# Comparison of the RGD Motif-Containing $\alpha_v \beta_6$ Integrin-Binding Peptides SFLAP3 and SFITGv6 for Diagnostic **Application in HNSCC**

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 $\alpha_{\nu}\beta_{6}$  integrin is overexpressed by several carcinomas and thus considered a target for diagnostic imaging and anticancer therapies. Recently, we presented the  $\alpha_v \beta_6$  integrin-binding peptide SFITGv6 as a novel potential tracer for imaging and targeted therapy of  $\alpha_{\nu}\beta_{6}$ integrin-positive carcinomas. Here, we analyzed the affinity and specificity of 5 native  $\alpha_v \beta_6$  integrin-specific binders in comparison to SFITGv6. Methods: Sunflower trypsin inhibitor 1 (SFTI1)-based peptides containing arginine-glycine-aspartic acid (RGD) motifspanning octamers of fibronectin (SFFN1), tenascin C (SFTNC), vitronectin (SFVTN), and latency-associated peptides (LAP) 1 (SFLAP1) and 3 (SFLAP3) were synthesized, and their binding potential to ανβ<sub>6</sub> integrin-expressing head and neck squamous cell carcinoma (HNSCC) cell lines was evaluated. Subsequently, stability, affinity, and specificity were assessed in vitro using radio-high-pressure liquid chromatography, surface plasmon resonance assay, and binding experiments including competition, kinetics, internalization, and efflux.  $\alpha_v \beta_0$  integrin binding specificity was further evaluated by peptide histochemistry. Finally, in vivo binding properties were assessed using small-animal PET imaging and biodistribution experiments in HNSCC-bearing mice, and <sup>68</sup>Ga-DOTA-SFLAP3 was applied for diagnostic PET/CT of an HNSCC patient. Results: When the newly designed peptides were compared, significant binding (>20%) to several HNSCC cell lines (HNO97, HNO399, and HNO223) and a fast internalization of up to 60% and 70% were observed for SFLAP3 (GRGDLGRL) and SFITGv6 (FRGDLMQL). In contrast, the other peptides displayed binding that was moderate (SFLAP1, 4.1%-12.1%) to marginal (SFFN1, SFTNC, and SFVTN, <1%) and were therefore excluded from further analysis. Notably, SFLAP3 exhibited improved affinity for  $\alpha_v \beta_6$  integrin (mean half-maximal inhibitory concentration, 3.5 nM; dissociation constant, 7.4). Moreover, small-animal PET imaging and biodistribution studies of HNSCC xenograft mice revealed an increased tumor-specific accumulation 30-60 min after injection of <sup>68</sup>Ga-labeled or <sup>177</sup>Lu-labeled DOTA-SFLAP3. Peptide staining further demonstrated binding specificity for SFLAP3 to HNSCC tumor cells. Finally, PET/CT scanning of an HNSCC patient showed specific SFLAP3 accumulation in the primary tumor lesion (SUV<sub>max</sub>,

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5.1) and in corresponding lymph node metastases (SUV<sub>max</sub>, 4.1). Conclusion: SFLAP3 represents a promising tracer for prognostic assessment, diagnostic imaging, and possibly targeted therapy of  $\alpha_{\nu}\beta_{6}$  integrin–expressing tumors.

**Key Words:**  $\alpha_v \beta_6$ ; integrin; novel peptide; head and neck squamous cell carcinoma; PET

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Integrins comprise a large family of cellular adhesion receptors that play an important role in development, immune response, and cancer (1-3). Unlike most epithelial integrins,  $\alpha_v \beta_6$  integrin is upregulated in many carcinomas associated with a poor prognosis, including lung, ovarian, pancreatic, colorectal, and cervical (4–8). In contrast, healthy tissues show no or a rather low  $\alpha_{\nu}\beta_{6}$  integrin expression (9). Therefore,  $\alpha_{\nu}\beta_{6}$  integrin is considered a prognostic biomarker and an important target for imaging and anticancer therapies (10,11). Using a sunflower trypsin inhibitor 1 (SFTI1)-based phage display library for biopanning against head and neck squamous cell carcinoma (HNSCC) cells and fractionated high-pressure liquid chromatography-derived membrane proteins, we identified the novel  $\alpha_v \beta_6$  integrin–specific peptide SFITGv6 (12). Because of the molecular scaffold of SFTI1, a 14-residue cyclic miniprotein isolated from sunflower seeds that is stabilized by a single disulfide bridge, the peptide exhibits excellent stability (13). SFITGv6 demonstrates high binding affinity to several  $\alpha_v \beta_6$  integrin–positive tumor cells and to HNSCC xenografts. Moreover, it accumulates in tumor lesions of HNSCC and non-small cell lung carcinoma but not in inflammatory lesions of cancer patients (12).

