

Near-Infrared Diffuse Optical Imaging for Early Prediction of Breast Cancer Response to Neoadjuvant Chemotherapy: A Comparative Study Using ^{18}F -FDG PET/CT

Shigeto Ueda¹, Nobuko Yoshizawa², Takashi Shigekawa¹, Hideki Takeuchi¹, Hiroyuki Ogura³, Akihiko Osaki¹, Toshiaki Saeki¹, Yukio Ueda⁴, Tomohiko Yamane⁵, Ichiei Kuji⁵, and Harumi Sakahara²

¹Department of Breast Oncology, International Medical Center, Saitama Medical University, Yamane, Hidaka, Japan; ²Department of Diagnostic Radiology and Nuclear Medicine, Hamamatsu University, School of Medicine, Handayama, Hamamatsu, Japan;

³Department of Breast Surgery, Hamamatsu University, School of Medicine, Handayama, Hamamatsu, Japan; ⁴Central Research Laboratory, Hamamatsu Photonics K.K., Hamakitaku, Hamamatsu, Japan; and ⁵Department of Nuclear Medicine, International Medical Center, Saitama Medical University, Yamane, Hidaka, Japan

Diffuse optical spectroscopic imaging (DOSI) is used as an indicator of tumor blood volume quantified by tissue hemoglobin concentrations. We aimed to determine whether early changes in tumor total hemoglobin (tHb) concentration can predict a pathologic complete response (pCR) to neoadjuvant chemotherapy in patients with operable breast cancer, and we compared the predictive value of pCR between DOSI and ^{18}F -FDG PET combined with CT. **Methods:** Of the 100 patients enrolled, 84 patients were prospectively evaluated for primary objective analysis. Sixty-four of the patients underwent both sequential DOSI scans at baseline after their first and second chemotherapy courses and ^{18}F -FDG PET/CT at baseline and after their second chemotherapy course. The mean tHb (tHb_{mean}) concentration and SUV_{max} of the lesion were measured using DOSI and ^{18}F -FDG PET/CT, respectively, and the percentage change in tHb_{mean} ($\Delta\text{tHb}_{\text{mean}}$) and change in SUV_{max} ($\Delta\text{SUV}_{\text{max}}$) were calculated. We compared the diagnostic performances of DOSI and ^{18}F -FDG PET/CT for predicting pCR via the analysis of the receiver-operating-characteristic curves. **Results:** pCR was achieved in 16 patients, and neoadjuvant chemotherapy caused a significant reduction of $\Delta\text{tHb}_{\text{mean}}$ in pCR compared with non-pCR after the 2 chemotherapy courses. When the tentative $\Delta\text{tHb}_{\text{mean}}$ cutoff values after the first and second courses were used, the ability to predict pCR was as follows: 81.2% sensitivity/47.0% specificity and 93.7% sensitivity/47.7% specificity, respectively. Comparison of the diagnostic performances of DOSI and ^{18}F -FDG PET/CT revealed areas under the curve of 0.69 and 0.75 of $\Delta\text{tHb}_{\text{mean}}$ after the first and second courses, respectively, which were lower than those of $\Delta\text{SUV}_{\text{max}}$ (0.90). **Conclusion:** DOSI predicted pCR in patients with breast cancer with moderate accuracy. The diagnostic performance of DOSI was inferior to that of the early metabolic response as monitored by ^{18}F -FDG PET/CT.

Key Words: optical imaging; hemoglobin; neoadjuvant chemotherapy; breast cancer; FDG-PET

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Neoadjuvant chemotherapy (NAC) has been established as the standard of care for patients with locally advanced breast cancer (1). Although it is increasingly used in early breast cancer depending on the histologic subtype, further predictive tools are required as companion diagnostics to identify and treat patients with responsive disease.

Biofunctional imaging techniques for early response assessment may soon change the process of cancer management. Presently, ^{18}F -FDG PET combined with CT is accepted as a noninvasive method for the early evaluation of the response to therapy because decreased glucose metabolism precedes tumor shrinkage (2). However, the expensive technology using ^{18}F -FDG PET/CT during NAC has precluded its integration into clinical practice (3). Near-infrared optical imaging based on the visualization of the hemodynamic status of the tissue (such as oxyhemoglobin [O_2Hb] and deoxyhemoglobin [HHb] concentrations) is reportedly promising for determining the physiologic status of tumor-bearing breast tissue and for monitoring early responses (4).

