Molecular Imaging and Quantitation of EphA2 Expression in Xenograft Models with ⁸⁹Zr-DS-8895a

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Subtype A2 of the erythropoietin-producing hepatocellular tyrosine kinase (EphA2) cell surface receptor is expressed in a range of epithelial cancers. This study evaluated the molecular imaging of EphA2 expression in vivo in mouse tumor models using SPECT/MR and PET/MR and a humanized anti-EphA2 antibody, DS-8895a. Methods: DS-8895a was labeled with 111In, 125I, and 89Zr and assessed for radiochemical purity, immunoreactivity (Lindmo analysis), antigen-binding affinity (Scatchard analysis), and serum stability in vitro. In vivo biodistribution, imaging, and pharmacokinetic studies were performed with SPECT/MR and PET/MR. A dose-escalation study was also performed to determine EphA2 receptor saturability through tissue and imaging quantitative analysis. Results: All conjugates demonstrated good serum stability and specific binding to EphA2-expressing cells in vitro. In vivo biodistribution studies showed high uptake of 111In-CHX-A"-DTPA-DS-8895a and 89Zr-Df-Bz-NCS-DS-8895a in EphA2-expressing xenograft models, with no specific uptake in normal tissues. In comparison, retention of 125I-DS-8895a in tumors was lower because of internalization of the radioconjugate and dehalogenation. These results were confirmed by SPECT/MR and PET/MR. EphA2 receptor saturation was observed at the 30 mg/kg dose. Conclusion: Molecular imaging of tumor uptake of DS-8895a allows noninvasive measurement of EphA2 expression in tumors in vivo and determination of receptor saturation. 89Zr-Df-Bz-NCS-DS-8895a is suited for human bioimaging trials on the basis of superior imaging characteristics and will inform DS-8895a dose assessment and patient response evaluation in clinical trials.

Key Words: bioimaging; DS-8895a; EphA2; 89Zr; cancer

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he erythropoietin-producing hepatocellular (Eph) tyrosine kinase receptor group is the largest known family of tyrosine kinase receptors. The receptors consist of an extracellular ligand binding domain, a short transmembrane region, and a cytoplasmic kinase domain. There are 2 subclasses of receptor, EphA (EphA1-EphA10) and EphB (EphB1-EphB6), based on the sequence homologies of the extracellular domain and their binding affinity to glycosylphosphatidylinositol-linked ephrin A (ephrin A1–A5) or transmembrane ephrin B (ephrin B1–B3) ligands (1-3). Activation of the Eph receptor kinase domain can result from several processes, including binding of ligand to receptor, resulting in activation of downstream pathways; contact-dependent cell-cell communication (2); and crosstalk with other signaling systems. Eph/ephrin interactions are particularly important during embryonic development but are also involved in adult tissue homeostasis as they have roles in the development of neuronal pathways, axon guidance formation, maintenance and repair of synaptic junctions, vascular development, and epithelial homeostasis (4-7).

The EphA2 receptor is strongly overexpressed in several types of cancer, including glioblastoma (8,9) and cancers of the ovary (10), prostate gland (11), pancreas (12), and esophagus (13). Its expression has been associated with poor prognosis, increased metastasis, and decreased survival (14,15). DS-8895a is an afucosylated humanized anti-EphA2 IgG1 monoclonal antibody with enhanced antibody-dependent cellular cytotoxicity expressed using the proprietary Potelligent CHOK1SV system (Lonza and BioWa), showing in vitro and antitumor efficacy in EphA2-expressing xenograft models.

This study explored the radiolabeling of DS-8895a to ¹²⁵I and—via the bifunctional chelates C-functionalized *trans*-cyclohexyldiethylene-triaminepentaacetic acid (CHX-A"-DTPA) and *p*-isothiocyanatobenzyldesferrioxamine (Df-Bz-NCS)—to ¹¹¹In and ⁸⁹Zr, respectively, suitable for in vivo molecular imaging with SPECT (¹²⁵I and ¹¹¹In) and PET (⁸⁹Zr). The use of such radioconjugates for human bioimaging studies may inform the clinical development of DS-8895a through dose selection and patient response assessment.

