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# Reproducibility of $^{18}\text{F}$ -FDG microPET Studies in Mouse Tumor Xenografts

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$^{18}\text{F}$ -FDG has been used to image mouse xenograft models with small-animal PET for therapy response. However, the reproducibility of serial scans has not been determined. The purpose of this study was to determine the reproducibility of  $^{18}\text{F}$ -FDG small-animal PET studies. **Methods:** Mouse tumor xenografts were formed with B16F10 murine melanoma cells. A 7-min small-animal PET scan was performed 1 h after a 3.7- to 7.4-MBq  $^{18}\text{F}$ -FDG injection via the tail vein. A second small-animal PET scan was performed 6 h later after reinjection of  $^{18}\text{F}$ -FDG. Twenty-five sets of studies were performed. Mean injected dose per gram (%ID/g) values were calculated from tumor regions of interest. The coefficient of variation (COV) from studies performed on the same day was calculated to determine the reproducibility. Activity from the second scans performed after 6 h were adjusted by subtracting the estimated residual activity from the first  $^{18}\text{F}$ -FDG injection. For 7 datasets, an additional scan immediately before the second injection was performed, and residual activity from this additional delayed scan was subtracted from the activity of the second injection. COVs of both subtraction methods were compared. Blood glucose values were measured at the time of injection and used to correct the %ID/g values. **Results:** The COV for the mean %ID/g between  $^{18}\text{F}$ -FDG small-animal PET scans performed on the same day 6 h apart was  $15.4\% \pm 12.6\%$ . The delayed scan subtraction method did not produce any significant change in the COV. Blood glucose correction increased the COV. The injected dose, tumor size, and body weight did not appear to contribute to the variability of the scans. **Conclusion:**  $^{18}\text{F}$ -FDG small-animal PET mouse xenograft studies were reproducible with moderately low variability. Therefore, serial small-animal PET studies may be performed with reasonable accuracy to measure tumor response to therapy.

**Key Words:**  $^{18}\text{F}$ -FDG; small-animal PET; reproducibility; tumor xenograft; drug development

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**T**umors have a high metabolic rate and accumulate glucose at a higher rate than normal surrounding tissues in the body (1).  $^{18}\text{F}$ -FDG is an analog of deoxyglucose that has been used for cancer imaging using the radioactive label  $^{18}\text{F}$  (110-min half-life) and PET imaging techniques (2).

Applications of  $^{18}\text{F}$ -FDG include assessing response to therapy for tumor models. Serial scans are performed to monitor changes in tracer accumulation over time.  $^{18}\text{F}$ -FDG can therefore be used to test the efficacy of anticancer drugs, including drugs under development with microPET in preclinical animal studies (3,4). Serial studies are potentially useful to determine if the drug inhibits tumor metabolism.

With the increased use of  $^{18}\text{F}$ -FDG microPET scans for determining therapy response and drug efficacy, the reproducibility of scans needs to be studied. The levels of variation in these scans must be known so that serial changes reflect therapy effects rather than changes related to mouse physiology and method variability. The purpose of this study was to determine the reproducibility of microPET scans with  $^{18}\text{F}$ -FDG in a mouse xenograft model. We show that the reproducibility has a moderately low variability, which would likely be useful in serial drug or therapy evaluation. Changes in blood glucose levels can affect  $^{18}\text{F}$ -FDG accumulation in tumors (5). Glucose can compete with  $^{18}\text{F}$ -FDG, resulting in the decrease of  $^{18}\text{F}$ -FDG tumor accumulation. Changes in blood glucose levels depend on many factors, such as mode of anesthesia and fasting duration (6,7). Therefore, the other purpose of this study was to assess the relationship between blood glucose levels and  $^{18}\text{F}$ -FDG tumor accumulation.

## MATERIALS AND METHODS

### Radiotracers

$^{18}\text{F}$ -FDG was supplied by PETNET Pharmaceuticals with high specific activity.

### Cell Culture

B16F10 murine melanoma cells were grown in Dulbecco's modified Eagle media with high glucose and L-glutamine (Invitrogen) supplemented with 10% fetal bovine serum and 1% penicillin

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(100 U/mL)/streptomycin (100  $\mu$ g/mL). Cells were harvested by trypsinization at approximately 90% confluence.

