and, if necessary, manually corrected under guidance of a video system and reference skin marks.

A venous catheter in a forearm vein served for tracer application. Arterialized venous blood samples were drawn from a forearm vein contralateral to the injection side. The arm was warmed by heating pads to achieve sufficient arterialization (oxygen saturation $> 80\%$).

Radiosynthesis and formulation of ^{18}F -CPFPX were performed as previously described (16). The mean specific radioactivity was 75.6 ± 70 GBq/ μmol at the start times of the scans.

^{18}F -CPFPX PET was performed according to a bolus infusion schedule as previously described (18). Three slightly different ratios of bolus versus infusion (K_{bol} [time required for injecting the dose of the bolus at a selected infusion rate]) were used: 45 min ($n = 6$), 48 min ($n = 7$), and 61 min ($n = 3$). The radioligand was diluted with sterile saline solution (0.9%) and filled into a 50-mL syringe. A standard syringe pump was used for tracer application. Dynamic PET acquisition (140 min) in list mode began with the application of the ^{18}F -CPFPX bolus.

Blood samples were collected at 15-s intervals for the first 2 min; then at 3, 4, 5, 6, 8, and 10 min; and finally at 10-min intervals until 60 min and at 15-min intervals until 140 min. An additional blood sample was taken before ^{18}F -CPFPX administration, serving for the assessment of the caffeine plasma level.

List-mode data were framed into a dynamic sequence of 9×30 , 3×60 , 3×150 , and 25×300 s. Slices ($n = 63$; thickness, 2.425 mm; pixel size, 2×2 mm) were reconstructed per time frame by filtered backprojection (Shepp filter, cutoff, 2.5 mm) after Fourier rebinning into 2-dimensional sinograms. Datasets were fully corrected for random coincidences, scatter radiation, and attenuation. The resolution of the reconstructed images varied between 4.1 mm (in full width at half maximum) in the center and 7.8 mm at 20 cm from the center. The sensitivity of the scanner for true events was 5.7 cps/Bq/mL (24).

Metabolite Analysis

The activity concentration of the whole blood and plasma (after centrifugation of whole blood for 3 min at 1,000g) was quantified. The fraction of intact radioligand of total plasma activity was determined as previously described (25).

Caffeine Administration

Caffeine (Bedford Laboratories) was dissolved in 50 mL of saline (vehicle) and applied with a standard syringe pump as short intravenous infusions between 90 and 100 min. Caffeine concentrations were determined before the start of scanning and additionally in all blood samples from the time of caffeine administration onward. Plasma levels were assessed by high-performance liquid chromatography (in triplicate). Caffeine doses were initially increased in 1 mg/kg steps from 1 mg/kg to approximately 4 mg/kg. However, because the subjects in the upper dose range complained about mild to moderate dizziness and nausea, we did not pursue a further dose escalation. Instead, we attempted to cover the aforementioned dose range in approximately equally spaced dose steps (minor deviations from perfectly equal spacing are caused by the use of a caffeine ampulla of a predefined dosage).

Image Processing and Quantitative Analyses

Interactive 3-dimensional image registration software (MPI-Tool, version 3.35; ATV) was used to align individual MRI datasets to the anterior commissure–posterior commissure line. To correct for possible head movements during the acquisition, all frames were realigned to an integrated PET image of the first 10 min using a mutual-information algorithm as implemented in MPI-Tool. The integrated PET frame was then coregistered to the individual MR image, and the resulting parameters were used to coregister the dynamic PET dataset accordingly. Because of the use of customized head shells and rigorous monitoring of patients for possible movements, we encountered only minor movements, which did not exceed the spatial resolution of the scanner. Thus, we made no attempt to realign the individual transmission scans to the emission images. Volumes of interest were defined by freehand drawing of polygonal regions of interest onto individual MR images using the software package PMOD (version 2.5; PMOD Group). Maximum reproducibility was achieved using identical regions of interest for both conditions. All analyses were performed by a single well-trained investigator using high-resolution MRI data. Thus, interrater variability was avoided. These volumes were used to generate time–activity curves. Time–activity curves were calculated for the following side-averaged cerebral volumes of interest: frontal cortex, orbitofrontal cortex, cingulate gyrus, insula, parietal cortex, occipital cortex, pre- and postcentral gyrus, temporal cortex, mesiotemporal cortex, thalamus, striatum, pons, and cerebellar cortex. Time–activity curves were corrected for the contribution of intracerebral blood volume to the regional activity assuming a fractional blood volume of 5%.