MATERIALS AND METHODS

Cell Culture

The human breast carcinoma cell line MDA-MB-231 and the human lymphoblastic leukemia cell line CCRF-CEM were obtained

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from the American Type Culture Collection. The cells were cultured in Dulbecco modified Eagle medium or RPMI (Invitrogen) with 10% fetal calf serum and incubated at 37°C with 5% CO₂.

Flow Cytometry

EphA2 expression was assessed by staining 1×10^6 MDA-MB-231 cells with a 10 μ g/mL dose of humanized DS-8895a, followed by phycoerythrin antihuman secondary antibody. Flow cytometric analysis was performed using Guava flow cytometry (Guava easyCyte 8HT flow cytometer, model 0500-4008; Guava Technologies).

Conjugation of Deferoxamine-p-SCN to DS-8895a for Radiolabeling

DS-8895a was obtained from Daiichi Sankyo Co., Ltd., and was chelated either with the bifunctional metal ion chelator CHX-A"-DTPA (Macrocyclics Inc.) at a 5.0-fold molar excess or with deferoxamine-p-SCN (Df-Bz-NCS; Macrocyclics Inc.) at a 3.0-fold molar excess. Two-milligram aliquots of the conjugates in 50 mM sodium acetate buffer (BDH/VWR Chemicals), pH 5.6, containing 5% w/v sorbitol (BDH/VWR Chemicals) and 0.01% w/v polysorbate 80 (Croda) were stored at -80°C until required.

Radiolabeling and Quality Assurance

Analytic-grade reagents, sterile technique, and pyrogen-free plasticware were used in all labeling steps. After chelation, DS-8895a was trace-radiolabeled as follows: 125I (Perkin Elmer) was attached on tyrosine residues via IODO-GEN chemistry (Perkin Elmer); 111In (Mallinckrodt Australia Pty Ltd.), on lysine residues via the bifunctional metal ion chelating agent CHX-A"-DTPA; and 89Zr (PerkinElmer), on lysine residues via the bifunctional metal ion chelating agent Df-Bz-NCS. For the 2 conjugates that used chemical chelation (111In-CHX-A"-DTPA-DS-8895a and 89Zr-Df-Bz-NCS-DS-8895a), the outcomes of chelation were also assessed. For the former, a solution containing 122 MBq (3.2 mCi) of ¹¹¹In (Mallinckrodt Australia Pty Ltd.) was mixed with 0.5 mg of CHX-A"-DTPA-DS-8895a for 20 min. For the latter, a solution containing 44 MBq (1.2 mCi) of ⁸⁹Zr (PerkinElmer) was mixed with 1.0 mg of Df-Bz-NCS-DS-8895a for 30 min. Radiolabeled products were purified on a Sephadex G50 column (Pharmacia) equilibrated with a sodium chloride injection (British Pharmacopeia 0.9% w/v; Pfizer). To determine structural integrity after chelation and radiolabeling, constructs were analyzed under reducing and nonreducing condition on sodium dodecyl sulfate polyacrylamide gel electrophoresis (SDS-PAGE) gels. Antibody proteins from CHX-A"-DTPA-DS-8895a, Df-Bz-NCS-DS-8895a, and native DS-8895a samples were prepared with and without reducing agents in SDS-PAGE sample buffer. Aliquots of proteins ranging from 1.25 to 5.0 µg were prepared accordingly and analyzed together with known-molecular-weight markers.

Radiochemical Purity

The amount of free versus bound antibody after radiolabeling was determined by instant thin-layer chromatography using silica gel impregnated glass fiber strips (Gelman Sciences, Inc.). Assays were performed in duplicate. Radioactivity was measured with an automated γ -counter (Wizard).

Immunoreactivity and Scatchard Analysis

The immunoreactive fraction of the radiolabeled DS-8895a constructs with EphA2-positive MDA-MB-231 cells was determined by linear extrapolation to binding at an infinite antigen excess using a Lindmo assay as previously described (16,17). Scatchard analysis was used to calculate the apparent association constant and number of antibody molecules bound per cell (16).