### Mouse Tumor Xenograft Model

Animal protocols were approved by the Stanford Administrative Panel on Laboratory Animal Care. Eighteen 10- to 12-wk-old female nude (*nu/nu*) mice (Charles River Laboratories) were injected in the shoulder region with 2 million B16F10 cells in 100  $\mu$ L of phosphate-buffered saline (PBS) using 28-gauge  $\frac{1}{2}$ -in. insulin syringes (Becton Dickinson). Mice were anesthetized with 2% isoflurane in 2 L/min oxygen during cell injection. The tumor xenografts grew for 1–2 wk. Tumors were measured externally with calipers, and the mean tumor diameter was 15 mm, with a range of 9–20 mm.

### microPET

An R4 microPET (Siemens Medical Solutions USA, Inc.) was used for imaging, which has an approximate resolution of 2 mm in each axial direction (8). After a tail vein injection of 3.7–7.4 MBq of  $^{18}\text{F}$ -FDG in 200  $\mu$ L of PBS, a 7-min prone acquisition scan was performed approximately 60 min after injection. Mice were maintained under isoflurane anesthesia during the injection, accumulation, and scanning periods. A heating pad, heat lamp, or hot water was used to dilate the tail veins for injections. A second scan was performed with a repeat injection of  $^{18}\text{F}$ -FDG approximately 6 h after the first injection. Six hours was chosen to allow for the activity from the first injection to decay for approximately 3–4 half lives. It was assumed that the tumor xenografts did not significantly change during the 6 h. Caliper tumor measurements were not significantly different between the 2 scans. Mouse body weight, tumor size, and rectal temperature were also recorded. Mice were fasted for 4 h before the first tracer injection. After the first scan, the mice recovered from anesthesia and were given access to food for 1 h. The mice were then fasted for 4 h before the second injection. Mice were kept warm using a heating pad or heat lamp while under anesthesia to maintain a body temperature of around 35°C.

microPET images were reconstructed with the ordered-subsets expectation-maximization algorithm (9) using 16 subsets and 4 iterations. No attenuation correction was applied, as an attenuation-corrected cylinder phantom study and an attenuation-correction scan performed with the body outline of a mouse using uniform attenuation both showed very little change in the activity profile across the mouse (10).

### Imaging Sessions

Eighteen mice were used for scanning. Five of the mice had 3 sets of studies performed. Ten mice had 1 set of studies performed. Twenty-five datasets were obtained. During the experiment 5 mice died. One scan could not be retrieved and, therefore, was excluded from analysis. In addition, we performed an additional microPET scan just before the second injection to determine the residual activity from the first injection in 7 of the mice.

### microPET Image Analysis

Ellipsoidal 3-dimensional regions of interest (ROI) were manually drawn around the edge of the tumor xenograft activity by visual inspection using AMIDE software (11). Because the positions and orientations of the mice and tumors were somewhat different between scans, separate ROIs were drawn for each scan. The mean and maximum activities were recorded from the entire ROI. The percentage injected dose per gram (%ID/g) was calcu-

lated as follows: %ID/g = ROI activity divided by injected dose multiplied by 100%. The standardized uptake value (SUV) was calculated as follows: SUV = ROI activity multiplied by mouse weight divided by injected dose. The coefficient of variation (COV) was calculated as the SD of the %ID/g (or SUV) of the first scan and repeat second scan divided by their mean %ID/g (or SUV). COV has been used as a statistical measure of absolute reliability (12). In addition, the intraclass correlation coefficient was calculated between scans.

### Delayed Scan Subtraction Method

For all mice, activity in the second 6-h scan was adjusted by subtracting the decay-corrected activity of the first scan. For 7 mice, an additional delayed scan was performed just before the second injection. The residual activity from this delayed scan was decayed and was then subtracted from the activity of the second scan. COVs of 2 subtraction methods were compared.