Distribution volumes were calculated using an equilibrium analysis. In the notation of a 2-tissue-compartment model, cerebral ^{18}F -CPFPX concentration can be assumed to be distributed in the intracerebral free and nonspecifically bound (nondisplaceable) (C_{ND}) compartment and in the specifically bound (displaceable) (C_{S}) compartment, as well as in a plasma compartment (C_{P}). At equilibrium conditions, ligand concentrations in the arterial and venous plasma can be assumed to be equal. The concentration of ^{18}F -CPFPX in venous plasma can therefore be used as a measure of C_{P} , as has been shown previously (18). The blood volume–corrected tissue time–activity curves summarize C_{ND} and C_{S} . Under equilibrium conditions, the total distribution volume (V_{T}) is defined as the sum of the nondisplaceable distribution volume (V_{ND}) and specific distribution volume (V_{S}), each composed of C_{ND} and C_{S} related to C_{P} (V_{T} = time–activity curve [equilibrium conditions]/ C_{P}).

Parametric images representing V_{T} were generated by dividing each frame voxelwise by its corresponding plasma concentration of ^{18}F -CPFPX. Frames were then time-averaged for the baseline and displacement conditions.

Occupancy Estimation and Estimation of Caffeine IC_{50}

To estimate the occupancy of A_1 AR by caffeine, V_{T} at baseline (70–90 min) was compared with V_{T} after caffeine administration (120–140 min). The fraction of occupancy was determined by the Lassen plot (26,27). This approach is based on the assumption that all regions have identical V_{ND} estimates. If the reduction in V_{T} by the pharmacologic intervention is plotted versus V_{T} at baseline, the slope of the resulting regression line corresponds to the occupancy and the y-axis intercept to V_{ND} . True equilibrium conditions have to be fulfilled during baseline and displacement estimations of V_{T} to gain valid estimates of V_{T} and, consequently, of fractional occupancy and V_{ND} .

On the basis of the occupancy estimates from the Lassen plot, the IC_{50} can be determined by fitting the occupancy data versus the corresponding plasma caffeine concentration using the following formula:

$$\text{Occupancy} = (\text{caffeine dose})/(\text{IC}_{50} + \text{caffeine dose}). \quad \text{Eq. 1}$$

RESULTS

^{18}F -CPFPX Bolus Infusion

Mean injected radioactivity was 346 ± 49 MBq (range, 220–370 MBq). The quantity of injected CPFPX was 17.5 ± 18.7 nmol (range, 1.6–66 nmol). The mean rate of change of the concentration of parent compound between 50 and 90 min was $6.4\% \pm 8.3\%/h$. Figure 1 depicts the time course of ^{18}F -CPFPX in plasma and the respective concentration in cerebral tissue in a representative subject. The steady state of ^{18}F -CPFPX in plasma and tissue was achieved 40–50 min after the start of injection. On infusion, caffeine displaced ^{18}F -CPFPX rapidly in all brain regions. It also led to an increase of the plasma concentration of ^{18}F -CPFPX (Fig. 1) by competitive inhibition of CYP1A2 (as previously described in the studies by Meyer et al. (18) and Matusch et al. (28)). The tissue-to-plasma ratio (reflecting V_{T} during equilibrium) attained steady-state conditions after 60–70 min. Average regional V_{T} estimates, based on the tissue-to-plasma ratio between 70 and 90 min, can be found in Table 1. The V_{T} values found in the present study are in agreement with previously reported values (18).

Caffeine Plasma Levels

There is a highly significant, linear relationship ($r = 0.94$, $P < 10^{-8}$) between intravenously applied caffeine doses (per body weight) and attained caffeine plasma concentrations (Fig. 2, left). The time course of plasma caffeine concentrations is displayed on the right graph in Figure 2.

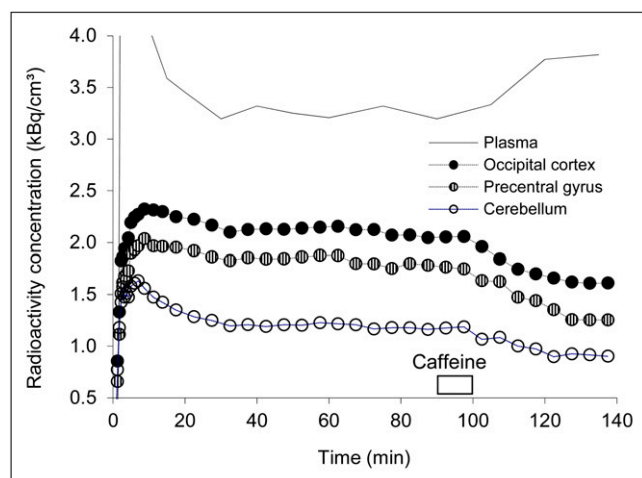


FIGURE 1. Representative regional time–activity curves and corresponding concentration of unmetabolized ^{18}F -CPFPX in plasma in subject who received highest dose of caffeine and showed highest displacement (caffeine challenge at 90–100 min with a dose of 4.3 mg/kg of body weight).