We recently established a time-resolved (TR)-diffuse optical spectroscopic imaging (DOSI) system (TRS20; Hamamatsu Inc.) for breast measurement and reported that elevation of the total hemoglobin (tHb) concentration in lesions compared with that of the background normal tissue reflects hypervascularity of the lesion (5). We hypothesized that changes in lesional tHb concentrations would indicate the degree of tumor angiogenesis during treatment, thereby predicting the therapeutic response.

Several recent studies have revealed that decreased lesional tHb concentrations observed on longitudinal DOSI scans can accurately distinguish pathologic responders to cytotoxic chemotherapy from others (6,7).

Therefore, we aimed to prospectively evaluate the diagnostic performance of sequential TR-DOSI scans for monitoring early chemotherapy response and primarily to determine whether changes in lesional tHb concentration measured after the first and second courses of cytotoxic drug administration can predict pathologic complete response (pCR) in patients with primary breast cancer. Secondarily, we compared the diagnostic performances of TR-DOSI and ^{18}F -FDG PET/CT for predicting pCR.

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For correspondence or reprints contact: Shigeto Ueda, Saitama Medical University, International Medical Center, 1371-1 Yamane, Hidaka, Saitama, 350-1298, Japan.

E-mail: syueda@saitama-med.ac.jp

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MATERIALS AND METHODS

Patient Eligibility

Patients older than 18 y who had newly diagnosed, biopsy-proven breast cancer; clinical stage T1c-4, N0-2 primary breast cancer according to the TNM classification (sixth edition); and who planned to undergo at least 4 chemotherapy cycles were eligible for this prospective TR-DOSI chemotherapy monitoring study. The exclusion criteria included pregnancy, previous breast cancer treatment, bilateral breast cancer, or ineligibility for surgery. Patients enrolled at Saitama Medical University and Hamamatsu University, School of Medicine, participated in our TR-DOSI study. The institutional review board at each of these centers approved this study, and written informed consent was obtained from each patient. The study was conducted in accordance with the Declaration of Helsinki and was registered at the UMIN Clinical Trials Registry (no. 000011888). The physicians determined a standard-of-care chemotherapy regimen for each patient according to the patient's age, cancer stage, and tumor subtype. All patients underwent breast-conserving surgery or a mastectomy with sentinel node biopsy or axillary dissection after completing their courses of chemotherapy.

Study Design

All patients in this study had previously undergone a mammogram, ultrasound, or contrast-enhanced MRI.

TR-DOSI was performed before treatment and after the first and second infusions of the anticancer drug (Fig. 1). Only patients with clearly visible lesions on ultrasound were considered evaluable and underwent sequential TR-DOSI scans. In our study, measurements were obtained an average of 18 d (range, 14–30 d) after the core biopsy and at day –2 to day 1 before the initial infusion of the anticancer drug. The subsequent assessments were taken at day –2 to day 1 before the second or third drug infusions. The patients also underwent ^{18}F -FDG PET/CT scans (Biograph 6/16; Siemens) at baseline and 2–3 wk after the second course of NAC.

TR-DOSI Scan Protocol

The system has been described previously in detail (8). In brief, after locating the tumor by ultrasound, a grid was manually drawn using a marker pen, mapping 7 × 7 points with 10-mm intervals between the points in the x–y dimension, with the tumor located at the center of the grid. A handheld probe with a 2.8-cm source-detector distance was brought into contact with each point on the breast, thus measuring the optical properties of the tissue at each point. The contralateral normal breast was also measured as a reference.

The imaging systems at the 2 institutions were confirmed to have comparable imaging quality and data acquisition capability before the start of the study. After the subtraction of water and lipid absorption

(using the estimate that normal breast tissue comprises 18.7% water and 66.1% lipid) (9), tissue concentrations (μM) of O_2Hb and HHb were calculated from the absorption coefficient at wavelengths of 760, 800, and 830 nm. The tHb concentration was recorded as the sum of O_2Hb and HHb. The percentage of tissue oxygen saturation was defined as the ratio between the concentrations of O_2Hb and tHb ($\text{O}_2\text{Hb}/\text{tHb} \times 100$). The region of interest (ROI; a circle measuring 2 cm in radius) was assigned to the skin, including the area of the target lesion and the adjacent normal tissue. In total, 10–14 points were included for each ROI. We set the ROI, showing the highest concentration of tHb above the lesion as identified by ultrasound. After all imaging studies were completed, the optical images acquired at baseline and after the first and second courses of chemotherapy were analyzed by 2 investigators masked to all medical and pathologic reports. The percentage change in the mean tHb ($\Delta\text{tHb}_{\text{mean}}$) between the baseline and after chemotherapy was calculated as follows: $(\text{posttherapeutic tHb}_{\text{mean}} - \text{baseline tHb}_{\text{mean}})/\text{baseline tHb}_{\text{mean}} \times 100 (\%)$.