Serum Stability

Serum stability was assessed by incubating 5.0 µg of 111In-CHX-A"-DTPA-DS-8895a, 2.5 µg of 125I-DS-8895a, and 5.0 µg of 89Zr-Df-Bz-NCS-DS-8895a in 100 μL of human serum at 37°C for 6 d. Radiochemical purity and single-point immunoreactivity assays at 0 d (day of radiolabeling, no incubation), 2 d, and 6 d of incubation were performed. MDA-MB-231 cells (140×10^6) were used in the singlepoint binding assays under conditions of antigen excess. Radioconstruct integrity was assessed by size-exclusion chromatography performed on a Superdex 200 HR10/30 column (GE Healthcare) at a flow rate of 0.14 mL/min and fraction size of 3.6 mL. The elution buffer was phosphate-buffered saline at pH 7.4. Aliquots of serum containing radioconjugates were collected at the specified times and diluted to 1.0 mL using phosphate-buffered saline, and 10-µL aliquots were retained for radioactive counting to determine recovery. The remaining diluted samples of the radioconjugates in serum were loaded onto the column for size-exclusion chromatography analysis.

Animal Model

In vivo investigations were performed on 5- to 6-wk-old female athymic BALB/c nu/nu mice (Animal Research Centre) bearing established EphA2-expressing breast cancer MDA-MB-231 xenografts or, for antigen-negative control xenografts, the human lymphoblastic leukemia cell line CCRF-CEM. All animal studies were approved by the Austin Hospital Animal Ethics Committee and were conducted in compliance with the Australian Code for the care and use of animals for scientific purposes. To establish tumors, EphA2-positive or -negative cells (2 \times 106 cells) in a total volume of 0.1 mL of phosphate-buffered saline were injected subcutaneously into the left underside flank of the mice. Tumor volume was calculated by the formula [(length \times width²)/2], where length is the longest axis and width is the measurement at right angles to length.

Biodistribution Study

In a first biodistribution study, BALB/c nu/nu mice with established MDA-MB-231 xenografts (tumor volume, 150–200 mm³) received a mixture of 0.185 MBq of 125 I-DS-8895a (5.0 μ g, 5.0 μ Ci) or 0.6031 MBq of 111 In-CHX-A"-DTPA-DS-8895a (5.0 μ g, 16.3 μ Ci) intravenously. In a second biodistribution study, BALB/c nu/nu mice with established MDA-MB-231 xenografts (tumor volume range, 207–844 mg) or CCRF-CEM xenografts (tumor volume range, 129–503 mg) received a 0.1332-MBq dose of 89 Zr-Df-Bz-NCS-DS-8895a (5.0 μ g, 3.6 μ Ci) intravenously. On day 0 (2 h after injection), 1, 2, 3, 5, 7, and 9 or 10 after injection, groups of mice bearing MDA-MB-231 tumors (n=5) were sacrificed and biodistribution was assessed. For mice bearing EphA2-negative CCRF-CEM xenografts, biodistribution was assessed on only days 2 and 7 after injection.

At the designated time points, the mice were exsanguinated by cardiac puncture, and tumors and organs (liver, spleen, kidney, muscle, skin, bone [femur], lungs, heart, stomach, brain, small bowel, tail, and colon) were collected immediately. All samples were counted in a dual-channel γ -scintillation counter (Wizard; PerkinElmer). Triplicate standards prepared from the injected material were counted at each time point with tissue and tumor samples, enabling calculations to be corrected for the physical decay of the isotopes. The tissue distribution data were calculated as the mean \pm SD percentage injected dose (%ID) per gram of tissue for the radiolabeled constructs per time point.