### Mouse Blood Glucose Measurements

Mouse blood glucose levels were measured from lateral tail vein pricks around the time of the  $^{18}\text{F}$ -FDG injection of 16 mice using an Ascensia Elite XL glucose meter (Bayer) and Glucometer Elite test strips (Fisher Scientific). In the case of a successful initial  $^{18}\text{F}$ -FDG injection, a tail vein prick was performed on the opposite side of the tail for the glucose measurement. In the case of a failure of  $^{18}\text{F}$ -FDG injection in the first attempt, blood that flowed out was used for glucose measurements, and an  $^{18}\text{F}$ -FDG injection was later given on the opposite side of the tail. One glucose measurement required approximately 3  $\mu$ L of blood. Depending on the volume of blood that flowed out by a tail vein prick, 1 or 2 glucose measurements were taken. In the case of 2 measurements, the average was used in the calculations.

### Reproducibility of Glucose Strips

The reproducibility of glucose measurements was tested by 2 methods. In the first method, 51.1 mg of D-glucose anhydrous was dissolved in 50 mL of distilled water, leading to a concentration of 102.2 mg/dL. Ten readings were taken. In the second method, 75  $\mu$ L of retroorbital blood were removed from a mouse, and 10 readings were taken. COVs were calculated for both methods.

### Glucose Correction Method

Glucose correction was applied to the %ID/g by normalizing to a value of 100 mg/dL as follows: Glucose corrected %ID/g = %ID/g multiplied by the glucose concentration divided by 100. COVs were calculated for the glucose corrected %ID/g and compared with the noncorrected values.

### Effect of Anesthesia on Blood Glucose Levels

Six female nude mice without xenografts were maintained under 3% isoflurane anesthesia in 2 L/min oxygen, and mouse blood glucose levels were measured via tail vein pricks at various time points up to 2 h. The blood glucose concentration was plotted against time.

### Statistical Analysis

Statistical analysis was performed using Excel 2002 (Microsoft). Data were reported as mean  $\pm$  SD. Paired *t* tests were used when comparing paired data from the same mouse. Correlation coefficients were calculated when assessing associations between datasets. A significance value of  $P < 0.05$  was used.

## RESULTS

### <sup>18</sup>F-FDG microPET Studies of B16F10 Mouse Xenografts

Tumor xenografts were clearly visible in the microPET images of all mice. The peripheries of the tumors were easily delineated for ROI placement on the images. The tumor volumes of the ROIs drawn around the tumor activity in the AMIDE software correlated well with the tumor volumes measured by calipers ( $R^2 = 0.7$ ; data not shown). Several tumors exhibited more intense activity at the periphery, suggesting higher metabolism compared with central areas of necrosis (Fig. 1).

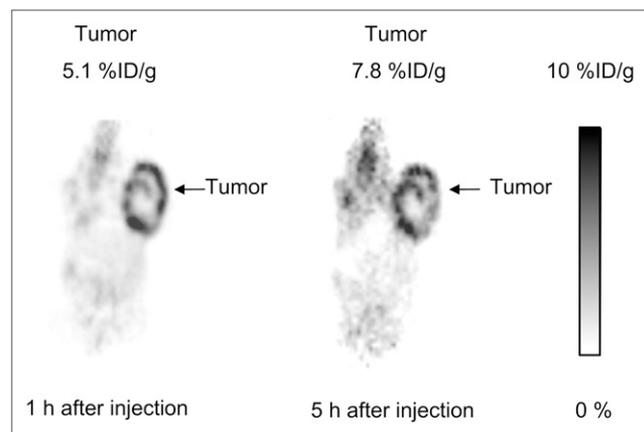
### Reproducibility of <sup>18</sup>F-FDG microPET Studies of B16F10 Mouse Xenografts

Twenty-five datasets were analyzed to assess the reproducibility of <sup>18</sup>F-FDG (Fig. 2). The COV for the mean %ID/g between <sup>18</sup>F-FDG microPET scans performed on the same day 6 h apart was  $15.4\% \pm 12.6\%$  (Table 1). The intraclass correlation coefficient between scans was 0.66. The mean %ID/g values of the first scans ( $5.6\% \pm 1.3\%$ ) and the second scans ( $5.8\% \pm 2.2\%$ ) were not significantly different ( $P = 0.44$ ). No significant correlations were seen between the COV and the parameters of body weight ( $R^2 = 0.02$ ), injected dose ( $R^2 = 0.02$ ), temperature ( $R^2 = 0.02$ ), or tumor size ( $R^2 = 0.004$ ).

