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# Nondisplaceable Binding Is a Potential Confounding Factor in $^{11}\text{C}$ -PBR28 Translocator Protein PET Studies

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The PET ligand  $^{11}\text{C}$ -PBR28 (*N*-((2-(methoxy- $^{11}\text{C}$ )-phenyl)methyl)-*N*-(6-phenoxy-3-pyridinyl)acetamide) binds to the 18-kDa translocator protein (TSPO), a biomarker of glia. In clinical studies of TSPO, the ligand total distribution volume,  $V_T$ , is frequently the reported outcome measure. Since  $V_T$  is the sum of the ligand-specific distribution volume ( $V_S$ ) and the nondisplaceable-binding distribution volume ( $V_{ND}$ ), differences in  $V_{ND}$  across subjects and groups will have an impact on  $V_T$ . **Methods:** Here, we used a recently developed method for simultaneous estimation of  $V_{ND}$  (SIME) to disentangle contributions from  $V_{ND}$  and  $V_S$ . Data from 4 previously published  $^{11}\text{C}$ -PBR28 PET studies were included: before and after a lipopolysaccharide challenge (8 subjects), in alcohol use disorder (14 patients, 15 controls), in first-episode psychosis (16 patients, 16 controls), and in Parkinson disease (16 patients, 16 controls). In each dataset, regional  $V_T$  estimates were obtained with a standard 2-tissue-compartment model, and brain-wide  $V_{ND}$  was estimated with SIME.  $V_S$  was then calculated as  $V_T - V_{ND}$ .  $V_{ND}$  and  $V_S$  were then compared across groups, within each dataset. **Results:** A lower  $V_{ND}$  was found for individuals with alcohol-use disorder (34%,  $P = 0.00084$ ) and Parkinson disease (34%,  $P = 0.0032$ ) than in their corresponding controls. We found no difference in  $V_{ND}$  between first-episode psychosis patients and their controls, and the administration of lipopolysaccharide did not change  $V_{ND}$ . **Conclusion:** Our findings suggest that in TSPO PET studies, nondisplaceable binding can differ between patient groups and conditions and should therefore be considered.

**Key Words:** PET; translocator protein;  $^{11}\text{C}$ -PBR28; simultaneous estimation; kinetic modeling

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**P**ET with radioligands for the glial marker 18-kDa translocator protein (TSPO) has been extensively used over the past 2 decades to assess brain immune function in vivo (1).  $^{11}\text{C}$ -PBR28 (*N*-((2-(methoxy- $^{11}\text{C}$ )-phenyl)methyl)-*N*-(6-phenoxy-3-pyridinyl)acetamide) is a second-generation TSPO radioligand with signal-to-noise characteristics superior to those of the first-generation radioligand  $^{11}\text{C}$ -PK11195 (2). As with other second-generation TSPO tracers, the affinity of  $^{11}\text{C}$ -PBR28 to TSPO is affected by a single-nucleotide polymorphism on the TSPO gene (rs6971), and in clinical studies, TSPO genotype is used to classify subjects as low-, mixed-, or high-affinity binders (3,4).

PET ligand binding to TSPO is often quantified by fitting a 2-tissue-compartment model (2TCM), or variants thereof (5), to the PET time–activity curves, using parent radioligand concentration in arterial plasma as the input function. The 2TCM describes the ligand kinetics using 2 tissue compartments, one for ligand that is bound specifically to the target of interest and one for nondisplaceable binding. The nondisplaceable compartment includes both free and nonspecifically bound radioligand. The standard outcome measure reported using 2TCM is the total distribution volume ( $V_T$ ), which represents the ratio of total activity concentration in tissue to that in plasma at equilibrium.  $V_T$  is the sum of the nondisplaceable and specific distribution volumes ( $V_T = V_{ND} + V_S$ ). Some radioligands display negligible specific binding in a certain brain region (i.e.,  $V_S = 0$ ). Such a region is usually referred to as a reference region and can be used to estimate  $V_{ND}$ , which is assumed to be constant throughout the brain. When a reference region is available, the binding potential with nondisplaceable uptake as a reference,  $BP_{ND} (=V_S/V_{ND})$ , is typically the reported

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outcome measure. TSPO is expressed throughout the brain, and thus, no reference region exists for this target. It is therefore challenging to obtain reliable estimates of the relative contributions from the specific and nondisplaceable binding, leaving a degree of uncertainty about the interpretation of  $V_T$ .