[Fig. 1]

[Table 1]

[Fig. 2]

RGB

TABLE 1
Regional V_T at Baseline

Region	V_T
Cerebellum	0.45 ± 0.08
Pons	0.46 ± 0.10
Thalamus	0.82 ± 0.16
Precentral gyrus	0.68 ± 0.13
Postcentral gyrus	0.72 ± 0.13
Cingulate gyrus	0.72 ± 0.15
Orbitofrontal gyrus	0.75 ± 0.14
Parietal cortex	0.79 ± 0.17
Occipital cortex	0.92 ± 0.02
Insula	0.70 ± 0.15
Mesiotemporal cortex	0.65 ± 0.13
Striatum	0.83 ± 0.15
Frontal cortex	0.77 ± 0.16
Temporal cortex	0.80 ± 0.14
Caudate nucleus	0.74 ± 0.16
Putamen	0.84 ± 0.17

Data are mean ± SD.

After an initial distribution phase, stable caffeine levels were observed from 120 min onward. This observation is in line with the terminal half-life of caffeine of approximately 5–6 h. Caffeine doses in the range of 0–9 mg/L were achieved at a time point of 120 min, which was used for further estimations of IC_{50} values.

Impact of Caffeine on ^{18}F -CPFPX V_T and Estimation of Caffeine IC_{50}

Caffeine displaced ^{18}F -CPFPX in a dose-dependent manner. Parametric images of V_T of 1 subject before and after caffeine administration are shown in Figure 3. Representative time courses of the apparent V_T after various doses of caffeine are plotted in Figure 4. The vehicle did not significantly affect V_T . Caffeine led also to a dose-dependent reduction of V_T in the cerebellum, the region with the lowest binding in the human brain. Maximum V_T displacement in the cerebellum was 33% at the highest caffeine dose.

Lassen plots and fits of all subjects are displayed in Figure 5. The maximum occupancy achieved in this study was 44%

(4.27 mg/kg). Cerebral A_1AR occupancy was clearly dependent on the plasma caffeine level (Fig. 6). According to Equation 1, the IC_{50} of caffeine amounted to 12.5 mg/L (SE of fit, 1.5 mg/L). V_{ND} based on the Lassen plot (x -axis intercept) was 0.11 ± 0.10 , which corresponds to one quarter of the average cerebellum V_T . [Fig. 6]

DISCUSSION

Caffeine is the most commonly and broadly used neurostimulant. Therefore, it is a longstanding desire in neuroscience and addiction research to investigate the effects of caffeine directly in the human brain. We used the PET tracer ^{18}F -CPFPX to visualize and quantify the occupancy of the A_1AR , the most abundant caffeine target in the human brain. The present study demonstrates that ^{18}F -CPFPX is highly displaceable by caffeine and allows the determination of the occupancy of A_1AR s by caffeine in vivo and in a quantitative manner.

On the basis of the present PET study, the IC_{50} of caffeine amounts to approximately 13 mg/L, corresponding to about 67 μM caffeine in plasma. This value can be extrapolated to an oral caffeine intake of 450 mg in a 70-kg subject, which corresponds to approximately 4–5 cups of coffee. It is therefore likely that usually consumed amounts of coffee and caffeinated beverages (29) result in brain concentrations of caffeine that block substantial portions of cerebral A_1AR s. Because A_1AR s are quantitatively the most important neocortical binding sites of caffeine in the human brain, it is likely that the cognition-enhancing effects of caffeine are exerted by this adenosine receptor subtype. With regard to future A_1AR PET studies, it is important to keep in mind that acute caffeine consumption will severely bias quantitative A_1AR PET measurement. Thus, a sufficiently long caffeine abstinence is mandatory before scanning.