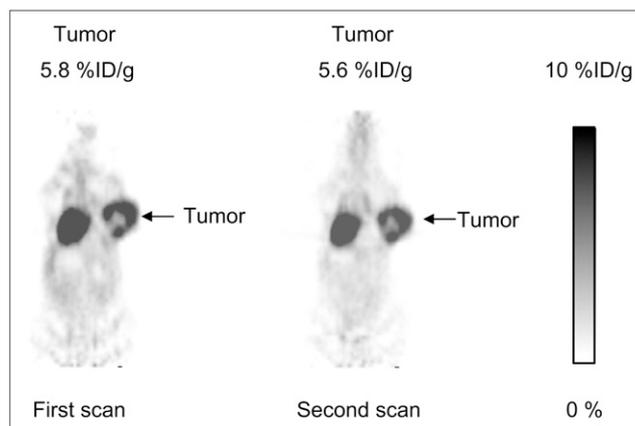
The COV for the mean SUV was  $15.1\% \pm 13.0\%$ , similar to the mean %ID/g value. The COVs for the maximum %ID/g and maximum SUV were  $18.0\% \pm 22.0\%$  and  $17.5\% \pm 22.4\%$ , respectively, which were both higher than the mean values.

### Effect of Delayed Scan Subtraction Method

The COV between the values of mean %ID/g of the 2 scans in 7 mice, using the delayed scan subtraction method, was  $13.9\% \pm 10.8\%$ , which was not significantly different



**FIGURE 1.** Coronal section of B16F10 nude mouse xenograft scan 1 h (left) and 5 h (right) after single <sup>18</sup>F-FDG injection using microPET to show change in tumor activity and tracer distribution over time. Both images are from a single mouse after a single injection of <sup>18</sup>F-FDG. This is mouse 5 in Table 2. Mean %ID/g values are shown adjacent to tumor xenograft. Note central photopenia consistent with central necrosis.



**FIGURE 2.** Coronal section of representative B16F10 nude mouse xenograft scan shows reproducibility of <sup>18</sup>F-FDG microPET. This is mouse 3 in Table 1. Initial first scan is shown (left), which is followed by repeat second scan 6 h later (right) after repeat second injection of <sup>18</sup>F-FDG. Mean %ID/g values are shown adjacent to tumor xenograft. Arrows point to tumor. Heart also shows high <sup>18</sup>F-FDG accumulation in both images.

from the COV obtained without the delayed scan, which was  $13.9\% \pm 11.8\%$  ( $P = 0.95$ ). Three mice had a slight increase in COV, whereas 4 mice had a slight decrease when using the delayed scan subtraction method. The %ID/g values calculated with the 2 different subtraction methods

**TABLE 1**  
COV in B16F10 Tumor Xenografts in Nude Mice Using Mean %ID/g from Repeat <sup>18</sup>F-FDG microPET Studies

Mouse no.	First scan Second scan		Mean	SD	COV
	(%ID/g)	(%ID/g)			
1	5.3	5.3	5.3	0.0	0.1
2	5.0	5.0	5.0	0.0	0.5
3	5.8	5.6	5.7	0.1	1.5
4	8.0	7.7	7.9	0.1	1.9
5	5.1	5.2	5.1	0.1	2.3
6	5.6	5.9	5.8	0.1	2.5
7	4.3	4.6	4.5	0.2	4.7
8	5.7	6.3	6.0	0.4	6.7
9	4.4	5.0	4.7	0.4	9.5
10	4.9	5.8	5.4	0.6	11.8
11	7.2	8.6	7.9	1.0	12.7
12	3.1	3.7	3.4	0.5	13.5
13	6.3	5.1	5.7	0.9	14.8
14	6.3	7.8	7.1	1.1	14.9
15	4.9	3.9	4.4	0.7	16.0
16	5.7	7.3	6.5	1.2	18.0
17	7.3	5.5	6.4	1.3	20.3
18	6.5	4.8	5.6	1.2	20.4
19	8.8	11.8	10.3	2.2	21.0
20	5.0	6.9	6.0	1.3	21.7
21	6.6	9.4	8.0	1.9	24.4
22	4.3	6.4	5.4	1.5	27.1
23	5.4	3.6	4.5	1.3	28.8
24	3.4	2.0	2.7	1.0	37.7
25	4.9	2.2	3.6	1.9	52.5
Mean $\pm$ SD	$5.6 \pm 1.3$	$5.8 \pm 2.2$			$15.4 \pm 12.6$