Recently, a method for simultaneous estimation of  $V_{ND}$  (SIME) (6) was developed to estimate  $V_{ND}$  for tracers without a reference region. SIME uses the assumption that nondisplaceable binding is constant throughout the brain and estimates a global value for  $V_{ND}$  by fitting a constrained 2TCM for several brain regions simultaneously. The performance of SIME with  $^{11}\text{C-PBR28}$  has been thoroughly tested in healthy human subjects (7). Using simulations, pharmacologic competition data, and test–retest data, SIME-derived estimates of  $V_{ND}$  and  $V_S$  (calculated using 2TCM  $V_T$  and SIME  $V_{ND}$ ) were shown to be accurate and reliable (7).

For comparison of  $V_T$  between groups to be meaningful, there must be an underlying assumption that  $V_{ND}$  is the same across the groups. Currently, there is limited scientific evidence to back up this assumption. Hence, our aim with this study was to investigate whether nondisplaceable binding can be a confounding factor in TSPO PET studies that use  $V_T$  as an outcome measure. To achieve this aim, SIME was used to quantify  $V_{ND}$  in  $^{11}\text{C-PBR28}$  data from 4 different published datasets. In the first dataset, an immune stimulator was administered to healthy subjects (8). The 3 remaining datasets contain controls and subjects with alcohol-use disorder (AUD) (9), first-episode psychosis (FEP) (10), and Parkinson disease (PD) (11).

## MATERIALS AND METHODS

This study includes 4 datasets obtained at 2 PET centers. All subjects underwent a  $^{11}\text{C-PBR28}$  PET scan in a high-resolution research tomograph (Siemens). Metabolite-corrected arterial input functions were collected for all scans. T1-weighted MRI scans were acquired to define regions of interest (ROIs). All subjects were genotyped for the rs6971 polymorphism, and low-affinity binders were excluded. In previous publications,  $V_T$  has been the primary reported

outcome measure. A list of the datasets, with subject information, is reported in Table 1, and the reader is referred to the original publications for further details on data acquisition and processing.

### Lipopolysaccharide

The lipopolysaccharide dataset (8) was collected at the Yale PET Center. Eight healthy men were scanned twice on the same day, at baseline and 3 h after injection of lipopolysaccharide (dose 1.0 ng/kg), an acute immune stimulus.  $^{11}\text{C-PBR28}$  was injected as a 1-min bolus, and the PET scan duration was 120 min.

### AUD

The AUD dataset (9) was collected at the Yale PET center. It consists of 14 subjects with AUD and 15 age-matched control subjects. Five of the control subjects also participated in the lipopolysaccharide experiment. AUD subjects were imaged 1–4 d (in 1 case, 24 d) after intake of their last alcoholic beverage.  $^{11}\text{C-PBR28}$  was injected as a 1-min bolus, and the PET scan duration was 120 min.

### FEP

The FEP dataset (10) was collected at Karolinska Institutet. It consists of 16 FEP patients and 16 age-matched controls. All patients were naïve to antipsychotic drugs.  $^{11}\text{C-PBR28}$  was injected as a 10-s bolus, and the PET scan duration was approximately 90 min.

### PD

The PD dataset (11) was collected at Karolinska Institutet. It consists of 16 patients with PD and 16 age-matched controls.  $^{11}\text{C-PBR28}$  was injected as a 10-s bolus, and the PET scan duration was 72 min.

### SIME

The SIME method (6) works by first defining a grid of possible  $V_{ND}$  values. Then, for each value in the grid, a 2TCM is fitted to the time–activity curves with the constraint that  $K_1 = V_{ND} \cdot k_2$  in all ROIs, reducing the number of rate constants from 4 to 3. The residual sum of squares is then computed for all ROIs and frames, and the  $V_{ND}$  that yields the lowest residual sum of squares is selected as the estimate of a brain-wide  $V_{ND}$ .