Animal Imaging

For in vivo SPECT imaging of 111 In-labeled DS-8895a, a separate group of 5 mice received a higher dose of 2.035 MBq (55 μ Ci) of 111 In-CHX-A"-DTPA-DS-8895a (15.7 μ g) and were imaged by SPECT and MR on days 0 (2 h after injection), 3, and 7 using

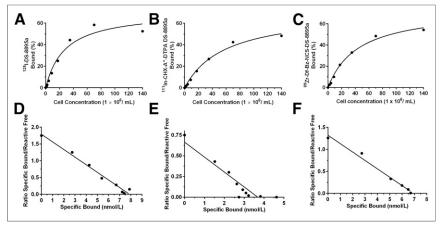


FIGURE 1. (A–C) Lindmo plots showing in vitro binding of ¹²⁵I-DS-8895a (A), ¹¹¹In-CHX-A"-DTPA-DS-8895a (B), and ⁸⁹Zr-Df-Bz-NCS-DS-8895a (C) to increasing concentrations of EphA2-positive MDA-MB-231 cells. (D–F) Scatchard plots showing in vitro binding of ¹²⁵I-DS-8895a (D), ¹¹¹In-CHX-A"-DTPA-DS-8895a (E), and ⁸⁹Zr-Df-Bz-NCS-DS-8895a (F) to MDA-MB-231 cells.

dedicated small-animal SPECT/CT and PET/MR (nanoScan; Mediso) cameras. For in vivo PET imaging of $^{89}\text{Zr-labeled}$ DS-8895a, a separate 5-mouse group received a 2.775-MBq (75 μCi) dose of $^{89}\text{Zr-Df-Bz-NCS-DS-8895a}$ (104.2 μg) and was imaged with PET and MR on days 0 (2 h after injection), 2, and 7 using the nanoScan camera.

Pharmacokinetics

Serum from blood collected from tumor-bearing mice injected with radiolabeled antibody was aliquoted and counted in a γ -counter (Packard). Triplicate standards prepared from the injected material were also counted at each time point to enable calculations to be corrected for the isotope physical decay. The results of the serum were expressed as %ID per liter, and the serum concentrations (μ g/mL) were calculated. A 2-compartment intravenous bolus model with macroparameters, no lag time, and first-order elimination was fitted to serum data for each animal using unweighted nonlinear least squares with Phoenix WinNonLin, model 8 (Certara). The following pharmacokinetic parameters were estimated: half-lives of the initial and terminal phases of disposition, volume at steady state, maximum serum concentration, area under the serum–concentration curve extrapolated to infinite time, and total serum clearance.

EphA2 Saturation In Vivo

The influence of DS-8895a protein dose on tumor uptake and EphA2 saturation in vivo was determined in a separate biodistribution and PET/MR imaging study using $^{89}\text{Zr-Df-Bz-NCS-DS-8895a}$. For the biodistribution study, 3 groups of mice (n=5) were injected with 0.2775 MBq of $^{89}\text{Zr-Df-Bz-NCS-DS-8895a}$ (5.5 μg , 7.5 $\mu Ci)$ combined with different amounts of unlabeled DS-8895a to achieve a total protein dose of 0.3, 3, and 30 mg/kg in a total volume of 0.1 mL of 0.9% w/v NaCl. On days 2 and 7 after injection, all animals were sacrificed and organs were collected as described above. The tissue distribution data were calculated as mean \pm SD %ID/g.

In parallel, 1–2 mice of each group were imaged with PET/MRI on days 0 (2 h after injection), 2, and 7 after injection using the nanoScan camera as described before, and the images was analyzed. Tumor uptake (kBq/cm³) was determined by marking volumes of interest on cross-sectional PET images. Tumor volume (cm³) was determined on the basis of marked volumes of interest on cross-sectional MR images. To convert (kBq/cm³)/mL to %ID/mL, total-body uptake (kBq/cm³) in mice was measured on day 0 as an approximation of injected dose.

Statistical Analysis

A paired t test was used to determine significant differences in the 89 Zr biodistribution results between tissues (%ID/g). An unpaired t test was used to determine significant differences in pharmacokinetic parameters between the 111 In- and 89 Zr-labeled DS-8895a antibodies. For multiple comparisons, 1-way ANOVA was used. All analyses were done using GraphPad Prism, version 6.03. Data are presented as the mean \pm SD, unless stated differently.