 $\alpha_{\nu}\beta_{6}$  integrin binds the tripeptide recognition sequence arginineglycine-aspartic acid (RGD) of several extracellular matrix proteins, including fibronectin, vitronectin, tenascin C, and latency-associated peptides (LAP) 1 and 3, which participate in carcinogenesis by promoting cell migration and invasion of cancer cells (14,15). Particularly,  $\alpha_v \beta_6$  integrin–mediated transforming growth factor  $\beta$  (TGF- $\beta$ ) activation plays an important role in epithelial-to-mesenchymal transition and thereby promotes tumor growth and metastasis (16). Noncovalently associated with the N terminus of TGF-β1 and TGF-β3,

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LAP prevents TGF- $\beta$  from binding to TGF- $\beta$  receptors. Binding of LAP1 or LAP3 to  $\alpha_v\beta_6$  integrin induces dissociation of the complex followed by TGF- $\beta$  activation (17,18). Considering both the requirement for additional tumor-specific peptides targeting epithelial tumors and the high stability of the SFT11 scaffold (13), we designed further RGD sequence–containing SFT11 derivates (SFT11-based peptides containing RGD motif–spanning octamers of fibronectin [SFFN1], tenascin C [SFTNC], vitronectin [SFVTN], LAP1 [SFLAP1], and LAP3 [SFLAP3]) and compared their  $\alpha_v\beta_6$  integrin–specific binding properties with those of SFITGv6. Thus, we discovered SFLAP3, a peptide that demonstrates high  $\alpha_v\beta_6$  integrin affinity and specificity for several  $\alpha_v\beta_6$  integrin–expressing tumor cells. Moreover, SFLAP3 displays an increased accumulation in HNSCC xenografts and patient tumors.

#### **MATERIALS AND METHODS**

### Cell Lines, Tumor Material, and Ethical Approval

The HNSCC-derived cell lines HNO97, HNO199, HNO210, HNO223, and HNO399 (19) were cultured in RPMI 1640 medium supplemented with 10% fetal calf serum at 37°C and 5% CO<sub>2</sub> and were negative for *Mycoplasma* contamination. Uniqueness was assessed by the German Collection of Microorganisms and Cell Culture. Patient-derived tumor tissues obtained intraoperatively were snap-frozen and stored at  $-80^{\circ}$ C. Written informed consent was obtained from all patients according to the research proposals approved by the Institutional Review Board at the Medical Faculty of the University of Heidelberg.

### In Vitro Binding Experiments

For assessment of peptide binding capacity in vitro,  $2.5-4 \times 10^5$  cells were seeded into 6-well plates and cultivated for 48 h. The cells were exposed to 125I-labeled peptides resuspended in 1 mL of serum-free medium for 10 or 60 min either with or without different concentrations of unlabeled peptide (10<sup>-5</sup>–10<sup>-10</sup> M). Unbound peptide was washed off (3 washes with phosphate-buffered saline), and finally, cells were harvested using 0.3 M NaOH. To evaluate kinetic properties, the cells were exposed to 177 Lu-DOTA-labeled peptides for 10, 30, 60, 120, 360, and 480 min, respectively, and harvested using 0.3 M NaOH. Efflux was assessed by incubating the cells with 177Lu-DOTA-labeled peptides for 60 min. Next, radioactive peptide-containing medium was replaced, and the cells were incubated for another 10, 30, 60, 120, and 240 min and finally harvested using 0.3 M NaOH. To assess peptide internalization, the cells were exposed to <sup>177</sup>Lu-DOTA-labeled peptides for 10, 30, 60, 120, and 240 min at 37°C. Surface-bound peptides were removed by 10 min of incubation with 1 M glycine-HCl solution (pH 2.2). The cells were rinsed with phosphate-buffered saline and lysed as described. Radioactivity (MBq) was determined using a y-counter (LB951G; Berthold Technologies) and calculated as percentage of applied injected dose (%AD) per 10<sup>6</sup> cells.

# **Surface Plasmon Resonance Assay**

Binding affinity was assessed via a BiaCore X100 system (GE Healthcare) as described in detail previously (12). Briefly, to prevent integrin heterodimer denaturation during immobilization,  $\alpha_{\nu}\beta_{6}$  integrin (1, 2, 3, and 4  $\mu$ g/mL) and  $\alpha_{\nu}\beta_{3}$  integrin (15, 30, 35, and 40  $\mu$ g/mL) were used as analytes. SFLAP3 was dissolved in HBS-EP (HEPES-buffered saline, containing EDTA and Surfactant P20) running buffer and immobilized (loading level, 12 response units) on the C1 sensor chip (both GE Healthcare) using a manual amine-coupling protocol. Next, the binding affinity of  $\alpha_{\nu}\beta_{6}$  and  $\alpha_{\nu}\beta_{3}$  integrin, dissolved in HBS-EP running buffer (1–50  $\mu$ g/mL), to SFLAP3 was measured (flow rate, 30  $\mu$ L/min). The dissociation constant ( $K_{D}$ ) was determined by a 1:1 Langmuir model fit of the surface plasmon resonance sensograms.