This is the first, to our knowledge, in vivo study on cerebral A_1AR occupation by caffeine in humans. Therefore, it is interesting to compare our results with previous in vitro investigations. We recently determined the IC_{50} of caffeine in human postmortem frontal cortex homogenates. Using 3H -CPFPX, the tritiated analog of ^{18}F -CPFPX, we

[Fig. 3]
[Fig. 4]
[Fig. 5]

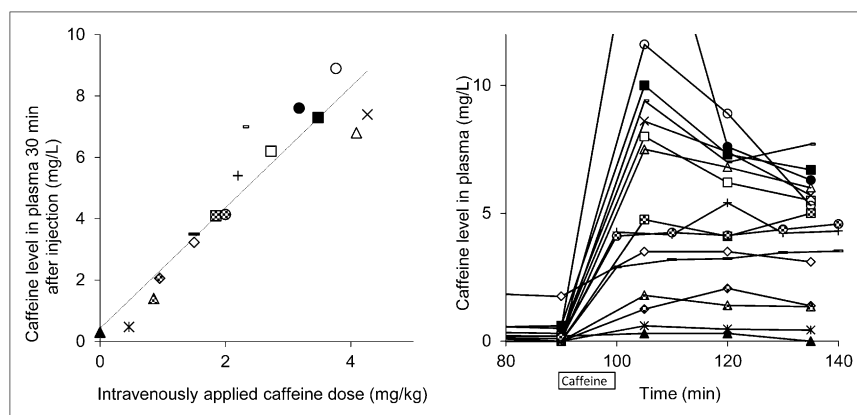


FIGURE 2. (Left) Correlation between caffeine doses and caffeine plasma levels determined 30 min after intravenous application of caffeine (dotted regression line). (Right) Time course of individual plasma caffeine levels (time scale corresponds to PET experiments). Identical markers for each subject were used in Figure 2 (left and right) and Figure 5.

RGB

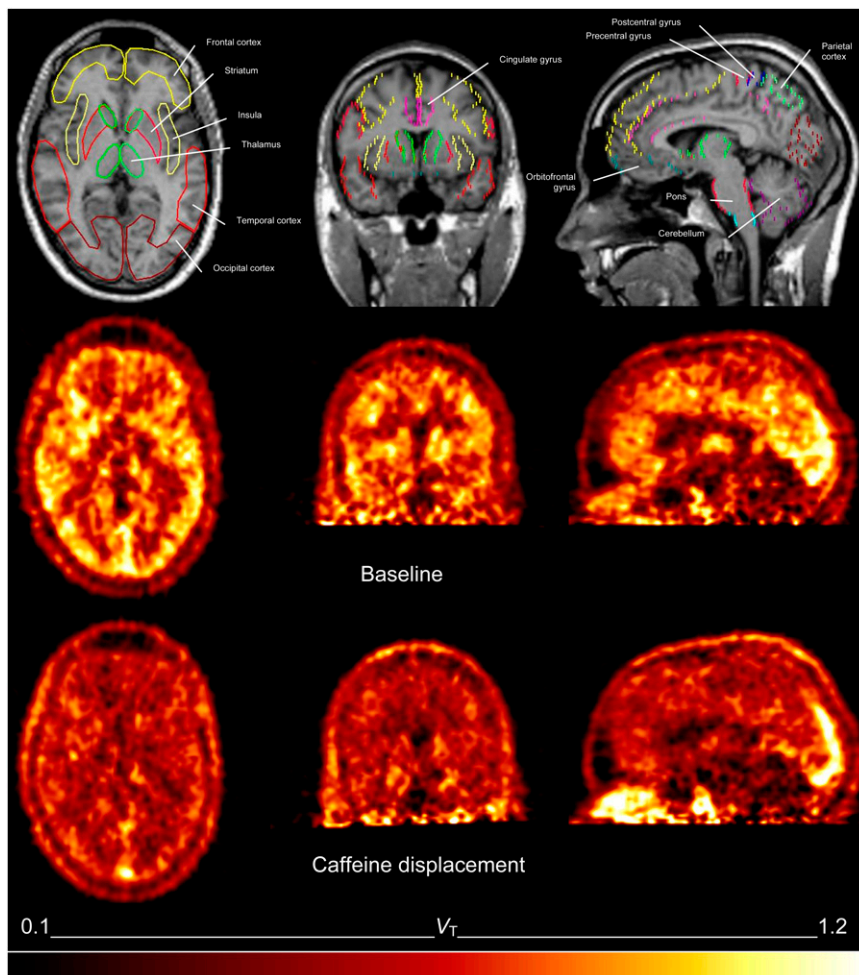


FIGURE 3. Representative parametric images of total distribution volume of 1 subject at baseline (average from 60 to 85 min, middle) and after 4.1 mg/kg dose of caffeine (average from 115 to 140 min, bottom). Corresponding anatomic MR images, with overlay of regions of interest, were used for analysis (top).