^{18}F -FDG PET/CT Scan Procedure

Patients with a clearly visible lesion at the baseline assessment underwent serial ^{18}F -FDG PET/CT scans. The imaging protocol was designed to ensure SUV measurements across all time points. Blood glucose levels were measured in all patients before ^{18}F -FDG administration; no patient had blood glucose levels exceeding 200 mg/dL. After fasting for at least 6 h, the patients received an intravenous injection of ^{18}F -FDG (3.7–4.0 MBq/kg). After a 60-min uptake period, all images were acquired from the thigh level to the skull base with the patients' arms raised using a PET/CT system combined with a 6- or 16-slice CT scanner. PET emission data were acquired in the 3-dimensional mode (2 min per bed position) and reconstructed using ordered-subsets expectation maximization. Tumor ^{18}F -FDG uptake was quantified by SUV, which normalizes the measured tissue activity in an ROI by the injected dose and body weight, calculated by the tracer concentration per the following equation: $(\text{Bq/mL})/(\text{injected activity [Bq]}/\text{patient body weight [g]})$.

All the PET/CT images were interpreted by experienced nuclear medicine physicians who were masked to all medical and pathologic information. When a hypermetabolic lesion was detected on PET/CT, the SUV_{max} was prospectively calculated, and the percentage change in $\Delta\text{SUV}_{\text{max}}$ was calculated as follows: $(\text{posttherapeutic SUV}_{\text{max}} - \text{baseline SUV}_{\text{max}})/\text{baseline SUV}_{\text{max}} \times 100 (\%)$.

Histopathologic Response

Resected surgical specimens were used as the reference standard for determining the residual disease status. The surgical specimens were cut into 0.5-cm-thick slices, fixed in 10% neutral-buffered formalin, and processed for histologic examination. For routine clinical practice, all slides sectioned from the paraffin-embedded blocks were reviewed and reported with respect to residual cancer cellularity, in situ disease, and the number of lymph nodes involved.

At least 2 experienced pathologists meticulously reviewed all surgical specimens and reached a consensus. A histopathologic response was assessed by applying the grading criteria to definitive surgery specimens in comparison with the initial core biopsy samples. The meta-analysis from Cortazar et al. showed that only pCR, defined as the absence of invasive cancer cells in the primary tumor and in lymph nodes, is associated with improved patient survival (10). In this study, however, we defined the primary endpoint of pCR as the absence of

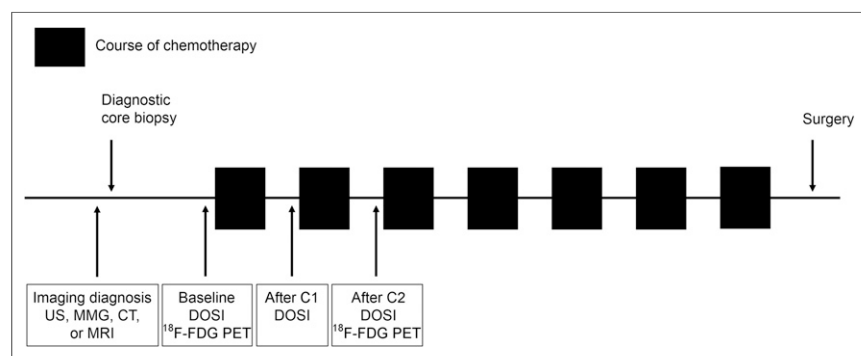


FIGURE 1. Longitudinal imaging study with ^{18}F -FDG PET and DOSI. C1 = first chemotherapy course; C2 = second chemotherapy course; MMG = mammography; US = ultrasound.

invasive cancer cells in the breast irrespective of the presence of lymph node infiltration by malignant cells (*ypT0/is*) (11). All other cases were classified as non-pCR.

