

immunoscintigraphy. Tricot et al. (26) described the dislocation of immature granulopoietic cells during myelodysplastic syndrome, including blasts in the bone marrow, as an abnormal localization of immature precursors (ALIP). They also reported that ALIP is an adverse prognostic finding that is very accurate in predicting which patients will have a short survival time and which will have early transformation to acute leukemia (26,27). We expect that the immunoscintigraphic technique described here can provide useful information to diagnose and classify this complex syndrome.

In the myelogenous leukemia patients, myelocytes expressed NCA-95 to a variable degree, and normal or increased uptake of the anti-NCA-95 antibody was observed in all four patients. Of course, because of the lack of lymphoid cell binding sites, there was markedly decreased uptake in acute lymphocytic leukemia subjects.

In patients with other disorders, such as iron deficiency anemia, pure red cell aplasia, thalassemia minor and Evan's syndrome, immunoscintigraphy revealed bone marrow expansion. Peripheral bone marrow expansion can also be evaluated with bone-seeking radiopharmaceuticals (1). Findings of marrow expansion in ^{99m}Tc-labeled phosphate bone scans are not specific or clear. In comparison, the immunoscintigraphy protocol described in this article provides more precise images and can be used to evaluate bone marrow functional states.

CONCLUSION

Until now, immunoscintigraphy with antigranulocyte antibody has been used to detect bone marrow metastasis and to localize inflammation (10,11,28,29). This preliminary report suggests that it may also be effectively used to evaluate the functional status of bone marrow during disease and treatment.

ACKNOWLEDGMENTS

We thank Ms. Mee Kyoung Hong and Ms. Sun Ho Lee of the Department of Nuclear Medicine, Seoul National University Hospital, for their excellent technical support, and Ms. Jung Hee Choi for administrative assistance. This study was supported in part by a grant from the Cancer Research Center of the Korea Scientific and Engineering Foundation (KOSEF SRC-56-CRC-94K3-1601-02-02-3).

REFERENCES

1. Fordham EW, Ali A. Radionuclide imaging of bone marrow. *Semin Hematol* 1981;18:222-239.
2. Padhy AK, Garg A, Kochupillai V, Gopinath PG, Basu AK. Marrow uptake index: a quantitative scintigraphic study of bone marrow in aplastic anemia. *Thymus* 1987;10:137-146.
3. Greenberg ML, Atkins HL, Schiffer LM. Erythropoietic and reticuloendothelial function in bone marrow in dogs. *Science* 1966;152:526-528.