#### **Animal Experiments**

Animal experiments were conducted in compliance with the German animal protection laws. For in vivo small-animal PET imaging and organ distribution studies, 8-wk-old BALB/c nude mice (Charles River Laboratories) were inoculated subcutaneously at the right shoulder with  $5\times 10^6$  tumor cells in Matrigel (BD Bioscience).

Xenografts were grown to a 10- to 15-mm diameter. The mice were anesthetized using isoflurane inhalation, and a 100-μL phosphate-buffered saline solution containing  $^{68}\text{Ga-DOTA-SFLAP3}$  (HNO97, 37.9 MBq; HNO399, 26 MBq; HNO223, 27 MBq) or  $^{68}\text{Ga-DOTA-SFITGv6}$  (HNO97, 30 MBq; HNO399, 34 MBq; HNO223, 34 MBq) was injected into the tail vein. Three-dimensional PET images were captured (Siemens Inveon PET scanner) as previously described (*12*). To assess the biodistribution, 100 μL of a 20 nM  $^{177}\text{Lu-DOTA-SFLAP3}$  or  $^{177}\text{Lu-DOTA-SFITGv6}$  solution (1 MBq) were administered as a bolus injection into the tail vein. At each time point (30, 60, 120, 240, 360 min), we sacrificed 3 animals, collected peripheral blood and the respective organs, weighed the tissues, and measured the radioactivity using a γ-counter. Radioactivity (MBq) was expressed as percentage of injected dose (%ID) per gram of tissue.

#### **Peptide Staining**

Histochemical staining was performed using biotinylated polyethylene glycol 12–labeled peptides on acetone-fixed cryosections (5  $\mu$ m) derived from snap-frozen HNSCC tissues as described previously (12). Briefly, to prevent background staining, HNSCC cryosections were preincubated with an SP-2001 avidin/biotin blocking kit (Vector Laboratories), and  $10^{-5}$  M peptide diluted in Dako Antibody Diluent (Agilent) was subsequently applied at 4°C overnight. Detection of bound peptide was assessed using the Vectastain Elite ABC Kit (PK-6100; Vector Laboratories) according to the manufacturer's instructions. Peptide-binding specificity was ensured by using a peptide containing a scrambled (GRD) sequence and by incubation without peptide. Because of the instability of the peptide binding, staining was assessed on the same day as the binding experiment.

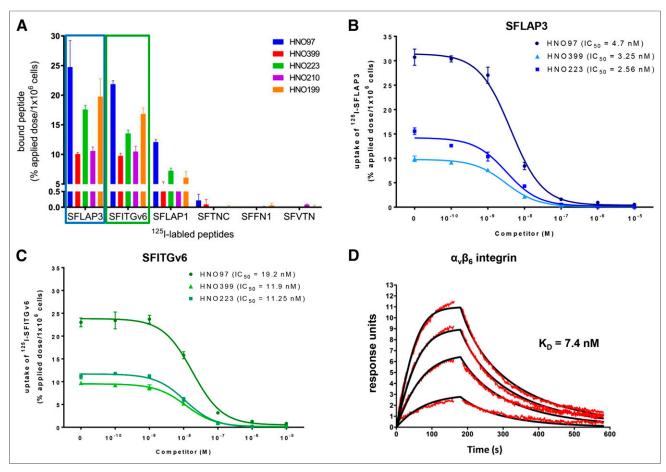
# PET/CT Scanning of HNSCC Tumor Patient

An unenhanced PET/CT scan of a patient was obtained 60 and 180 min after intravenous injection of the <sup>68</sup>Ga-DOTA-labeled peptide using a Biograph mCt Flow PET/CT scanner (Siemens Medical Solution) and the following parameters: slice thickness of 5 mm, increment of 3–4 mm, soft-tissue reconstruction kernel, and CARE Dose4D (Siemens). Immediately after CT scanning, a whole-body PET scan was acquired in 3 dimensions (matrix, 200 × 200) using FlowMotion continuous-bed-motion technology (Siemens) at 0.7 cm/min. The emission data were corrected for randoms, scatter, and decay. Images were reconstructed using ordered-subsets expectation maximization with 2 iterations and 21 subsets and were Gauss-filtered to a transaxial resolution of 5 mm in full width at half maximum. Attenuation correction was performed using the low-dose unenhanced CT data. Uptake was quantitatively assessed using a region-of-interest technique and SUVs.