are provided in Supplemental Table 1 (supplemental tables are available online only at <http://jnm.snmjournals.org>).  $^{18}\text{F}$ -FDG accumulation in the tumors changed over time. In the third dataset, the mean %ID/g of the first scan and the delayed scan (without repeat tracer injection) in 7 mice were compared (Fig. 1). One mouse showed a decrease in the  $^{18}\text{F}$ -FDG accumulation, whereas the other 6 showed increases (Table 2). Overall the %ID/g increased by 2.1 %ID/g, which was a statistically significant finding ( $P = 0.04$ ) and was consistent with the fact that  $^{18}\text{F}$ -FDG accumulation generally increased over time in most of these tumors.

### Reproducibility of Glucose Strips

The reproducibility of the glucose strips was tested by 2 methods. In the first method, 10 readings were taken from a 102.2-mg/dL solution of glucose in water, and the COV of the strips was found to be 3.8%. In the second method, a retroorbital blood sample was tested, and the COV was 4.7%. In both methods, the COVs were similar to the COV from the package insert of the glucose strips, which was listed as 4.0%.

### Glucose Correction Method

Mouse blood glucose levels were measured around the time of the  $^{18}\text{F}$ -FDG injections. The mean blood glucose level for the first injection was  $91.3 \pm 25.3$  mg/dL (range, 53–134 mg/dL). The mean glucose level for the second injection 6 h later was  $58.1 \pm 20.1$  mg/dL (range, 27–104 mg/dL). There was a significant difference in the glucose values between the first and second injections ( $P = 0.0005$ ). No significant correlation was found between the glucose levels and the %ID/g ( $R^2 = 0.05$ ), and no correlation was found between the change in glucose levels compared with the change in %ID/g between the first and second scans ( $R^2 = 0.007$ ).

The glucose correction method was applied to data from 16 mice. We expected that applying the glucose correction to the %ID/g would decrease the COV. In contrast, the COV increased from  $16.2\% \pm 14.4\%$  to  $37.2\% \pm 30.7\%$  ( $P = 0.007$ ) after application of glucose correction.

**TABLE 2**

Comparison Between Tumor Mean %ID/g of Initial 1-Hour Scan and Delayed 5-Hour Scan to Reveal Change in %ID/g Over Time

Mouse no.	Initial scan (mean %ID/g)	Delayed scan (mean %ID/g)	Increase or decrease
2	5.0	5.9	Increase
5	5.1	7.8	Increase
7	4.3	5.9	Increase
12	3.1	6.5	Increase
18	6.5	4.7	Decrease
22	4.3	8.5	Increase
23	5.4	8.7	Increase
Mean $\pm$ SD	$4.8 \pm 1.0$	$6.9 \pm 1.5$	

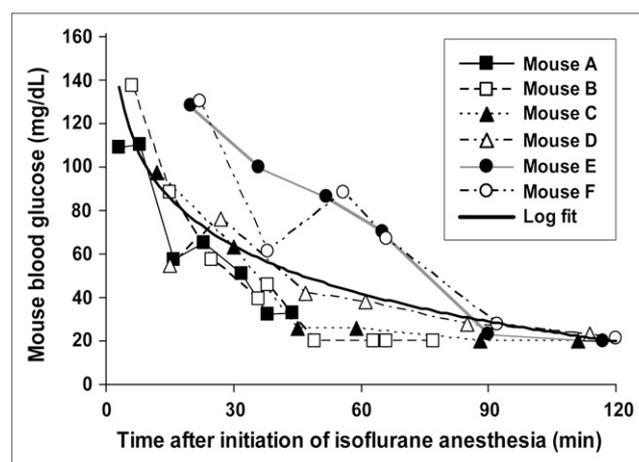
### Effect of Anesthesia on Glucose Levels

The effect of 3% isoflurane anesthesia over time on the mouse blood glucose levels was measured. The blood glucose concentration was plotted against time over 2 h (Fig. 3). Blood glucose values decreased over the first hour and remained very low over the second hour.