determined the *in vitro* IC_{50} to be in the range of 113–170 μM . To compare these values with the *in vivo* data, assumptions about the biodistribution of caffeine have to be made because no human data on intercellular caffeine accumulation are available. The ratio of plasma caffeine to CSF caffeine is close to 1 in rats (10). Assuming the cellular conditions in humans and rats are comparable in this respect, the IC_{50} for plasma will then lead to a CSF concentration of 67 μM , which is about half the *in vitro* value. This discrepancy might be caused by species differences in the plasma-to-CSF ratio, the *in vivo* versus the *in vitro* settings of the experiments, or postmortem changes. Besides these technical reasons, the presence of caffeine metabolites, which are probably also binding to the A_1AR , might explain the difference between *in vivo* and *in vitro* conditions as well. For instance, theophylline binds to A_1AR s with a K_i (binding affinity of the inhibitor) of 8.5 μM (30), and theobromine, another metabolite, has a K_i comparable to that of caffeine (97–197 μM) (31). Psychoactive Drug Screening Program database). Finally, incomplete kinetic equilibration after caffeine administration may also contribute to a possible underestimation of the IC_{50} : although stable concentrations of ^{18}F -CPFPX in plasma and the cerebral compartment were attained at baseline

(70–90 min), plasma concentrations of ^{18}F -CPFPX rose after caffeine administration. This increase of plasma concentration is most likely caused by competitive inhibition of caffeine and CPFPX at their common hepatic enzyme

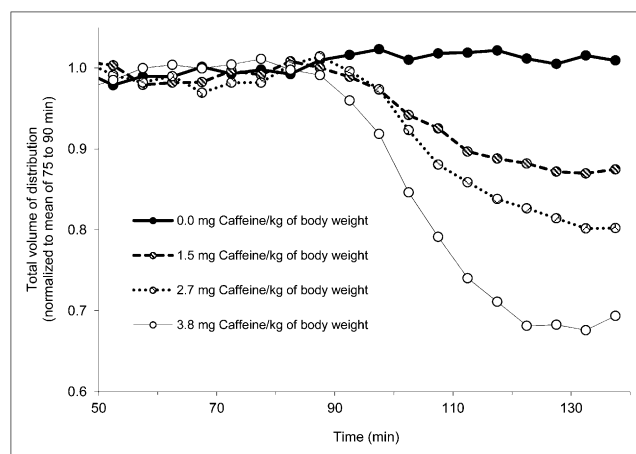


FIGURE 4. Dose-dependent displacement of ^{18}F -CPFPX by caffeine in frontal cortex. V_T is plotted vs. time for 4 subjects who received different doses of caffeine or vehicle at 90–100 min. For visualization purposes, V_T was normalized to mean of 75–90 min.

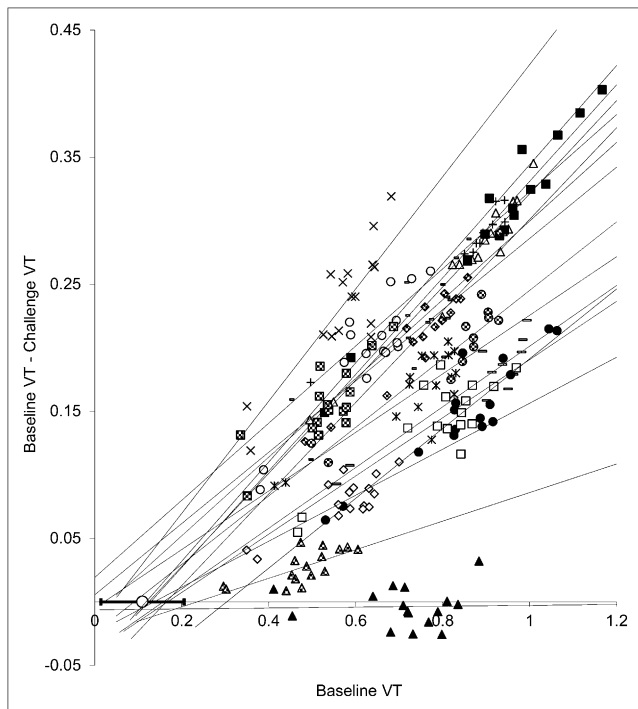


FIGURE 5. Occupancy (Lassen) plots obtained from 15 doses of caffeine and vehicle (\blacktriangle). Lines represent regression lines for each subject or dose. The open circle overlaid on x -axis shows average V_{ND} (corresponding to x -axis intercepts of regression lines). Error bars indicate SD of all experiments (except vehicle).