**TABLE 1**  
Dataset Summary

Dataset	Group	Subjects (n)		Age	
		HABs	MABs	HABs	MABs
Sandiego, 2015	Lipopolysaccharide	3	5	28.0 ± 6.0 (22.7–34.5)	23.6 ± 5.1 (19.1–31.1)
Hillmer, 2017	AUD				
	Controls	8	7	37.4 ± 9.0 (26.3–48.4)	32.8 ± 14.6 (19.1–55.6)
	Patients	7	7	40.9 ± 7.9 (31.6–55.2)	37.9 ± 10.4 (26.9–51.0)
Collste, 2017	FEP				
	Controls	9	7	27.8 ± 9.3 (22–50)	25.7 ± 8.2 (20–43)
	Patients	6	10	29.8 ± 8.2 (20–40)	27.7 ± 8.8 (19–47)
Varnäs, 2019	PD				
	Controls	8	8	64.9 ± 4.9 (57.8–71.5)	62.1 ± 5.3 (56.1–72.0)
	Patients	8	8	63.6 ± 4.3 (57.1–69.1)	63.4 ± 6.4 (55.2–73.2)

HAB = high-affinity binder; MAB = mixed-affinity binder.  
Age is given as mean ± SD, followed by range in parentheses.

For all datasets, we used a  $V_{ND}$  grid from 0.01 to 5, with steps of 0.01, based on previous studies with SIME and  $^{11}C$ -PBR28 (7,12). Initial evaluation of the data indicated that this range covers the cost function minimum. The residual sum of squares was weighted by the square root of the frame duration. Fractional blood volume was fitted for each ROI separately. SIME  $V_{ND}$  was calculated using time-activity curves from the cerebellum, parietal cortex, frontal cortex, occipital cortex, temporal cortex, putamen, caudate, and thalamus, thus covering various brain structures and tissue types.

### Calculation of Outcome Measures and ROIs

In each ROI,  $V_T$  was calculated using a standard 2TCM, including fitting of the fractional blood volume.  $V_S (=V_T - V_{ND})$  was calculated from the 2TCM  $V_T$  estimates and the SIME  $V_{ND}$  estimates. For all datasets except the PD dataset, we report ROI-specific outcome measures ( $V_T$ ,  $V_S$ ) in the cerebellum and frontal cortex. For PD, we report  $V_T$  and  $V_S$  in the striatum instead of the frontal cortex, because the striatum is considered a key region in the pathophysiology of PD and is more frequently reported in PET studies.

### Statistical Analysis

Statistical analyses were performed using MATLAB (version 9.5; MathWorks). For the lipopolysaccharide data, a paired-sample  $t$  test was used for all outcome measures ( $V_{ND}$ ,  $V_T$ , and  $V_S$ ) to test for a difference between the pre- and postlipopolysaccharide scans. The percentage change in the outcome measures for each subject was calculated as  $100 \cdot (\text{pre} - \text{post})/\text{pre}$ . For the remaining datasets, a univariate 2-way ANOVA without an interaction term was applied for each outcome measure ( $V_{ND}$ ,  $V_T$ , and  $V_S$ ) to determine the group differences between controls and patients, with log-transformed outcome measures as a dependent variable and diagnosis and genotype as fixed factors, as described earlier (12). Using the regression coefficients,  $\beta$ , from the ANOVA, the percentage difference between patients and controls across genotypes was calculated as  $100 \cdot (e^{\beta_{\text{patient}}} - \beta_{\text{control}} - 1)$ . The  $\alpha$ -level was set to 0.05. Reported  $P$  values were not corrected for multiple comparisons.

## RESULTS

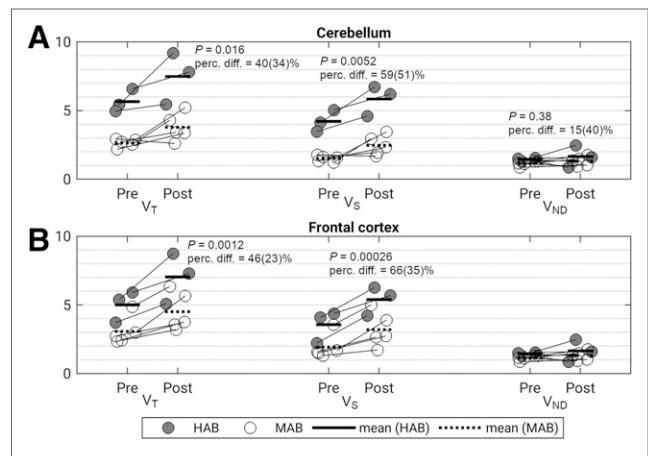
For all datasets, the results obtained for  $V_T$  are in accordance with those in the original publications. Below, we report the results for  $V_T$ ,  $V_S$ , and  $V_{ND}$  for each dataset separately. The results for the ROIs presented below are consistent with the remaining ROIs included in the SIME calculation (Supplemental Tables 1–4; supplemental materials are available at <http://jnm.snmjournals.org>). Results were also unchanged when an interaction term was included in the ANOVA (Supplemental Tables 5–7) and when volume-based weights were used in the SIME analysis (Supplemental Tables 8–11).