### DISCUSSION

We determined the reproducibility of  $^{18}\text{F}$ -FDG microPET scans for B16F10 tumor xenografts in nude mouse. The COV for the mean %ID/g was found to be  $15.4\% \pm 12.6\%$ . The  $^{18}\text{F}$ -FDG microPET studies were found to be reproducible with a moderately low variability. We recently reported a similar finding for 3'-deoxy-3'- $^{18}\text{F}$ -fluorothymidine ( $^{18}\text{F}$ -FLT) microPET scans, in which the COV was  $14\% \pm 10\%$  (10). Taken together, the reported variabilities suggest that small changes ( $<15\%$ ) on serial scans used to assess therapy are not likely reliable to indicate changes due to therapy in a single mouse. Larger changes are required to indicate a significant effect in assessing therapy response. However, if a larger number of animals were used in a therapy trial, then smaller changes may indicate a significant change due to therapy.

The variability of our animal  $^{18}\text{F}$ -FDG microPET studies was somewhat higher than the reported variabilities for human  $^{18}\text{F}$ -FDG PET studies, which ranged from 6% to 10% (13,14). The difference in variabilities highlights some of the difficulties in working with small animals. Several factors have been investigated that contribute to the variability, including anesthesia, fasting state, and temperature (6,7,10), which can be more difficult to regulate in animals. Variations in ROI placement were investigated in our previous study and found to be small when the analysis was performed by a single person (10).



**FIGURE 3.** Effect of isoflurane anesthesia on mouse blood glucose levels. Mouse blood glucose levels are plotted as function of time for 6 mice sampled at various times points after initiation of 3% isoflurane anesthesia. Composite logarithmic (log) fit is also displayed (solid black curve).

One factor that required more investigation was the effect of blood glucose levels on the variability of scans. Wahl et al. reported that rat xenografts under extreme hyperglycemic conditions ( $>500$  mg/dL) had significantly decreased  $^{18}\text{F}$ -FDG tumor accumulation, suggesting competition between glucose and  $^{18}\text{F}$ -FDG; however, only small changes were seen in some normal tissues, such as liver, heart, muscle, and fat (5). Nakamoto et al. found that applying a glucose correction to human  $^{18}\text{F}$ -FDG PET scans by normalizing to a glucose value of 100 mg/dL reduced the variability from 10.1% to 6.7% (13). When we applied a similar glucose correction to our studies, we found the opposite effect—namely, the COV increased from 16.2% to 37.2%. Our measured glucose value varied widely from as low as 27 mg/dL to as high as 134 mg/dL. This large range resulted in large correction factors being applied to the COV for the glucose corrected values compared with the noncorrected values. We also found that the blood glucose values were lower after the second injection; however, the %ID/g values were not significantly different between the 2 scans. This suggests that competition between glucose and  $^{18}\text{F}$ -FDG may not be the only factor affecting the %ID/g value in our studies.

Several factors may contribute to the variability in glucose values. Isoflurane anesthesia was found to alter the mouse glucose concentrations over time. By measuring glucose values in 6 mice over a period of 2 h, the glucose values dropped considerably from a normal range around 100 mg/dL to values around 20 mg/dL (Fig. 3). This is in contrast to Fueger et al., who revealed a modest increase in blood glucose with isoflurane anesthesia from 73 to 104 mg/dL (7). Possible explanations for the difference may include differences in mouse type, tumor type, or mouse handling. They also reported that isoflurane anesthesia slightly decreased tumor SUV from  $1.8 \pm 0.6$  to  $1.60 \pm 0.47$ , but the SUVs do not appear to be significantly different when inspecting the SD value. We have preliminary data showing mildly decreased tumor accumulation with isoflurane anesthesia, suggesting that anesthesia may influence  $^{18}\text{F}$ -FDG accumulation, perhaps due to decreased metabolism during anesthesia. Studies of Lee et al. have shown that injectable anesthetics, such as xylazine, ketamine, or pentobarbital, can have large effects on blood glucose levels and  $^{18}\text{F}$ -FDG accumulation in tumors (6).