Statistical Analysis

The Student *t* test was used when the data followed a normal distribution. Otherwise, the nonparametric Mann–Whitney *U* test was used. The χ^2 test was performed to analyze the associations between 2 categorical variables. To identify an optimal threshold for pCR prediction, receiver-operating-characteristic curve analysis was performed by incrementally increasing the cutoff values. The area under the curve (AUC), sensitivity, specificity, positive predictive value (PPV), negative predictive value (NPV), and accuracy were obtained from the receiver-operating-characteristic curve analysis. A *P* value of 0.05 or less was considered statistically significant. Data were analyzed using statistics software (version 15.2.2; MedCalc).

RESULTS

Patients

Of the 100 patients who were enrolled between September 2013 and February 2015 from the 2 institutes, 84 patients (84%) were included in the TR-DOSI study and 64 patients (64%) were included in a comparison study of TR-DOSI and ^{18}F -FDG PET. Patient characteristics are shown in Table 1. The number of patients included in each analysis are summarized in Supplemental Figure 1 (supplemental materials are available at <http://jnm.snmjournals.org>). After chemotherapy was completed, 39 patients (46.4%) underwent breast-conserving surgery. Histopathology revealed pCR in 16 (19%) and non-pCR in 68 (81%) of the 84 patients. pCR tumors had a significantly higher frequency of hormone-receptor negativity or human epidermal growth factor receptor 2 positivity than non-pCR tumors (*P* = 0.003). No difference was observed between pCR and non-pCR tumors with

TABLE 1
Patient and Tumor Characteristics

Characteristic	DOSI study			DOSI + PET study		
	Parameter	No. of patients	%	Parameter	No. of patients	%
Total number		84			64	
Age (y)						
Mean	56			55.9		
SD	10.4			11.4		
Range	35–77			35–77		
Tumor size (mm)						
Mean	37.5			39.3		
SD	16.8			17.1		
Range	7–97			7–97		
Histology						
IDC		76	90.5	56	87.5	
ILC		2	2.4	2	3.1	
Other		6	7.1	6	9.4	
Estrogen receptor status						
Positive		47	55.9	37	57.8	
Negative		37	44.1	27	42.2	
Progesterone receptor status						
Positive		37	44.1	32	50	
Negative		47	55.9	32	50	
HER2 status						
Positive		18	21.4	14	21.9	
Negative		66	78.6	50	78.1	
Nodal status						
Positive		58	69	43	67.2	
Negative		26	31	21	32.8	
Histologic assessment after NAC						
pCR (<i>ypT0/is</i> , <i>ypN0</i>)		13	15.5	11	17.2	
pCR (<i>ypT0/is</i> , <i>ypN1</i>)		3	3.5	3	4.7	
Non-pCR		68	81	50	78.1	

IDC = invasive ductal carcinoma; ILC = invasive lobular carcinoma; HER2 = human epidermal growth factor receptor 2.

TABLE 2
Chemotherapy Regimens

Type of regimen	No. of courses	No. of patients	%
Nab-paclitaxel, 260 mg/m ² , q3w	4	22	26.2
Followed by epirubicin, 90 mg/m ² + cyclophosphamide, 600 mg/m ² , q3w	4		
Epirubicin, 90 mg/m ² + cyclophosphamide, 600 mg/m ² , q3w	4	30	35.7
Followed by docetaxel, 75 mg/m ² , q3w	4		
Docetaxel, 75 mg/m ² + doxorubicin, 50 mg/m ² + cyclophosphamide, 500 mg/m ² , q3w	4	1	1.2
Fluorouracil, 500 mg/m ² + epirubicin, 90 mg/m ² + cyclophosphamide, 500 mg/m ² , q3w	4	2	2.3
Followed by docetaxel, 75 mg/m ² , q3w	4		
Fluorouracil, 500 mg/m ² + epirubicin, 90 mg/m ² + cyclophosphamide, 500 mg/m ² , q3w	4	4	4.8
Followed by docetaxel, 75 mg/m ² + trastuzumab, 6 mg/kg, q3w*	4		
Carboplatin AUC6 + docetaxel, 75 mg/m ² + trastuzumab, 6 mg/kg, q3w*	6	15	17.9
Paclitaxel, 90 mg/m ² , qw×3 + bevacizumab, 10 mg/kg, q2w×2	6	10	11.9

*Initial dose of trastuzumab was 8 mg/kg.
Nab = nanoparticle albumin-bound.

respect to patient age, tumor size, histology, or axillary involvement. The mean tumor depth from the skin as seen by ultrasound was 6.8 mm (range, 0–17.3 mm). The chemotherapy regimens administered in this study, including the doses and schedules, are summarized in Table 2.