#### RESULTS

# Binding of SFTI1 Derivates to $\alpha_{\nu}\beta_{6}$ Integrin–Expressing HNSCC Cell Lines

RGD motif–containing octamers of the natural  $\alpha_v\beta_6$  integrin ligands fibronectin, tenascin C, vitronectin, LAP1, and LAP3 (Supplemental Table 1; supplemental materials are available at http://jnm.snmjournals.org) were grafted between Thr4 and Cys11 into the binding loop of the SFTI1 scaffold. First, the binding properties of  $^{125}$ I-labeled SFFN1, SFTNC, SFVTN, SFLAP1 SFLAP3, and SFITGv6 were compared using 5 HNSCC cell lines differing in their  $\alpha_v\beta_6$  integrin expression as assessed by flow cytometry



**FIGURE 1.** (A) Binding of  $^{125}$ I-labeled SFLAP3, SFITGv6, SFLAP1, SFTNC, SFFN1, and SFVTN to different HNSCC cells after exposure to peptides for 60 min. Bars represent %AD/10<sup>6</sup> cells (HNO97, HNO399, HNO223, HNO210, and HNO199). Increasing concentrations ( $^{10-5}$ - $^{10-10}$  M) of respective unlabeled peptide were used to compete for binding of  $^{125}$ I-labeled SFLAP (B) and SFITGv6 (C) to HNSCC cell lines HNO97, HNO399, and HNO223 (%AD/10<sup>6</sup> cells). Data are mean and SD of triplicate measurements from representative experiment. (D) Affinity of  $\alpha_v \beta_6$  integrin (applied concentrations: 1, 2, 3, and 4 μg/mL) for immobilized SFLAP3 (loading level: 12 response units) was measured by surface plasmon resonance assay (n = 3) with flow rate of 30 mL/min. Surface plasmon resonance sensograms were evaluated with BiaCore evaluation software (black curves) and correspond to experimentally fitted red curves.  $K_D$  was determined by 1:1 Langmuir model fit of surface plasmon resonance sensograms.  $IC_{50} = half$ -maximal inhibitory concentration.

(Supplemental Fig. 1). As shown in Figure 1A, <sup>125</sup>I-SFLAP3 displayed the highest binding capacity to all tested HNSCC cell lines (HNO97, 24.7%; HNO399, 10.1%; HNO199, 19.7%; HNO223, 17.6%; HNO210, 10.6%)—higher even than that of <sup>125</sup>I-SFITGv6 (HNO97, 21.8%; HNO399, 9.8%; HNO199, 16.8%; HNO223, 13.5%; HNO210, 10.5%). In contrast, only a moderate binding capacity was detected for SFLAP1 (4.1%–12.1%) and almost none (<1%) for SFFN1, SFTNC, and SFVTN (Fig. 1A). In summary, SFLAP3 and SFITGv6 demonstrated the highest binding capacity and, thus, were further investigated comparatively.

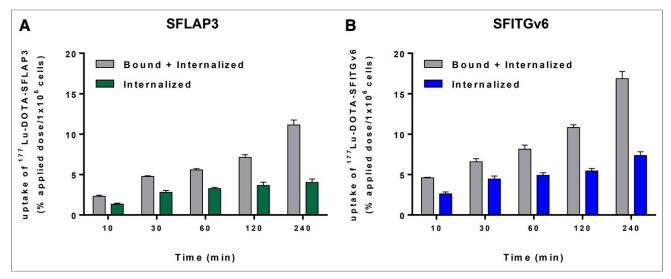
# SFLAP3 Affinity for $\alpha_v \beta_6$ Integrin and Serum Stability

To assess the specificity of the peptide, binding competition experiments were performed. In all HNSCC cell lines, binding of  $^{125}\text{I-SFLAP3}$  and  $^{125}\text{I-SFITGv6}$  could almost be completely inhibited by adding  $10^{-6}$  M unlabeled counterparts as competitor (Figs. 1B and 1C). However, SFLAP3 exhibited higher affinity than SFITGv6 (mean half-maximal inhibitory concentrations, 3.5 and 14.11 nM, respectively). Concordantly, the surface plasmon resonance assay revealed that SFLAP3 had a higher affinity than SFITGv6 for  $\alpha_{\rm v}\beta_{\rm 6}$  integrin ( $K_{\rm D}=7.4$  and 14.8 nM, respectively) (Fig. 1D) (12). In

contrast, SFLAP3 had a 10-fold lower affinity to  $\alpha_v \beta_3$  integrin ( $K_D = 167$  nM) (Supplemental Fig. 2A), further ensuring the  $\alpha_v \beta_6$  integrin specificity of SFLAP3. Additionally, SFLAP3 showed high proteolytic stability, with no degradation over 24 h (Supplemental Fig. 2B), demonstrating suitability for in vivo applications.