RESULTS

Conjugation, Radiolabeling, and Quality Assurance

The results of chelation and radiolabeling were assessed using MDA-MB-231 cells, which were confirmed to have high EphA2 expression. All 3 radioconjugates were

shown to be intact by SDS-PAGE analysis under reducing and nonreducing conditions. Data were also obtained on the stability of ¹¹¹In-CHX-A"-DTPA-DS-8895 (purity, 91.2%; immunoreactivity, 44.0%), ¹²⁵I-DS-8895a (purity, 94.5%; immunoreactivity, 46.6%), and ⁸⁹Zr-Df-Bz-NCS-DS-8895a (purity, 97.5%; immunoreactivity, 51%) at 6 d in human serum.

Using a Lindmo binding assay with MDA-MB-231 cells, the ¹²⁵I-DS-8895a chelate showed 98.9% radiochemical purity, immunoreactivity of 53.8%, and an apparent association constant of

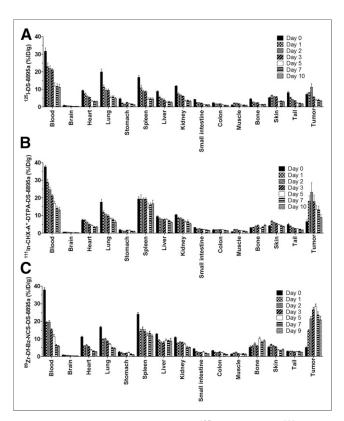


FIGURE 2. Biodistribution properties of 125 I-DS-8895a (A), 111 In-CHX-A"-DTPA-DS-8895a (B), and 89 Zr-Df-Bz-NCS-DS-8895a (C) in MDA-MB-231-xenografted BALB/c nu/nu mice. Bars indicate mean \pm SD (n=5).

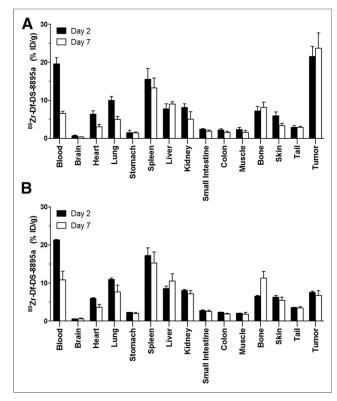


FIGURE 3. Biodistribution properties of 89 Zr-Df-Bz-NCS-DS-8895a in BALB/c *nu/nu* mice bearing EphA2-positive MDA-MB-231 breast tumors (A) and EphA2-negative CCRF-CEM human lymphoblastic leukemia (B) on days 2 and 7 after injection. Bars indicate mean \pm SD (n=5).

 $2.14\times10^8~M^{-1}$ (Fig. 1A). The $^{111}\mathrm{In}\text{-CHX-A''}\text{-DTPA-DS-8895}$ chelate showed high purity (99.6%), immunoreactivity of 55.4%, and an apparent association constant of $2.10\times10^8~M^{-1}$ (Fig. 1B). $^{89}\mathrm{Zr}\text{-Df-Bz-NCS-DS-8895a}$ had a radiochemical purity of 99.6% and immunoreactivity of 54.2% (Fig. 1C). Scatchard analysis indicated that the $^{111}\mathrm{In}\text{-conjugate}$ bound to approximately 40,000 sites per cell (Fig. 1D), compared with 60,000 antibody binding sites per cell for both $^{125}\mathrm{I-DS-8895a}$ and $^{89}\mathrm{Zr-Df-Bz-NCS-DS-8895a}$ (Figs. 1E and 1F).

Biodistribution

Figure 2 summarizes the biodistribution results for $^{125}\text{I-DS-}8895a$, $^{111}\text{In-CHX-A"-DTPA-DS-}8895a$, and $^{89}\text{Zr-Df-Bz-NCS-DS-}8895a$ in EphA2-positive MDA-MB-231 tumors. $^{125}\text{I-DS-}8895a$ tumor uptake was lowest, reaching only 11.23 \pm 4.34 %ID/g by day 2 after injection and declining to 3.42 \pm 0.73 %ID/g by day 10. In comparison, uptake of $^{111}\text{In-CHX-A"-DTPA-DS-}8895a$ reached a maximum of 23.19 \pm 12.17 %ID/g on day 2 after injection and gradually declined to 8.76 \pm 3.65 %ID/g by day 10. Uptake of $^{89}\text{Zr-Df-Bz-NCS-DS-}8895a$ reached 26.59 \pm 3.04 %ID/g on day 3 after injection and then stayed at 28.24 \pm 3.66 %ID/g until day 5 before gradually declining to 20.82 \pm 4.67 %ID/g by day 9.