### Lipopolysaccharide

Lipopolysaccharide injection was associated with a significant increase in  $V_T$  in both the cerebellum (mean, 40% [SD, 34%];  $P = 0.016$ ) and the frontal cortex (mean, 46% [SD, 23%];  $P = 0.0012$ ).  $V_{ND}$  was not affected by lipopolysaccharide (mean, 15% [SD, 40%];  $P = 0.38$ ). The mean increase in  $V_S$  was 59% (SD, 51%) ( $P = 0.0052$ ) in the cerebellum and 66% (SD, 35%) ( $P = 0.00026$ ) in the frontal cortex. The results are summarized in Figure 1.

### AUD

$V_T$  was significantly lower in AUD subjects than in controls, both in the cerebellum (18%,  $P = 0.012$ ) and in the frontal cortex (23%,  $P = 0.0048$ ).  $V_{ND}$  was 34% lower in patients than in controls ( $P = 0.00084$ ).  $V_S$  did not differ significantly between the groups. These results are shown in Figure 2. Genotype had a significant effect on both  $V_T$  and  $V_S$  ( $P < 0.0005$ ) but not on  $V_{ND}$ .



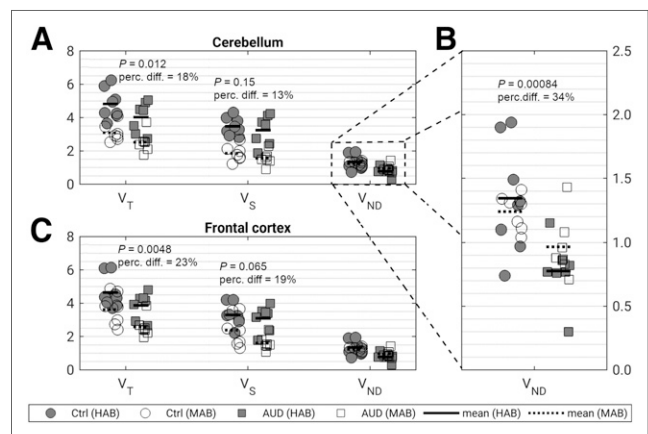
**FIGURE 1.** Change in outcome measures ( $V_T$ ,  $V_S$ , and  $V_{ND}$ ) between pre- and postlipopolysaccharide scans in cerebellum (A) and frontal cortex (B). Individual subjects are connected with a line.  $P$  values and percentage difference (perc. diff.) between pre- and postlipopolysaccharide scans are shown. HAB = high-affinity binder; MAB = mixed-affinity binder.

### FEP

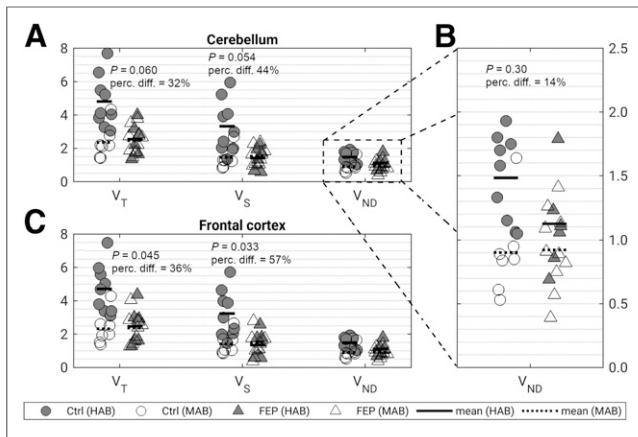
In the FEP dataset,  $V_T$  was overall lower in patients than in controls (32%,  $P = 0.060$  in the cerebellum; 36%,  $P = 0.045$  in the frontal cortex). There was no significant difference in  $V_{ND}$  between patients and controls ( $P = 0.30$ ).  $V_S$  exhibited a larger percentage separation between patients and controls than that observed for  $V_T$  in both the cerebellum (44%,  $P = 0.054$ ) and the frontal cortex (57%,  $P = 0.033$ ). The results are shown in Figure 3. The effect of genotype was statistically significant for  $V_T$  in the cerebellum and frontal cortex ( $P = 0.011$  and  $0.017$ , respectively), for  $V_{ND}$  in the ■■■ ( $P = 0.0043$ ), and for  $V_S$  in the frontal cortex ( $P = 0.017$ ) but not in the cerebellum ( $P = 0.099$ ).