# Comparative Evaluation of Kinetics, Internalization, and Efflux

Considering time-dependent deionization of <sup>125</sup>I, the determination of kinetics, internalization, and efflux was performed using <sup>177</sup>Lu-DOTA-labeled peptides. Kinetic experiments revealed a continuous increase in peptide uptake over the whole period of measurement for both peptides. Yet, <sup>177</sup>Lu-DOTA-SFLAP3 exhibited a lower maximum binding capacity (HNO97, 18.5%; HNO223, 9.66%; HNO399, 4.31%) (Supplemental Fig. 3A) than <sup>177</sup>Lu-DOTA-SFITGv6 (HNO97, 22.15%; HNO223, 14.45%; HNO399, 5.85%) (Supplemental Fig. 3B). Accordingly, within 60 min after exposure to HNO97, we measured an increase in <sup>177</sup>Lu-DOTA-SFITGv6 binding of up to 16.85% and a fast internalization of up to 70% of the total bound peptide (Fig. 2B), but up to 11.14% binding and 60% internalization of <sup>177</sup>Lu-DOTA-SFLAP3



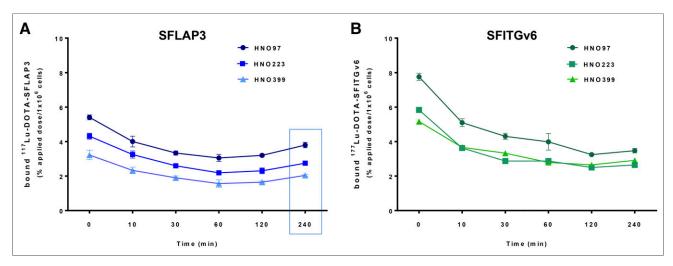
**FIGURE 2.** Uptake (gray bars) and internalization of <sup>177</sup>Lu-DOTA-labeled SFLAP3 (A) and SFITGv6 (B) in HNO97 cells. After incubation for 10, 30, 60, 120, and 240 min, radioactivity in lysates was determined and calculated as %AD/10<sup>6</sup> cells. Data are mean and SD of triplicate measurements from representative experiment.

(Fig. 2A). For both peptides, similar trends regarding a time-dependent increase in peptide binding and internalization were observed after exposure to HNO399 (Supplemental Figs. 4A and 4B) and HNO223 (Supplemental Figs. 4C and 4D), although the amount of internalized peptide slightly decreased (>45%). Concordantly, an efflux of more than 50% of the originally accumulated SFLAP3 and SFITGv6 within 120 min after termination of the uptake was measured (Figs. 3A and 3B). Notably, for <sup>177</sup>Lu-DOTA-SFLAP3, we observed a moderate renewed increase in binding and internalization after 240 min (Fig. 3A), possibly indicating peptide reuptake from the culture medium.

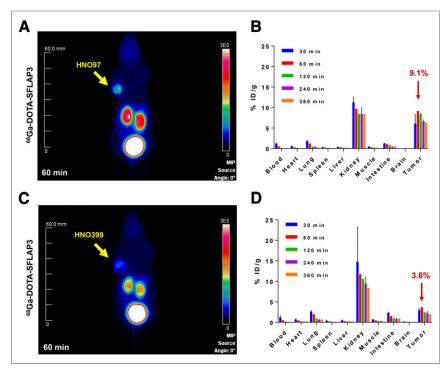
### In Vivo Targeting Properties of SFLAP3 and SFITGv6

To compare the in vivo targeting properties of the peptides, small-animal PET imaging of HNO97, HNO399, and HNO223 xenografts was performed using <sup>68</sup>Ga-DOTA-labeled SFLAP3 and SFITGv6 as radiotracer. In HNO97 tumor lesions, a fast and continuous