Hemodynamic Response with TR-DOSI

The first TR-DOSI scan was obtained at a median of −1 d (range, −2 to 1 d) before the first infusion. No significant differences were found in the baseline hemoglobin parameters between pCR and non-pCR irrespective of the intrinsic subtypes (Supplemental Table 1). The second and third scans were obtained at a mean (±SD) of 25.1 d ± 7.2 and 48.8 d ± 11.7 after the first infusion, respectively. Representative optical images of lesional tHb from 3 different subjects at baseline and after the first and second chemotherapy courses are shown in Figure 2. Figure 3A shows ΔtHb_{mean} during chemotherapy in pCR and non-pCR lesions. pCR tumors showed a significantly larger decrease in ΔtHb_{mean} after the first chemotherapy course (first-course ΔtHb_{mean}) than did non-pCR tumors (mean, −23.4% ± 4.3 SE vs. mean, −14.1% ± 1.7 SE; $P = 0.02$) and after the second chemotherapy course (second-course ΔtHb_{mean}) (mean, −33.9% ± 3.8 SE vs. mean, −20.2% ± 1.7 SE; $P = 0.001$). Figure 3B compares the absolute value tHb_{mean} between pCR and non-pCR lesions. The tHb_{mean} at baseline and after the first course did not differ between pCR and non-pCR tumors (baseline: median, 31.1; 95% confidence interval [CI], 25.7–49.8, vs. median, 33.5; 95% CI, 31.2–38.3 [$P = 0.4$]; and first course: median, 23.8; 95% CI, 20.8–31.5, vs. median, 29.8; 95% CI, 27.8–31.9 [$P = 0.06$]). The second-course tHb_{mean} differed significantly between pCR and non-pCR tumors (median, 19.9; 95% CI, 16.8–27.3, vs. median, 28.0; 95% CI, 24.4–31.2 [$P = 0.02$]). The ability to predict pCR was as follows: sensitivity, 81.2%; specificity, 47.0%; PPV, 26.5%; NPV, 91.4%; and accuracy, 53.5%, with an optimal cutoff value of −12.4% for the first-course ΔtHb_{mean} , and sensitivity, 93.7%; specificity, 47.7%; PPV, 30.0%; NPV, 96.9%; and accuracy, 56.6%, with an optimal cutoff value of −20.5% for the second-course ΔtHb_{mean} .

Metabolic Response with ¹⁸F-FDG PET/CT

Of the 69 patients who agreed to participate in the PET study and underwent sequential ¹⁸F-FDG PET/CT scans, 64 (92.7%) patients who had a tumor SUV_{max} greater than 3.0 at baseline were evaluated for PET-guided monitoring of their response to treatment (3). The patients' distributions between the 2 studies were similar (Table 1). A significant decrease in ΔSUV_{max} was observed in pCR tumors compared with that of non-pCR tumors (mean, −72.5% ± 3.5 SE vs. −35.6% ± 3.4 SE; $P < 0.0001$). For an optimal threshold of ΔSUV_{max} set at −53.3%, the diagnostic performance for predicting pCR was as follows: sensitivity, 100%; specificity, 77.7%; PPV, 55.5%; and NPV, 100%. The diagnostic accuracy was 82.6%.