Organs with a high blood supply, including the heart, kidneys, liver, spleen, and lungs, showed high initial uptake of radiolabeled DS-8895a (Fig. 2) consistent with biodistribution and catabolism of radiolabeled antibodies. Uptake of radioiodinated DS-8895a in these organs declined over time. In contrast, uptake in the spleen, liver, and bone remained high or increased over time with the

¹¹¹In- and ⁸⁹Zr-conjugates, consistent with catabolism of radio-metal-conjugated antibodies (Fig. 2).

The tumor-to-blood ratio for 125 I-DS-8895a increased from 0.23 (2 h after injection) to 0.33 (day 7 after injection). In comparison, the tumor-to-blood ratio increased from 0.17 (2 h after injection) to 0.94 (day 7 after injection) for 111 In-CHX-A"-DTPA-DS-8895a and from 0.14 (2 h after injection) to 3.62 (day 7 after injection) for 89 Zr-Df-Bz-NCS-DS-8895a. The tumor specificity of 89 Zr-Df-Bz-NCS-DS-8895a was confirmed by assessing uptake in the EphA2-negative tumor CCRF-CEM (Fig. 3). Uptake of 89 Zr-Df-Bz-NCS-DS-8895a in CCRF-CEM tumors was significantly lower than that of MDA-MB-231 on days 2 (7.58 \pm 0.29 %ID/g vs. 21.52 \pm 2.65, respectively; $P=8.40\times10^{-6}$) and 7 (6.73 \pm 1.21 %ID/g vs. 23.64 \pm 4.06, respectively; $P=4.43\times10^{-5}$).

In Vivo Molecular Imaging of EphA2 Expression in Tumors

Whole-body SPECT/MR images showed localization of ¹¹¹In-CHX-A"-DTPA-DS-8895a to tumors at early time points after injection (from 2 h onward) (Fig. 4A). ¹¹¹In-CHX-A"-DTPA-DS-8895a uptake in tumors was more discernible at later time points of up to 7 d, even in small tumors.

Similarly, whole-body PET/MR images showed localization of ⁸⁹Zr-Df-Bz-NCS-DS-8895a (Fig. 4B) to tumors at early time points after injection (from 2 h onward). ⁸⁹Zr-Df-Bz-NCS-DS-8895a uptake in tumors was also clearly discernible at later time points of up to 7 d after injection, even in small tumors. Some spleen, liver, and bone activity, consistent with catabolism of ⁸⁹Zr-Df-Bz-NCS, was also observed.

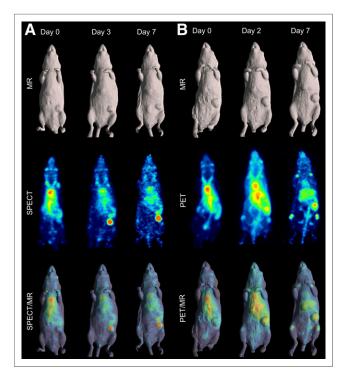


FIGURE 4. (A) MR (surface-rendered), SPECT (maximum-intensity projection), and fused SPECT/MR images of MDA-MB-231-xenografted mice at 2 h (day 0), 3 d, and 7 d after injection of ¹¹¹In-CHX-A"-DTPA-DS-8895a. (B) MR (surface-rendered), PET (maximum-intensity projection), and fused PET/MR images of MDA-MB-231-xenografted mice at 2 h (day 0), 2 d, and 7 d after injection of ⁸⁹Zr-Df-Bz-NCS-DS-8895a.