accumulation of <sup>68</sup>Ga-DOTA-SFLAP3 (SUV<sub>mean</sub>, 0.63) (Fig. 4A; Supplemental Fig. 5A) and <sup>68</sup>Ga-DOTA-SFITGv6 (SUV<sub>mean</sub>, 0.68) (Supplemental Figs. 5B and 5C) was measured within 60 min after injection and stayed for at least 140 min (Supplemental Figs. 5D and 5E). Nonspecific peptide activity cleared quickly from the blood, resulting in images with excellent tumor-to-background ratios. Accordingly, the biodistribution of <sup>177</sup>Lu-DOTA-SFLAP3 in tumor lesions and individual organs of HNO97 xenografts revealed maximal peptide accumulation in the tumors after 60 min (9.1  $\pm$ 1.2 %ID/g), followed by a decrease to 5.80  $\pm$  1.44 %ID/g at 360 min after injection (Fig. 4B). In contrast, the maximal uptake of  $^{177}$ Lu-DOTA-SFITGv6 in HNO97 tumors (6.73  $\pm$  1.00 %ID/g) was already present at 30 min after injection, and uptake decreased to  $2.43 \pm 0.51$  %ID/g after 360 min (Supplemental Fig. 5F). Smallanimal PET imaging of HNO399 (Fig. 4C; Supplemental Fig. 6B) and HNO223 xenografts (Supplemental Figs. 7A and 7B) revealed less accumulation of <sup>68</sup>Ga-DOTA-SFLAP3 (SUV<sub>mean</sub>, 0.44 for



**FIGURE 3.** Time-dependent efflux of SFLAP3 (A) and SFITGv6 (B) from HNSCC cell lines. HNO97, HNO399, and HNO223 cells were exposed to <sup>177</sup>Lu-DOTA-labeled peptides for 60 min. After replacement of culture medium, radioactivity in cell lysates was measured immediately and after 10, 30, 60, 120, and 240 min and calculated as %AD/10<sup>6</sup> cells. Data are mean and SD of triplicate measurements from representative experiment.



**FIGURE 4.** Small-animal PET imaging of mice bearing HNO97 (A) and HNO399 (C) xenografts 60 min after injection of <sup>68</sup>Ga-DOTA-SFLAP3. Biodistribution of <sup>177</sup>LU-DOTA-SFLAP3 in tumor and organs of HNO97 (B) and HNO399 (D) tumor-bearing mice was measured 30, 60, 120, 240, and 360 min after injection and calculated as %ID/g. Data are mean of 3 per time point and SD. MIP = maximum-intensity projection.

HNO399 and 0.32 for HNO223) (Supplemental Figs. 6A and 7C) and of <sup>68</sup>Ga-DOTA-SFITGv6 (SUV<sub>mean</sub>, 0.33 for HNO399 and 0.23 for HNO223) (Supplemental Figs. 6C and 7D). Accordingly, we measured a maximal <sup>177</sup>Lu-DOTA-SFLAP3 accumulation of 3.6 % ID/g (Fig. 4D) and 3.4 %ID/g (Supplemental Fig. 7E) in HNO399 and HNO233 xenografts, respectively, at 60 min after injection, followed by a decrease to almost 2% at 360 min. Less than 1 %ID/g was detected in the blood and most tissues of xenograft mice 120 min after injection of either peptide, accounting for tumor-to-tissue ratios predominantly above 1 (Supplemental Tables 2A–2D). However, in the kidneys we observed a constant high SFLAP3 retention (8–14 % ID/g), which was indeed clearly reduced in comparison to SFITGv6 (Supplemental Fig. 5F).

# In Situ Binding Properties of SFLAP3

In analogy to the previous experiments (12), we compared the binding specificity of the peptides to sections of HNO97 xenografts and patient-derived HNO399 and HNO210 tumors by peptide histochemical staining using biotin-labeled SFLAP3 and SFITGv6. Although SFLAP3 showed a slightly fainter staining, both peptides revealed tumor cell–specific binding, whereas lower peptide binding was observed at the stromal compartments (Fig. 5). In contrast, no binding of the GRD sequence containing peptide was observed, further corroborating the specificity of the SFLAP3 peptide.

# SFLAP3 Accumulation in HNSCC Lesions and Lymph Node Metastases

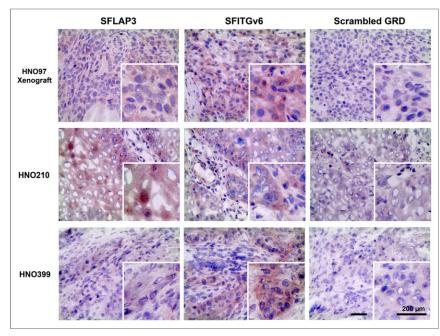
Finally, we investigated the therapeutic or diagnostic suitability of SFLAP3, using the example of a 79-y-old male carcinoma patient who presented with lymph node swelling in the right cervical area,