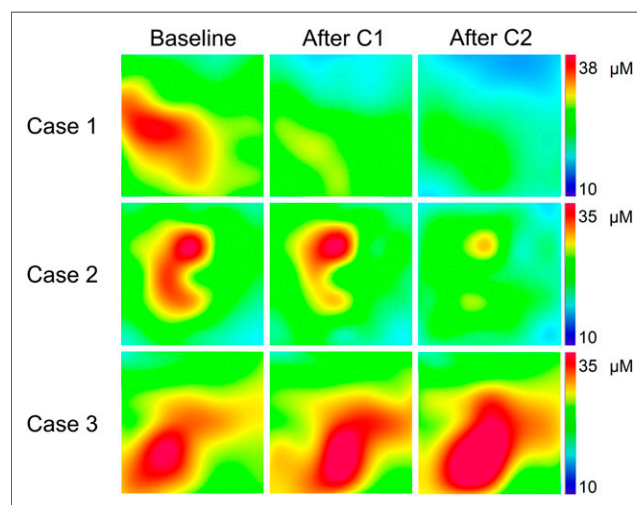


FIGURE 2. Lesional total hemoglobin maps from 3 different subjects at baseline, after C1, and after C2. Each map shows a 60 × 60 mm measurement area that includes tumor and surrounding normal margin. (Top) Example of pCR. Tumor size was 22.0 mm before chemotherapy. (Middle) Example of 47.0-mm tumor that partially responded to chemotherapy. (Bottom) Example of 24.2-mm tumor that did not respond to chemotherapy. C1 = first chemotherapy course; C2 = second chemotherapy course.

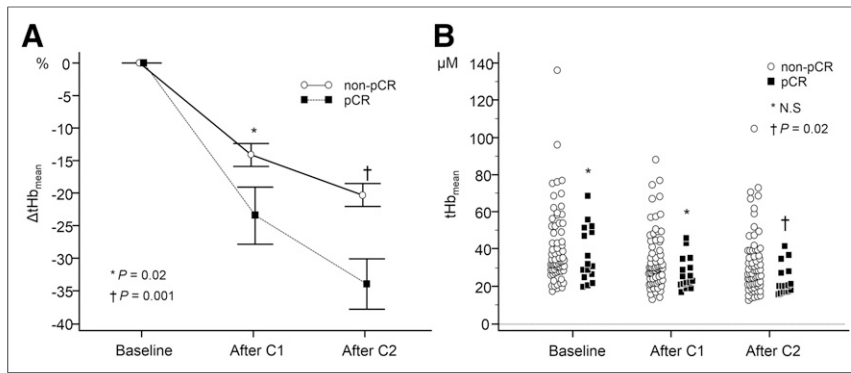


FIGURE 3. (A) Change in tHb_{mean} (ΔtHb_{mean}) during neoadjuvant chemotherapy in pCR and non-pCR. (B) Absolute value of tHb_{mean} concentration at baseline, after C1, and after C2 in pCR and non-pCR. χ^2 test was performed. C1 = first chemotherapy course; C2 = second chemotherapy course; N.S = not significant.

Comparison of TR-DOSI with ^{18}F -FDG PET/CT

Comparison of the diagnostic performance for predicting pCR between TR-DOSI ΔtHb_{mean} and ^{18}F -FDG PET/CT ΔSUV_{max} using receiver-operating-characteristic curve analysis indicated that the AUCs of both first- and second-course ΔtHb_{mean} were inferior to that with ΔSUV_{max} (Fig. 4). There was no significant difference between those of the first- and second-course ΔtHb_{mean} . Scatterplots showed no significant linear correlation between second-course ΔtHb_{mean} and ΔSUV_{max} ($r = 0.23$, $P = 0.06$; Fig. 5). When combined with second-course ΔtHb_{mean} and ΔSUV_{max} using an optimal cutoff, the results were as follows: diagnostic accuracy, 93.7%; sensitivity, 100%; specificity, 92.0%; PPV, 77.7%; and NPV, 100%.

DISCUSSION

Early Response of Optical Hemodynamic Biomarker

Both the first- and the second-course ΔtHb_{mean} for the pCR tumors decreased significantly more than those for the non-pCR tumors. In most of the pCR tumors, the lesional tHb decreased