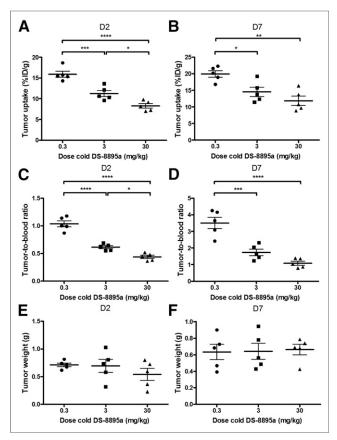


FIGURE 5. Influence of cold-dose DS-8895a on tumor uptake of 89 Zr-Df-Bz-NCS-DS-8895a in BALB/c *nu/nu* mice bearing MDA-MB-231 xenografts on days 2 (A) and 7 (B) after injection, and tumor-to-blood ratios on days 2 (C) and 7 (D) after injection. There was no significant difference in average tumor size among the various dose levels on days 2 (E) and 7 (F) after injection. Bars indicate mean \pm SD (n=5). *P<0.05. *P<0.005. **P<0.005. **P<0.0001.

In Vivo Receptor Saturation

A combination study of biodistribution and PET/MR imaging explored saturation of the EphA2 receptor in vivo. A biodistribution study compared 0.3, 3, and 30 mg/kg doses of $^{89}\text{Zr-labeled DS-8895a}$ in mice bearing MDA-MB-231 xenografts (tumor volume, 0.647 \pm 0.194 g). No significant differences were observed in blood and normal-tissue biodistribution patterns.

A clear protein dose effect was evident for MDA-MB-231 tumor uptake. At all study time points, the highest tumor uptake was observed with the 0.3 mg/kg DS-8895a dose and the lowest with the 30 mg/kg dose, and significantly higher tumor-to-blood ratios were observed with the 0.3 mg/kg protein dose than with the 30 mg/kg dose over the duration of the study (Fig. 5). No significant differences in average tumor size among the various doselevel groups were observed, indicating that the protein dose effect was not influenced by tumor size.

Representative individual-animal PET/MR images obtained with a 0.3, 3, and 30 mg/kg dose of ⁸⁹Zr-labeled DS-8895a on days 2 and 7 are shown in Figure 6. MDA-MB-231 tumor uptake was clearly evident on days 2 (Fig. 6A) and 7 (Fig. 6B) at all dose levels. Compared with the 0.3 mg/kg dose, both the 3 and the 30 mg/kg doses showed less uptake in the xenografts with time,

consistent with the measured %ID/g levels and tumor-to-blood ratios as obtained from the biodistribution study (Fig. 5). Quantitative image analysis of tumor volumes and tumor uptake confirmed a substantial reduction in uptake with both the 3 mg/kg dose and the 30 mg/kg dose.

Pharmacokinetics

The mean pharmacokinetic parameters for 111 In- and 89 Zr-labeled DS-8895a administered at a protein dose of 5 µg (0.25 mg/kg) are presented in Table 1. An unpaired t test determined significant differences in pharmacokinetic parameters between the two radioconjugates. The slightly faster clearance observed with 89 Zr-labeled DS-8895a is consistent with its higher uptake in tumors.

DISCUSSION

We have shown that it is feasible to radiolabel DS-8895a, an anti-EphA2 antibody, with several radioligands suitable for molecular imaging with SPECT (¹²⁵I and ¹¹¹In) and PET (⁸⁹Zr). Chelation and radiolabeling did not alter the structural integrity or immunoreactivity of the constructs. These constructs were also stable in plasma for up to 6 d.

The in vivo biodistribution and imaging patterns showed that ¹²⁵I-DS-8895a had the lowest tumor uptake of all the conjugates at all time points tested. This finding likely reflects internalization and translocation of ¹²⁵I-DS-8895a to the lysosomes, with subsequent degradation of the conjugate and release of the ¹²⁵I-catabolites from the cells. In contrast, ¹¹¹In- and ⁸⁹Zr-catabolites

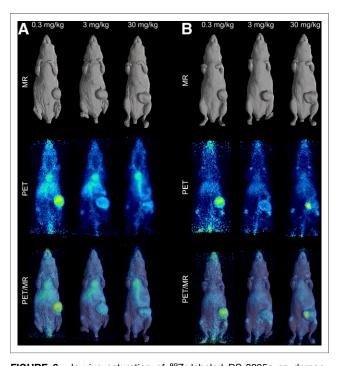


FIGURE 6. In vivo saturation of ⁸⁹Zr-labeled DS-8895a as demonstrated by PET/MR on days 2 (A) and 7 (B) after injection. Representative whole-body surface-rendered MR images, maximum-intensity-projection PET images, and fused PET/MR images are shown for each time point with different dose levels of cold DS-8895a (0.3, 3, and 30 mg/kg). Hot spot in tumor on day 7 PET and PET/MR images of mouse receiving 30 mg/kg is due to blood crust.