assuming the diagnosis cancer of unknown primary. To clarify the diagnosis, 322 MBq of <sup>68</sup>Ga-DOTA-labeled SFLAP3 were administered and PET/CT performed. After 60 min, we observed a tumor-specific accumulation of SFLAP3 at the primary tumor lesion (right site of aryepiglottic folds; median  $SUV_{max}$ , 5.1) (Fig. 6) and at the right cervical area (SUV<sub>max</sub>, 4.1) (Supplemental Table 3). The histopathologic examination of the surgically resected respective tissues proved the presence of level II/III squamous cell carcinoma and corresponding lymph node metastases at the respective locations. The correlation of PET findings and histopathologic findings revealed the primary tumor lesion to be subepithelial connective tissue infiltrated by moderately differentiated squamous cell carcinoma (Fig. 6C). The tumor lesion at the right cervical area was classified as cyst wall and content; histopathologic analysis showed infiltrates of an epithelial neoplasia with a solid growth pattern (Fig. 6B). Moderate tracer accumulation was also seen in a lymph node in the right cervical area (SUV<sub>max</sub>, 2.2), which was histopathologically classified as a lymph node infiltrated by epithelial tumor cells and neoplasia with a solid growth pattern (Fig. 6D).

## **DISCUSSION**

SFTI1 has already been proven to be a suitable scaffold for the development of extremely stable peptides targeting tumor-associated receptors, including the  $\alpha_{\nu}\beta_{6}$  integrin–specific peptide SFITGv6 (12,20).  $\alpha_{\nu}\beta_{6}$  integrin has been shown to be expressed in up to 99.9% of HNSCC (9,14), as well as in lung (4), colon (7), breast (21), and pancreas carcinoma (6), and is often associated with a poor prognosis (9). Thus,  $\alpha_{\nu}\beta_{6}$  integrin represents an important target for imaging and therapy for a variety of epithelial malignancies (22–25). To design novel target-specific peptides, we introduced the RGD-containing octamer of natural  $\alpha_{\nu}\beta_{6}$  integrin ligands resembling the RGDLXXL sequence into the SFTI1 scaffold and compared the specificity and affinity of the novel peptides with that of SFITGv6.

In comparing the binding properties of these SFTI1 derivates, we identified the superiority of the  $\alpha_{\rm v}\beta_6$  integrin–specific peptide SFLAP3, containing the amino acid sequence GRGDLGRL. Comparative analysis of SFLAP3 and SFITGv6 revealed improved binding (>20%) of the novel peptide to several HNSCC cell lines corresponding to their  $\alpha_{\rm v}\beta_6$  integrin expression profile. Considering the importance of the RGDLXXL motif—in particular, the DLXXL sequence—for  $\alpha_{\rm v}\beta_6$  integrin binding affinity and specificity (26–28), it is not surprising that SFLAP3 provides significant binding properties. In contrast, for SFLAP1, SFFN1, SFVTN, and SFTNC—partially or completely lacking the LXXL motif—we observed less or even almost no binding. Although being physiologically involved in  $\alpha_{\rm v}\beta_6$  integrindependent promotion of migration, invasion, and signal transduction pathways (14), the RGD motif–containing sequences of



**FIGURE 5.** Histochemical peptide staining of HNSCC cyrosections of HNO97 xenografts and of patient-derived HNO399 and HNO210 tumor sections performed with  $10^{-5}$  M biotinylated polyethylene glycol 12–labeled SFLAP3 and SFITGv6. As control, scrambled SFLAP3 derivate containing GRD was applied. Scale bar =  $50 \ \mu m$ .

LAP1, fibronectin, vitronectin, and tenascin C incorporated into the SFTI1 scaffold might not allow for  $\alpha_v\beta_6$  integrin affinity and specificity in vitro.

A.
B. C.
D.
Histology:
Cyst wall and content with infiltrates of an epithelial neoplasia with solid growth pattern

C.
Histology:
Connective tissue with infiltrates of a moderately differentiated squamous cell carcinoma with infiltration of the subepithelial connective tissue (right lateral aryepiglottic fold).

D.
Lymph node infiltrated by epithelial tumor cells. Neoplasia with solid growth pattern.

**FIGURE 6.** Transaxial PET/CT scans of HNSCC tumor patient after application of 322 MBq of <sup>68</sup>Ga-DOTA-SFLAP3, with arrowheads indicating peptide accumulation. (A) Level showing unspecific binding. (B) Level showing cyst wall and content. (C) Level showing primary tumor. (D) Level showing lymph node infiltration.