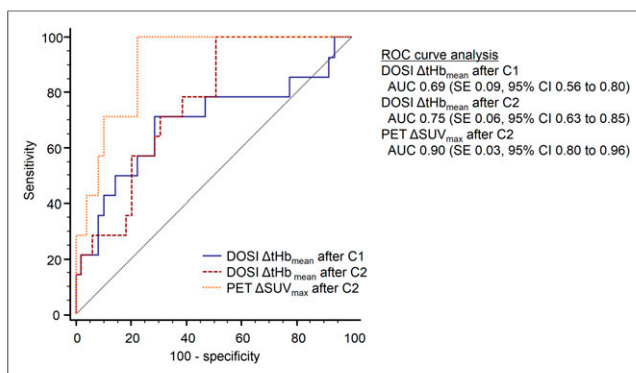


FIGURE 4. Comparison of diagnostic performance between DOSI ΔtHb_{mean} and ^{18}F -FDG PET ΔSUV_{max} for predicting pCR. Receiver-operating-characteristic (ROC) curve analysis indicated AUC of 0.69 for ΔtHb_{mean} after C1, AUC of 0.75 for ΔtHb_{mean} after C2, and AUC of 0.90 for ΔSUV_{max} . ΔtHb_{mean} after C1 was significantly inferior to ΔSUV_{max} ($P = 0.03$); there were no significant differences between ΔtHb_{mean} after C2 and ΔSUV_{max} ($P = 0.06$) and between ΔtHb_{mean} after C1 and ΔtHb_{mean} after C2 ($P = 0.2$). C1 = first chemotherapy course; C2 = chemotherapy course.

sharply after beginning chemotherapy and remained at a low level equivalent to that of the background tissue. In contrast, ΔtHb_{mean} of non-pCR tumors varied greatly in response to chemotherapy. In half of the non-pCR patients, the tumor tHb concentration decreased by $\sim 20\%$ or less. Consequently, although the specificity and PPV were low, the high sensitivity and high NPV of this method could help physicians exclude non-responding patients early on in the course of NAC.

In contrast, baseline hemoglobin parameters, including tHb and oxygen saturation, did not differ between pCR and non-pCR (Supplemental Fig. 1). Optical researchers showed that tHb or oxygen saturation of pCR-achieving tumors was significantly

higher than that of non-pCR tumors (12,13). This discrepancy may be explained by differences of technology and measurement procedures or physiologic variations of the baseline hemoglobin concentration.

Comparison Between TR-DOSI and ^{18}F -FDG PET/CT

Comparison of TR-DOSI and ^{18}F -FDG PET/CT for predicting pCR revealed that the AUC (0.75) after the second-course ΔtHb_{mean} was inferior to the AUC (0.90) after the second-course ΔSUV_{max} . This finding indicates that ^{18}F -FDG PET technology is more useful than tHb optical imaging with regard to the early prediction of tumor response. PERCIST is still well suited to early prediction of the tumor response to chemotherapy (14). Coudert et al. conducted a successful ^{18}F -FDG PET-guided response-adopted randomized trial and revealed that the combination chemotherapy of bevacizumab and trastuzumab plus docetaxel had a higher pCR rate (43.8%) than that (24.0%) of trastuzumab plus docetaxel in human epidermal growth factor receptor 2-positive breast cancer that was less responsive to trastuzumab based on ^{18}F -FDG PET/CT (15). In metabolic responders treated with trastuzumab plus docetaxel, the pCR rate was close to 54%.

Although optical imaging could be a low-cost alternative to ^{18}F -FDG PET/CT, tHb measurements alone may not be enough to replace tumor glycolysis measurements for predicting histologic outcomes. The weak linear correlation ($r = 0.23$, $P = 0.06$) we observed between ΔtHb_{mean} and ΔSUV_{max} demonstrates the significance of using multiple parameters to assess the response to chemotherapy (Fig. 5). The combined results from TR-DOSI and ^{18}F -FDG PET/CT distinguished pCR from non-pCR with an accuracy of 93.7%, which was higher than that of either modality alone (^{18}F -FDG PET/CT accuracy, 82.6%, and DOSI accuracy, 56.6%). This result suggests that the response of breast cancer to chemotherapy is complex and multifactorial—that is, the use of multiparametric and multimodal imaging biomarkers may more precisely stratify the tumor response (16). The present criteria used for histologic assessment depend on the degree of cancer cell eradication and tumor shrinkage; however, tumor stromal changes, such as remodeling of the vasculature, are not considered. Therefore, a subgroup of patients classified as non-pCR might have responded but simply were not recognized as having responded under the current classification system. Further study is required to clarify whether assessment of early tHb response using TR-DOSI will translate into survival benefits.