CYP1A2 (18,28). The changed equilibrium of ^{18}F -CPFPX in plasma and tissue may accordingly not have been fully attained between 120 and 140 min (Fig. 1, precentral gyrus). Because the cerebral kinetics of ^{18}F -CPFPX may be delayed relative to plasma kinetics, V_T could be overestimated during displacement, resulting in an underestimation of IC_{50} . However, available data up to 140 min suggest that the underestimation is less than 5%.

The present estimate of V_{ND} from the Lassen plots is relatively low (V_{ND} , 0.11 ± 0.10), corresponding to about one quarter of the cerebellar V_T . In an earlier ^{18}F -CPFPX displacement study using unlabeled CPFPX, V_{ND} was about two thirds of the V_T of the cerebellum (19). Again, incomplete equilibration might be accountable for this difference. In a previous study, we have carefully evaluated changes of specific binding in the reference region with regard to their effects on noninvasive outcome parameters such as the binding potential (20). We also investigated the constraints for using the cerebellum as a reference region, which allows omitting blood sampling and reduces the additional noise introduced by blood analyses.

In the field of neuroimaging (especially the blood oxygen level-dependent [BOLD] contrast imaging–functional MRI), caffeine is known to lower the resting state or baseline BOLD signal (32). It is likely that the observed caffeine effects on the BOLD contrast are a combination of the increased neuronal activation (33) through a disinhibitory mechanism at the

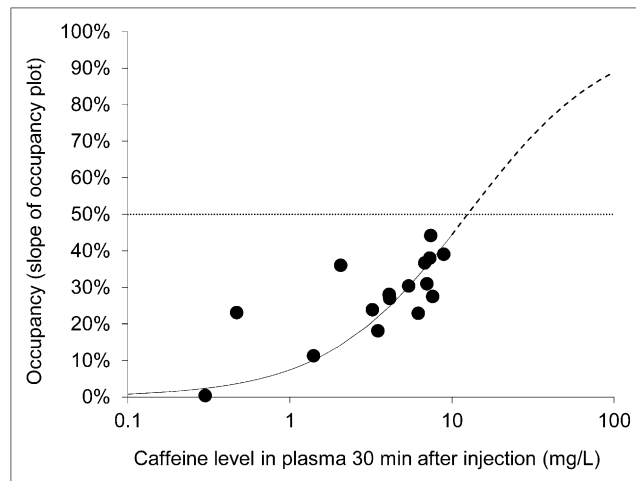


FIGURE 6. Relationship between caffeine plasma concentration and A_1AR occupancy ($n = 16$) estimated for all regions using slope of occupancy (Lassen) plot. Line represents corresponding fit used to determine IC_{50} (dotted line), with maximal occupancy constrained to 100%. Solid line represents fit according to Equation 1, and dashed line represents extrapolated values of this fit for higher concentrations of caffeine (as described in “Materials and Methods” section).

A_1AR and a reduction of the cerebral blood flow (34) by inhibition of vascular A_{2A} adenosine receptors. The present method of A_1AR occupancy measurements with ^{18}F -CPFPX, by providing individual data of A_1AR densities and acute caffeine effects in a regional and quantitative manner, could help to solve current inconsistencies in findings related to caffeine and functional MRI (32).

An important finding of the present study is that in most regular consumers of caffeine, about half of the cerebral A_1AR s may be occupied by caffeine. It is likely that this phasic blockade of a substantial amount of cerebral A_1AR s will result in adaptive changes and lead to chronic alterations of receptor expression and availability. There is substantial epidemiologic evidence that caffeine is protective against neurodegenerative diseases such as Parkinson or Alzheimer disease. Several investigations (e.g., the Cardiovascular Risk Factors, Aging and Dementia study) show that moderate coffee consumption of 3–5 cups per day at mid life is linked to a smaller risk of dementia in late life (35). The present study provides evidence that typical caffeine doses result in a high phasic receptor occupancy, which will most likely induce chronic cerebral, especially neocortical, A_1AR changes. These findings support the view that the A_1AR deserves broader attention in the context of neurodegenerative disorders. Further studies will be needed to investigate the precise interplay of age, adenosine receptors, and neurodegenerative pathophysiology.

CONCLUSION

This study demonstrates that caffeine occupancy studies of the cerebral A_1AR can be performed with ^{18}F -CPFPX bolus-plus-constant-infusion PET protocols. Our data provide evidence that repeated intake of caffeinated

beverages results in a 50% occupancy of the cerebral A₁AR during longer periods of the day. ¹⁸F-CPFPX PET represents a valuable technique for studying the neurostimulant and chronic neuroplastic effects of caffeine in humans.