As expected from stability analysis of the naturally occurring SFTI1 (13) and the SFTI1 derivates DLL4 (20) and SFITGv6 (12), SFLAP3 also demonstrated marked stability in human serum over 24 h. Additionally, an improved affinity of SFLAP3  $(K_D = 7.4 \text{ nM}) \text{ for } \alpha_v \beta_6 \text{ integrin when}$ compared with SFITGv6 was measured. Subsequent investigation of 177Lu-DOTAlabeled SFLAP3 and SFITGv6 regarding kinetics, internalization, and efflux revealed a continuous increase in SFLAP3 binding (≤18.5% within 240 min) and fast internalization (>60%) followed by a decrease (<50%). Correspondingly, we observed greater than 50% efflux and almost 50% retention of the originally accumulated peptide over 120 min, justifying further in vivo evaluation. These experiments also demonstrated a consistently higher binding (≤5.7%) of <sup>177</sup>Lu-DOTAlabeled SFITGv6 than of SFLAP3. It is thought that the chemical properties of the SFLAP3 and SFITGv6 amino acid composition influence the binding capacity of DOTA-labeled peptides differently.

On the basis of the excellent tumor-tobackground ratios, we were able to selectively image HNSCC xenografts using

small-animal PET at 60–140 min after the administration of <sup>68</sup>Ga-DOTA-labeled SFLAP3 and SFITGv6. Unbound and non-specifically bound peptide rapidly cleared from the blood and the

surrounding tissues, except for the kidneys. As expected from the  $\alpha_v \beta_6$  integrin expression profile of HNSCC cell lines, we detected a rather low but clearly visible accumulation of both <sup>68</sup>Ga-DOTA-SFLAP3 (SUV<sub>mean</sub>, 0.63) and <sup>68</sup>Ga-DOTA-SFITGv6 (SUV<sub>mean</sub>, 0.68) in HNO97 xenografts. In contrast, HNO399 and HNO223 xenografts showed a lower uptake of the 68Ga-DOTAlabeled peptides but a generally higher affinity of <sup>68</sup>Ga-DOTA-SFLAP3 (SUV<sub>mean</sub>, 0.44; SUV, 0.32) than did 68Ga-DOTA-SFITGv6 (SUV<sub>mean</sub>, 0.32; SUV<sub>mean</sub>, 0.23). The biodistribution of <sup>177</sup>Lu-DOTA-labeled peptides in HNSCC xenograft mice confirmed the improved affinity of SFLAP3 for  $\alpha_v \beta_6$  integrin-expressing tumors. In HNO97 tumors, we found a marked accumulation of SFLAP3 (≤9.10 %ID/g) and SFITGv6 (6.73 %ID/g), compared with that in healthy tissues, even after 240 and 360 min. In contrast, less than 4 %ID/g of SFLAP3 was measured for HNO399 and HNO223, emphasizing the importance of pronounced target expression for selective in vivo tumor imaging and targeting. As expected from a previous biodistribution analysis of  $\alpha_v \beta_6$  integrin binding peptides in HNO97 (12) and BxPC-3 xenografts (11), a remarkable but slightly decreasing

accumulation of <sup>177</sup>Lu-DOTA-SFLAP3 was noticed in the kidneys of HNSCC xenografts. Although the renal retention of SFLAP3 was clearly lower than that of SFITGv6, we can recommend that the pharmacokinetic properties of the peptide be improved.

Even though peptide-based histochemical staining revealed a moderate but tumor cell–specific binding of SFLAP3 to HNO97 xenografts and patient-derived HNSCC tumor cyrosections, the  $^{68}\text{Ga-DOTA-labeled}$  peptide was successfully used as a radiotracer for PET/CT imaging of a patient with a carcinoma of unknown primary, leading to the discovery of a histologically proven HNSCC and a corresponding lymph node metastasis. In line with the small-animal PET imaging results for HNSCC xenografts, the SUVs in the patient persisted from 60 min (SUV $_{\rm max}$ , 5.1) to 180 min (SUV $_{\rm max}$ , 4.6) after injection, demonstrating the diagnostic suitability of the peptide.

In analogy to the  $^{68}\text{Ga-DOTA-SFITGv6}$  PET/CT findings for patients with HNSCC and non–small cell lung carcinoma (12),  $^{68}\text{Ga-DOTA-SFLAP3}$  PET/CT revealed peptide accumulation in the kidneys, secretion into the gastrointestinal tract, and intraluminal transport to the terminal ileum and the cecum. Thus, when SFLAP3 is being considered for imaging of  $\alpha_v\beta_6$  integrin–positive carcinomas occurring below the diaphragm, administration of laxatives (reducing intrabowel activity and avoiding a high background signal) and improvement of the pharmacokinetic properties of the peptide are required.

### CONCLUSION

We found that the  $\alpha_{\nu}\beta_{6}$  integrin–binding peptide SFLAP3 provides improved affinity and excellent binding properties for  $\alpha_{\nu}\beta_{6}$  integrin–expressing HNSCC tumors in vitro and in vivo. Thus, SFLAP3 represents a promising tracer for both diagnostic imaging and targeted therapy of  $\alpha_{\nu}\beta_{6}$  integrin–expressing tumors.

### **DISCLOSURE**

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