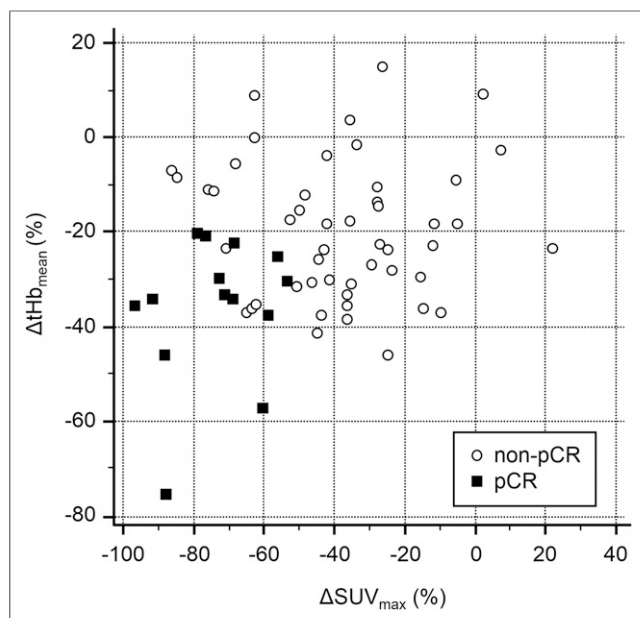


FIGURE 5. Scatterplots showed no significant linear correlation between ^{18}F -FDG PET $\Delta\text{SUV}_{\text{max}}$ and DOSI $\Delta\text{tHb}_{\text{mean}}$ ($r = 0.23$; 95% CI, -0.01 to 0.45 ; $P = 0.06$). Results using post-second-course $\Delta\text{tHb}_{\text{mean}}$ and $\Delta\text{SUV}_{\text{max}}$ with optimal cutoffs for pCR identification were as follows: sensitivity, 100%; specificity, 92.0%; PPV, 77.7%; NPV, 100%; accuracy, 93.7%.

Further work is required to overcome the limitations of the present study. First, systemic stratification of intrinsic subtypes is recommended when conducting a clinical study because different biologic characteristics and administration of targeted drugs may influence tumor vascularity. Previous ^{18}F -FDG PET studies demonstrated that triple-negative breast cancers are more intensely ^{18}F -FDG-avid than others (17,18). A prospective comparison study stratified by intrinsic subtype with identical regimes for all patients is required. Second, although pCR is a suitable surrogate prognostic marker in patients with breast cancer, a recent meta-analysis of neoadjuvant trials has understated the importance of pCR in patients with luminal tumors (10).

We had 3 reasons why we defined the primary endpoint as pCR with *ypT0/is* irrespective of lymph node involvement. First, unlike ^{18}F -FDG PET/CT, TR-DOSI can only measure primary tumors, including the surrounding normal tissue, but cannot detect axillary metastatic lymph nodes. Second, our aim was to evaluate the correlation between early tHb changes of the primary tumor and the histologic response of the primary tumor after completion of neoadjuvant chemotherapy. Third, we consider the knowledge of the primary tumor achieving a pCR as still being informative because the surgeon may decide to perform minimal breast-conserving surgery on the patient.

The TR-DOSI and PET comparison study included only 64 patients because some patients refused further exposure to radiation or for financial reasons.

There are several limitations of DOSI technology. First, the measurement of optical absorption is limited to the reach of photons and up to only a few centimeters depth from the skin. The entire tumor blood volume cannot be observed using this approach, which may result in partial-volume effects. In addition, the chest wall thickness can be tilted at different angles, thereby compromising the

measurement (19). Second, the low sensitivity and poor spatial resolution of this technique may decrease the reproducibility of the results. Some investigators have argued that the use of ultrasound- or MRI-guided diffuse optical tomography may provide better results than DOSI alone, which could improve the quality of the study (20,21). Third, no consensus has been reached for determining the ROI of the lesional tHb regarding user and device independence. Fourth, our TR-DOSI cannot assess the tissue content of water and lipid. To improve the diagnostic accuracy, more data should be acquired at the longer wavelengths that are absorbed by water and lipids.

CONCLUSION

To the best of our knowledge, the present prospective study is the first to demonstrate that the early tHb response of a tumor to chemotherapy can be used to identify pCR with moderate accuracy and with a lower diagnostic performance than the ^{18}F -FDG PET/CT response classification in numerous patients with breast cancer. However, the combination of DOSI and ^{18}F -FDG PET/CT improved the diagnostic performance over that of each modality alone. This noninvasive DOSI technology has the potential to provide complementary information for directing individualized therapy.

DISCLOSURE

The costs of publication of this article were defrayed in part by the payment of page charges. Therefore, and solely to indicate this fact, this article is hereby marked “advertisement” in accordance with 18 USC section 1734. No potential conflict of interest relevant to this article was reported.

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