### PD

In the PD dataset, we found no statistically significant difference in  $V_T$  or  $V_S$  between patients and controls, in either the cerebellum ( $P = 0.74$  for  $V_T$ ,  $P = 0.11$  for  $V_S$ ) or the striatum ( $P = 0.32$  for  $V_T$ ,  $P = 0.42$  for  $V_S$ ).  $V_{ND}$  was, however, lower in patients than in



**FIGURE 2.** (A and C) Difference in outcome measures ( $V_T$ ,  $V_S$ , and  $V_{ND}$ ) between controls (Ctrl) and subjects with AUD in cerebellum (A) and frontal cortex (C). (B) Zoomed view of results for  $V_{ND}$ .  $P$  values and percentage difference (perc. diff.) between controls and patients are shown. HAB = high-affinity binder; MAB = mixed-affinity binder.



**FIGURE 3.** (A and C) Difference in outcome measures ( $V_T$ ,  $V_S$ , and  $V_{ND}$ ) between controls (Ctrl) and FEP patients in cerebellum (A) and frontal cortex (C). (B) Zoomed view of results for  $V_{ND}$ .  $P$  values and percentage difference (perc. diff.) between controls and patients are shown. HAB = high-affinity binder; MAB = mixed-affinity binder.

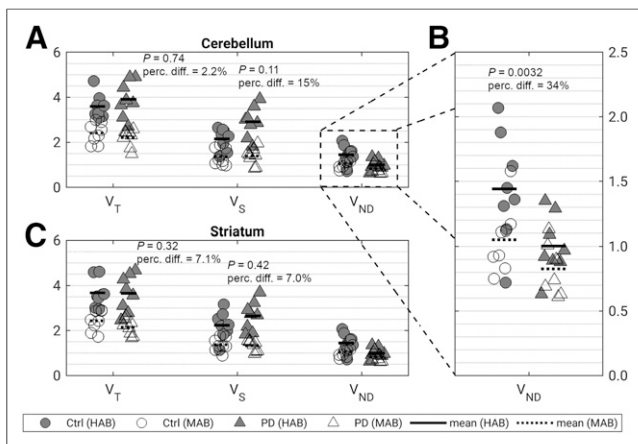
controls (34%,  $P = 0.0032$ ). These results are shown in Figure 4. Across all outcome measures and ROIs, there was a significant effect of genotype ( $P = 0.012$  for  $V_{ND}$ ,  $P < 10^{-6}$  for  $V_T$  and  $V_S$ ).

## DISCUSSION

In this study, we used a new method to estimate  $V_{ND}$  in 4 clinical  $^{11}\text{C}$ -PBR28 datasets. We found that  $V_{ND}$  estimated with this method was lower in AUD and PD than in their matched controls, whereas no difference was found between FEP patients and their controls or in subjects before and after lipopolysaccharide injection. This was, to our knowledge, the first attempt to disentangle the extent by which differences in nondisplaceable binding may contribute to the observed differences in  $V_T$ .

### Lipopolysaccharide

Although leading to a pronounced increase in  $V_T$ , administration of lipopolysaccharide had no apparent effect on SIME  $V_{ND}$ . Lipopolysaccharide is a useful model to study an acute immune



**FIGURE 4.** (A and C) Difference in outcome measures ( $V_T$ ,  $V_S$ , and  $V_{ND}$ ) between controls (Ctrl) and PD patients in cerebellum (A) and striatum (C). (B) Zoomed view of results for  $V_{ND}$ .  $P$  values and percentage difference (perc. diff.) between controls and patients are shown. HAB = high-affinity binder; MAB = mixed-affinity binder.