DISCLOSURE STATEMENT

The costs of publication of this article were defrayed in part by the payment of page charges. Therefore, and solely to indicate this fact, this article is hereby marked “advertisement” in accordance with 18 USC section 1734.

ACKNOWLEDGMENTS

We thank Dirk Bier, Marcus H. Holschbach, Jürgen Burhenne, and Walter E. Haefeli for the determination of plasma caffeine levels. We gratefully acknowledge Marlene Vögeling, Lutz Tellmann, Elisabeth Theelen, Suzanne Schaden, Hans Herzog, and Markus Lang for excellent technical assistance and Johannes Ermert, Silke Grafmüller, Bettina Palm, and Erika Wabbals for the synthesis of ¹⁸F-CPFPX. This work was supported by the Federal Ministry of Education and Research, Germany (FKZ01GP1002B). No other potential conflict of interest relevant to this article was reported.

REFERENCES

1. Brunyé TT, Mahoney CR, Lieberman HR, Taylor HA. Caffeine modulates attention network function. *Brain Cogn.* 2010;72:181–188.
2. Suzuki F, Shimada J, Shiozaki S, et al. Adenosine A₁ antagonists. 3. Structure-activity relationships on amelioration against scopolamine- or N₆-(R)-phenylisopropyl adenosine-induced cognitive disturbance. *J Med Chem.* 1993;36:2508–2518.
3. Prediger RD, Takahashi RN. Modulation of short-term social memory in rats by adenosine A₁ and A_{2A} receptors. *Neurosci Lett.* 2005;376:160–165.
4. Chen Y, Parrish TB. Caffeine dose effect on activation-induced BOLD and CBF responses. *Neuroimage.* 2009;46:577–583.
5. Landolt HP, Retey JV, Tonz K, et al. Caffeine attenuates waking and sleep electroencephalographic markers of sleep homeostasis in humans. *Neuropsychopharmacology.* 2004;29:1933–1939.
6. Landolt HP, Dijk DJ, Gaus SE, Borbely AA. Caffeine reduces low-frequency delta activity in the human sleep EEG. *Neuropsychopharmacology.* 1995;12:229–238.
7. Blanchard J, Sawers SJ. The absolute bioavailability of caffeine in man. *Eur J Clin Pharmacol.* 1983;24:93–98.
8. Arnaud MJ, Bracco I, Welsch C. Metabolism and distribution of labeled theophylline in the pregnant rat: impairment of theophylline metabolism by pregnancy and absence of a blood-brain barrier in the fetus. *Pediatr Res.* 1982;16:167–171.
9. Bonati M, Latini R, Galletti F, Young JF, Tognoni G, Garattini S. Caffeine disposition after oral doses. *Clin Pharmacol Ther.* 1982;32:98–106.
10. Liu X, Smith BJ, Chen C, et al. Evaluation of cerebrospinal fluid concentration and plasma free concentration as a surrogate measurement for brain free concentration. *Drug Metab Dispos.* 2006;34:1443–1447.
11. Lazarus M, Shen HY, Cherasse Y, et al. Arousal effect of caffeine depends on adenosine A_{2A} receptors in the shell of the nucleus accumbens. *J Neurosci.* 2011;31:10067–10075.
12. Chen JF, Yu L, Shen HY, He JC, Wang X, Zheng R. What knock-out animals tell us about the effects of caffeine. *J Alzheimers Dis.* 2010;20(suppl 1):S17–S24.
13. Huang ZL, Qu WM, Eguchi N, et al. Adenosine A_{2A}, but not A₁, receptors mediate the arousal effect of caffeine. *Nat Neurosci.* 2005;8:858–859.
14. Bauer A, Holschbach MH, Meyer PT, et al. In vivo imaging of adenosine A₁ receptors in the human brain with [¹⁸F]CPFPX and positron emission tomography. *Neuroimage.* 2003;19:1760–1769.
15. Bauer A, Holschbach MH, Cremer M, et al. Evaluation of ¹⁸F-CPFPX, a novel adenosine A₁ receptor ligand: in vitro autoradiography and high-resolution small animal PET. *J Nucl Med.* 2003;44:1682–1689.
16. Holschbach MH, Olsson RA, Bier D, et al. Synthesis and evaluation of no-carrier-added 8-cyclopentyl-3-(3-[¹⁸F]fluoropropyl)-1-propylxanthine ([¹⁸F]CPFPX): a potent and selective A₁-adenosine receptor antagonist for in vivo imaging. *J Med Chem.* 2002;45:5150–5156.