An additional factor that is difficult to control is the effect of stress on glucose levels. Several reports, summarized by Balcombe et al. (15), indicate that differences in the handling of animals (e.g., movement of cages, cage changing, physical contact with animals, and blood collection) can lead to wide variations in glucose levels. In addition, there are inherent difficulties in measuring glucose levels around the time of injection due to difficulties associated with tail vein injection. This may also contribute to the variability in glucose values.

Maintaining and measuring a consistent glucose level can be a difficult task in a mouse. Further studies into the

factors affecting glucose levels are necessary to better understand the complex relationship among such factors as anesthesia, glucose levels, and  $^{18}\text{F}$ -FDG accumulation. Use of intravenous catheters would be helpful to attain more consistent blood glucose measurements, and rigorous methodology controls are needed to minimize the variations in blood glucose and to account for the multiple factors that can affect  $^{18}\text{F}$ -FDG accumulation. In addition, use of slower growing tumors and a separate-day protocol may be investigated to reduce the frequency of anesthesia exposure. Measurement of  $^{18}\text{F}$ -FDG blood activity and tissue biodistribution may also help clarify some of these issues. Overall, we have developed a protocol to expose animals to the same length and type of anesthesia and to minimize stress to the animals with gentle handling to minimize variations between animals. In our hands, we have shown that despite wide ranges in measured glucose values, moderately low variability can be achieved by adherence to a strict protocol.

### Limitations

The accuracy of the %ID/g of the second scan performed 6 h after the first scan relies on the accuracy with which this residual activity from the first scan is subtracted from the second scan (10). For a subset of 7 mice, we performed a delayed scan after the first injection and used that to subtract the residual activity hoping to achieve an improvement in the COV. Although the mean %ID/g increased in the delayed scan for most mice, the COV was  $13.9\% \pm 10.8\%$ , which was not significantly different from the COV obtained without the delayed scan, which was  $13.9\% \pm 11.8\%$ . In our previous study with  $^{18}\text{F}$ -FLT microPET in 4 mice, the COV improved from  $9.2\% \pm 6.7\%$  to  $4.9\% \pm 5.4\%$  with the delayed scan method (7). Possible explanations may include difference in the tracer kinetics, tumor types, or the smaller sample size. Overall, the residual activity from the first scan is small after 3–4 half lives, such that the contribution to the variability should be very modest.

The COV was calculated using only 2 data points. Additional data points would be helpful to better delineate the COV; however, tumors continue to grow such that additional scanning would likely be confounded by changes in the tumor metabolism unless slower-growing tumors can be used. Our choice of a single-day protocol using a 6-h delay between scans was a compromise between the changing tumor volume versus the use of anesthesia and fasting twice in the same day. We did see a difference between the glucose values between the 2 scans that may be related to the fasting conditions or anesthesia; however, a simple relationship between the glucose values and the FDG accumulation could not be determined even with a glucose correction factor. Fasting conditions and anesthesia exposures likely affect the FDG accumulation; however, the exact relationship cannot be completely explained from our data. The use of a slower-growing tumor and a separate-day protocol may be helpful to reduce the overall variability and to further investigate the influence of different fasting conditions

and anesthesia exposures on FDG accumulation. A separate-day protocol may more closely mimic serial therapeutic response studies performed on separate days.

Future studies will also benefit from exploring other tumor lines as well as other xenograft locations on the mouse to determine if the results reported here generalize further. Studies that determine the blood time–activity curve for  $^{18}\text{F}$ -FDG may also lead to lower variation as compared with the current approach of quantifying only with the %ID/g or SUV.

## CONCLUSION

$^{18}\text{F}$ -FDG microPET mouse xenograft studies are reproducible with moderately low variability. Blood glucose corrections did not lead to an improvement in the variability; however, close monitoring of glucose levels and anesthesia exposure would be helpful for FDG microPET studies to further evaluate the influence of these variables on FDG accumulation. Overall, the level of variability seen in this study is sufficiently small for reasonable assessments of serial changes. These results may be applied to follow tumor therapy response, including preclinical drug evaluation.

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