response, and upregulation of TSPO has been observed in vivo in several species, including mice (13), rats (14), pigs (15), and non-human primates (16). When using  $V_S$  as an outcome measure, we observed a larger percentage separation between the pre- and post-lipopolysaccharide scans, with mean differences of 59% and 66% in the cerebellum and frontal cortex, respectively, and with variability similar to that of  $V_T$  (coefficient of variation [SD/mean] was 0.85 for  $V_T$  and 0.86 for  $V_S$ ). This higher percentage difference occurred because  $V_{ND}$  is not affected by the challenge. In a scenario in which  $V_{ND}$  is unaffected by a particular disease, and  $V_T$  consists of one third of  $V_{ND}$  and two thirds of  $V_S$ , a 50% difference in specific TSPO binding translates to only a 33% difference in  $V_T$ . In such a scenario, though the effect sizes might likely be the same, it follows that changes in  $V_S$  more directly reflect changes in TSPO densities, whereas changes in  $V_T$  are attenuated by the contribution from  $V_{ND}$ .

### AUD

Both  $V_T$  and  $V_{ND}$  were lower in AUD subjects than in their age-matched controls, with a similar trend in  $V_S$ . This finding may explain a previous report in which mixed-affinity binders with AUD had a lower  $^{11}\text{C}$ -PBR28  $V_T$  than mixed-affinity binder controls across several brain regions, whereas no difference was seen in high-affinity binders (17), since  $V_{ND}$  composes a larger fraction of  $V_T$  in mixed-affinity binders than in high-affinity binders. In a separate cohort, Kalk et al. reported a lower  $^{11}\text{C}$ -PBR28 hippocampal  $V_T$  in alcohol-dependent subjects than in controls, across both genotypes (18). In the present analysis, although some of the differences in  $V_T$  between AUD and controls were ascribed to differences in  $V_{ND}$ , frontal cortex  $V_S$  still showed a sizeable (albeit nonsignificant) percentage difference between AUD subjects and their controls. We can only speculate why  $V_{ND}$  would be lower in AUD subjects; pharmacologic competition studies in this population would be needed to conclusively establish levels of specific and nondisplaceable radiotracer uptake. Chronic alcohol exposure induces brain tissue atrophy, reduces cerebral perfusion, and accelerates aging (19,20). Including gray matter volume as a covariate in the statistical analysis did not change the results, indicating that the findings are not driven by partial-volume effects (Supplemental Table 12). Age-related alterations in tissue composition have been proposed as an explanation for differences in  $V_{ND}$  observed with the 5-hydroxytryptamine receptor 2A ligand  $^{18}\text{F}$ -altanserin (21). Although these questions remain unanswered, the findings here reported illustrate how separation of  $V_{ND}$  and  $V_S$  could change the interpretation of results from TSPO PET studies.

### FEP

Patients with FEP had SIME  $V_{ND}$  estimates similar to those of their matched controls. Frontal cortex  $V_T$  and  $V_S$  values were lower in patients. Using  $V_S$  as an outcome measure resulted in a larger percentage difference between the groups. Most previous TSPO PET studies of FEP and schizophrenia have found no significant differences in  $V_T$  (22–24), whereas a recent metaanalysis, which pooled PET data from 5 studies on psychosis and schizophrenia using second-generation TSPO radioligands (152 subjects in total), found strong evidence for lower  $V_T$  values in patients than in controls (25). If  $V_S$  had been used as the outcome measure in previous TSPO PET studies of FEP and schizophrenia, it is possible that the power to detect the population effect of a lower TSPO also in the individual samples of patients would have been higher.

## PD

We found that SIME  $V_{ND}$  was lower in PD patients than in controls, but we observed no significant differences in  $V_T$ , consistent with findings in TSPO PET studies using another second-generation radioligand (26,27). One study, using  $^{11}\text{C}$ -PK11195 and a basis-function implementation of the simplified reference tissue model, found a higher  $BP_{ND}$  in PD patients than in controls (28). Since  $BP_{ND}$  is defined as  $V_S/V_{ND}$ , and given our findings, it is possible that the higher  $BP_{ND}$  reported in the  $^{11}\text{C}$ -PK11195 study was due to lower nondisplaceable binding rather than higher specific binding. This possibility illustrates that  $V_{ND}$  is a potential confounding factor not only in studies using  $V_T$  as an outcome measure but also in those reporting  $BP_{ND}$ . By using ratio-based methods to provide  $BP_{ND}$  in TSPO PET studies, one may mistakenly interpret a decrease in  $V_{ND}$  as an increase in TSPO binding. Similar to the finding in the AUD dataset, PD might be associated with increased global atrophy (29), and it is possible that altered tissue composition could explain the lower  $V_{ND}$  in PD patients. Further studies are required to establish the reason for this observed group difference.