17. Fukumitsu N, Ishii K, Kimura Y, et al. Imaging of adenosine A₁ receptors in the human brain by positron emission tomography with [¹¹C]MPDX. *Ann Nucl Med.* 2003;17:511–515.
18. Meyer PT, Elmenhorst D, Bier D, et al. Quantification of cerebral A₁ adenosine receptors in humans using [¹⁸F]CPFPX and PET: an equilibrium approach. *Neuroimage.* 2005;24:1192–1204.
19. Meyer PT, Elmenhorst D, Matusch A, Winz O, Zilles K, Bauer A. A₁ adenosine receptor PET using [¹⁸F]CPFPX: displacement studies in humans. *Neuroimage.* 2006;32:1100–1105.
20. Elmenhorst D, Meyer PT, Matusch A, Winz OH, Zilles K, Bauer A. Test-retest stability of cerebral A₁ adenosine receptor quantification using [¹⁸F]CPFPX and PET. *Eur J Nucl Med Mol Imaging.* 2007;34:1061–1070.
21. Elmenhorst D, Garibotto V, Prescher A, Bauer A. Adenosine A₁ receptors in human brain and transfected CHO cells: inhibition of [³H]CPFPX binding by adenosine and caffeine. *Neurosci Lett.* 2011;487:415–420.
22. Meyer PT, Bier D, Holschbach MH, Cremer M, Tellmann L, Bauer A. Image of the month: in vivo imaging of rat brain A₁ adenosine receptor occupancy by caffeine. *Eur J Nucl Med Mol Imaging.* 2003;30:1440.
23. Mandel HG. Update on caffeine consumption, disposition and action. *Food Chem Toxicol.* 2002;40:1231–1234.
24. Brix G, Zaers J, Adam LE, et al. Performance evaluation of a whole-body PET scanner using the NEMA protocol. National Electrical Manufacturers Association. *J Nucl Med.* 1997;38:1614–1623.
25. Meyer PT, Bier D, Holschbach MH, et al. Quantification of cerebral A₁ adenosine receptors in humans using [¹⁸F]CPFPX and PET. *J Cereb Blood Flow Metab.* 2004;24:323–333.
26. Cunningham VJ, Rabiner EA, Slifstein M, Laruelle M, Gunn RN. Measuring drug occupancy in the absence of a reference region: the Lassen plot re-visited. *J Cereb Blood Flow Metab.* 2010;30:46–50.
27. Lassen NA, Bartenstein PA, Lammertsma AA, et al. Benzodiazepine receptor quantification in vivo in humans using [¹¹C]flumazenil and PET: application of the steady-state principle. *J Cereb Blood Flow Metab.* 1995;15:152–165.
28. Matusch A, Meyer PT, Bier D, et al. Metabolism of the A₁ adenosine receptor PET ligand [¹⁸F]CPFPX by CYP1A2: implications for bolus/infusion PET studies. *Nucl Med Biol.* 2006;33:891–898.
29. Fredholm BB, Battig K, Holmen J, Nehlig A, Zvartau EE. Actions of caffeine in the brain with special reference to factors that contribute to its widespread use. *Pharmacol Rev.* 1999;51:83–133.
30. Bruns RF, Lu GH, Pugsley TA. Characterization of the A₂ adenosine receptor labeled by [³H]NECA in rat striatal membranes. *Mol Pharmacol.* 1986; 29:331–346.
31. Fredholm BB, Lindstrom K. Autoradiographic comparison of the potency of several structurally unrelated adenosine receptor antagonists at adenosine A₁ and A_{2A} receptors. *Eur J Pharmacol.* 1999;380:197–202.
32. Laurienti PJ, Field AS, Burdette JH, Maldjian JA, Yen YF, Moody DM. Relationship between caffeine-induced changes in resting cerebral perfusion and blood oxygenation level-dependent signal. *AJNR.* 2003;24:1607–1611.
33. Koppelstaetter F, Poeppel TD, Siedentopf CM, et al. Does caffeine modulate verbal working memory processes? An fMRI study. *Neuroimage.* 2008;39:492–499.
34. Chen Y, Parrish TB. Caffeine's effects on cerebrovascular reactivity and coupling between cerebral blood flow and oxygen metabolism. *Neuroimage.* 2009;44:647–652.
35. Santos C, Costa J, Santos J, Vaz-Carneiro A, Lunet N. Caffeine intake and dementia: systematic review and meta-analysis. *J Alzheimers Dis.* 2010;20(suppl 1):S187–S204.