TABLE 1
Pharmacokinetic Parameters of ⁸⁹Zr- and ¹¹¹In-Labeled DS-8895a in MDA-MB-231 Tumor–Bearing Mice

Parameter	⁸⁹ Zr-labeled DS-8895a	¹¹¹ In-labeled DS-8895a	Р
AUC (h × μg/mL)	185.7 ± 26.96	417.6 ± 90.60	0.0033
$t_{1/2\alpha}$ (h)	1.48 ± 0.26	8.85 ± 4.97	0.0295
$t_{1/2\beta}$ (h)	102.4 ± 14.65	215.1 ± 72.88	0.0244
C _{max} (µg/mL)	3.03 ± 0.43	2.07 ± 0.29	0.0033
C _L (mL/h)	0.027 ± 0.004	0.012 ± 0.002	< 0.0001
V _{ss} (mL)	3.90 ± 0.11	3.59 ± 0.43	0.1845

AUC = area under curve; $t_{1/2\alpha}$ = half-life of initial phase of disposition; $t_{1/2\beta}$ = half-life of terminal phase of disposition; C_{max} = maximum plasma-serum concentration; C_L = total serum clearance; V_{ss} = volume of distribution at steady state.

Data are mean \pm SD (n = 5). P values are result of unpaired t test; Welch correction was used when variances were significantly different.

are trapped in the cells, allowing higher retention of ¹¹¹In- and ⁸⁹Zr-conjugates in the xenografts.

In vivo targeting of tumor with ¹¹¹In-CHX-A"-DTPA- and ⁸⁹Zr-Df-Bz-NCS-DS-8895a was similar, although the latter was higher, particularly at later time points. The results for ⁸⁹Zr-Df-Bz-NCS-DS-8895a were superior to those of a prior study of anti-EphA2 ⁶⁴Cu-DOTA-1C1, particularly at later time points, when maximal uptake in human tumors is anticipated and when ⁸⁹Zr half-life is better suited to human trials (*18*). These results were comparable to uptake of other ⁸⁹Zr-labeled antibodies in animal models, including trastuzumab (Herceptin; Genentech), although expression of ErbB2 on tumor cell surfaces is much higher than that of EphA2 (*19*–22).

To our knowledge, the impact of protein dose on EphA2 targeting and receptor saturation in vivo has not previously been assessed; reduced uptake of ⁸⁹Zr-Df-Bz-NCS-DS-8895a in tumors was observed at the 3 mg/kg dose level, with slightly lower uptake at the 30 mg/kg level. The 3 mg/kg dose is within the likely range for clinical trials, indicating that EphA2 receptor saturation may occur during dose escalation, thus justifying a bioimaging approach to dose assessment in early-phase trials (23).

In all, we have developed 3 radiolabeled conjugates for DS-8895a, and 89 Zr-Df-Bz-NCS-DS-8895a is our lead compound because of its superior imaging and tumor uptake characteristics. These findings have direct clinical relevance, as we have previously shown in several first-in-human bioimaging studies an excellent correlation between preclinical and clinical biodistribution data and γ -camera imaging using radiolabeled monoclonal antibodies (24–27).

CONCLUSION

We have shown that molecular imaging of radiolabeled DS-8895a allows noninvasive quantitative assessment of EphA2 expression, and receptor saturation, in tumor models. These results are directly relevant to the design and conduct of DS-8895a trials on cancer patients, and a clinical trial of ⁸⁹Zr-Df-Bz-NCS-DS-8895a on patients with EphA2-expressing tumors is under way.

DISCLOSURE

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