### Effect of $V_{ND}$ on Genotype

We observed a pronounced effect of genotype on SIME  $V_{ND}$  in both the FEP and the PD datasets but not in the AUD data. The observed effect, if true, complicates interpretation of our current understanding of the TSPO polymorphism, by implicating effects both on the tracer's affinity to TSPO and on nondisplaceable uptake. When all the controls in this study were pooled, a difference in  $V_{ND}$  between genotypes was quite evident ( $P = 0.00016$ ). We identify 3 potential interpretations for this observation. One possibility is that SIME-derived estimates of  $V_{ND}$  are artefactually contaminated by estimates of  $V_S$ , so that high specific binding results in an overestimation of  $V_{ND}$ . However, this spillover across compartments has previously been tested and discarded using simulations (7). This finding is also supported by the lipopolysaccharide experiment, in which increased  $V_S$  is not reflected in  $V_{ND}$ . A second interpretation is that the higher affinity of the radioligand in high-affinity binders leads to a higher nondisplaceable binding because equilibrium conditions are achieved at a later time for a high-affinity versus a low-affinity radioligand. The same mechanisms could potentially lead to higher nondisplaceable tracer binding in high-target-density brain regions than in regions with low target densities. For  $^{11}\text{C}$ -raclopride, it has been suggested that regional differences in observed occupancy could in fact be attributable to spatially varying nondisplaceable uptake (30,31). The third possibility is that SIME-derived  $V_{ND}$  estimates are affected by other features, which are, in turn, dependent on the genotype. For instance, it has previously been shown that  $V_{ND}$  estimated with SIME may be sensitive to the shapes of the arterial input function (32). The fact that input functions may differ between genotypes has been shown for both  $^{11}\text{C}$ -PBR28 (7) and the TSPO SPECT radioligand  $^{123}\text{I}$ -CLINDE (33), as is to be expected from the different levels of binding to TSPO in peripheral tissue (34). Irrespective of cause, estimates of  $V_{ND}$  (and, as a consequence, of  $BP_{ND}$ ) may not be directly comparable across genotype groups, and their difference could itself be a confounder in clinical studies if the cohort is not balanced across genotypes. The datasets included in this study, however, are well balanced across genotypes; as such, a potential influence of differences in  $V_{ND}$  estimates is unlikely. Pharmacologic competition data would be needed to conclusively establish any effect of genotype on  $V_{ND}$ .

However, previous  $^{11}\text{C}$ -PBR28 blocking studies have included only high-affinity-binder individuals (35) and therefore cannot provide insights into potential differences between genotypes.

### Limitations

For any arterial input model, including SIME,  $V_{ND}$  estimates are sensitive to the input function shape. Further, similar to reference-tissue modeling, we did not consider spatial variations in  $V_{ND}$ . SIME was additionally executed on a larger set of ROIs, which resulted in close-to-identical findings (Supplemental Table 13). Yet, a formal procedure on how to establish a suitable ROI set for estimation of  $V_{ND}$  remains to be investigated.

### CONCLUSION

Our findings suggest that  $V_{ND}$  may be a potential confounding factor in  $^{11}\text{C}$ -PBR28 PET studies. This outcome warrants further studies to establish the observed  $V_{ND}$  differences and, if possible, reveal their causes. We recommend the use of  $V_S$  as an additional outcome parameter in TSPO PET studies since this measure more directly reflects binding to TSPO.

### DISCLOSURE

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### KEY POINTS

**QUESTION:** Is nondisplaceable binding a confounding factor in  $^{11}\text{C}$ -PBR28 PET studies?

**PERTINENT FINDINGS:** Nondisplaceable uptake was estimated for 4  $^{11}\text{C}$ -PBR28 PET datasets. In 2 of these (AUD and PD) there was a significant difference in nondisplaceable uptake between patients and controls.

**IMPLICATIONS FOR PATIENT CARE:** The possibility of obtaining estimates of specific binding to TSPO may improve the interpretability of nuclear imaging studies addressing the role of neuroinflammation in several disorders.

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