4. Farrer PA, Saha GB, Kalz M. Further observation of the use of indium 111-transferrin for the visualization of bone marrow in man. *J Nucl Med* 1973;14:394-395.
5. McNeil BJ, Holman BL, Button LN, et al. Use of indium-chloride scintigraphy in patients with myelofibrosis. *J Nucl Med* 1974;15:647-651.
6. Chaudhri TK, Ehrhardt JC, DeGowin RL, et al. Ferrous-59 whole-body scanning. *J Nucl Med* 1974;15:667-673.
7. Knospe WH, Rayudu GV, Cardello M, et al. Bone marrow scanning with iron-52. Regeneration and extension of marrow after ablative doses of radiotherapy. *Cancer* 1976;37:1432-1442.
8. Steintraesser A, Schorlemmer HU, Schwarz A, Kuhlmann L, Bosslet K. A novel ^{99m}Tc-labeled antibody for in vivo targeting of granulocyte. *J Nucl Med* 1988;29:925.
9. Choi CW, Chung J-K, Lee DS, Lee MC, Chung H-K, Koh C-S. Development of bone marrow immunoscintigraphy using a ^{99m}Tc-labeled anti-NCA-95 monoclonal antibody. *Nucl Med Biol* 1995;22:117-123.
10. Reske SN, Karstens JH, Gloeckner MW, Schwarz A, Steintraesser A, Ammon J, Buell U. Radioimmunoimaging of bone marrow. Results in patients with breast cancer and skeletal metastases and patients with malignant melanoma. *Lancet* 1989;2:299-301.
11. Duncker CM, Carrio I, Berna L, et al. Radioimmune imaging of bone marrow in patients with suspected bone metastases from primary breast cancer. *J Nucl Med* 1990;31:1450-1455.
12. Lee KH, Choi CW, Bang YJ, et al. Bone marrow immunoscintigraphy for the detection of skeletal metastases in malignant tumors: a comparison with ^{99m}Tc-MDP bone scan. *Kor J Nucl Med* 1994;28:89-97.
13. Lee J-H, Chung H-K, Kimm S-W. Purification of carcinoembryonic antigen from culture supernatant of human colon cancer cell line LS174T using monoclonal immunoaffinity chromatography. *Kor J Biochem* 1988;20:23-32.
14. Lilien DL, Berger HG, Anderson DP, et al. Indium-111-chloride: a new agent for bone marrow imaging. *J Nucl Med* 1973;14:184-186.
15. McNeil BJ, Rapoport JM, Nathan DG. Indium chloride scintigraphy: an index of severity in patients with aplastic anemia. *Br J Haematol* 1976;34:599-604.
16. Mishkin FS, Freeman LM. Miscellaneous applications of radionuclide imaging. In: Freeman LM, ed. *Freeman and Johnson's clinical radionuclide imaging*, 3rd ed. Orlando: Grune & Stratton; 1984:1365-1460.
17. McIntyre RA, Larson SM, Scheffel U, et al. Comparisons of metabolism of iron-transferrin and indium-transferrin by erythropoietic marrow. *J Nucl Med* 1973;14:425-426.
18. Staub RF, Gorston E. Indium-111-chloride distribution kinetics in hematologic disease. *J Nucl Med* 1973;14:456-457.
19. Joseph K, Hoeffken H, Bosslet K, Schorlemmer HU. In vivo labeling of granulocytes with ^{99m}Tc anti-NCA monoclonal antibodies for imaging inflammation. *Eur J Nucl Med* 1988;14:367-373.
20. Berna L, Germa JR, Estorch M, Torres G, Blanco R, Carrio I. Bone marrow regeneration after hormonal therapy in patients with bone metastases from prostate carcinoma. *J Nucl Med* 1991;32:2295-2298.
21. Najean Y, Le Danvic M, Le Mercier N, Pecking A, Colonna P, Rain JD. Significance of bone marrow scintigraphy in aplastic anemia: concise communication. *J Nucl Med* 1980;21:213-218.
22. Sayle BA, Helmer III RE, Birdsong BA, Balachandran S, Gardner FH. Bone marrow imaging with indium-111-chloride in aplastic anemia and myelofibrosis: concise communication. *J Nucl Med* 1982;23:121-125.
23. Hotta T, Murate T, Inoue C, et al. Patchy haemopoiesis in long-term remission of idiopathic aplastic anemia. *Eur J Haematol* 1990;45:73-77.
24. Gordon MY, Gordon-Simth EC. Bone marrow fibroblastoid colony-forming cells (F-CFC) in aplastic anemia: colony growth and stimulation of granulocyte-macrophage colony forming cells (GM-CFC). *Br J Haematol* 1981;49:465-477.
25. Reske SN. Recent advances in bone marrow scanning. *Eur J Nucl Med* 1991;18:203-221.
26. Tricot G, Do Wolf-Peters C, Vlietinck R, et al. Bone marrow histology in myelodysplastic syndromes: II. Prognostic value of abnormal localization of immature precursors in MDS. *Br J Haematol* 1984;58:217-225.
27. Tricot G, Vlietinck R, Verwilghen RL. Prognostic factors in the myelodysplastic syndromes: a review. *Scand J Haematol* 1986;36 (suppl 45):107-113.
28. Locher JT, Seybold RY, Andres PA, Schubiger JP, Mach F. Imaging of inflammatory and infectious lesions after injection of radioiodinated monoclonal anti-granulocyte antibodies. *Nucl Med Commun* 1986;7:659-670.
29. Seybold K, Locher JT, Coosemans C, et al. Immunoscintigraphic localization of inflammatory lesions: clinical experience. *Eur J Nucl Med* 1988;13:587-593

EDITORIAL

Noninvasive Evaluation of the Bone Marrow

The study reported by Chung et al. (1) in this issue reflects the evolution of sophisticated, noninvasive tech-

nology for the evaluation of bone marrow anatomy, function and disease. Such methods offer the major advantage of visualizing the entire marrow, or at least a major portion of the bone marrow, as compared to the small sampling obtained by bone marrow aspiration and biopsy. Each of these new technologies, however, has its own shortcomings that limit

it as a sole method of studying the marrow. Such methods alone are not likely to replace bone marrow aspiration or biopsy and pathologic review. In combination, however, they may offer complementary information to the aspirate and biopsy and to each other, and help to improve patient management. There are two major methods of noninvasively studying the

Received Dec. 14, 1995; accepted Dec. 15, 1995.
For correspondence or reprints contact: David A. Scheinberg, MD, PhD, Leukemia Service, Division of Hematologic Oncology, Memorial Sloan-Kettering Cancer Center, 1275 York Ave., New York, NY 10021.

bone marrow: (a) MRI and spectroscopy and (b) radiopharmaceuticals.

Nuclear magnetic resonance (NMR) imaging utilizes the difference in proton relaxation properties (T1 and T2 relaxation times) of fat and water (cells) to create a map of the cellularity of the bone marrow. It thus provides an assessment of its *anatomy* (2). Patterns of bone marrow disorders that can be evaluated by MRI include recruitment of fatty marrow by increased demand for hematopoiesis, marrow infiltration or replacement with leukemia, metastases, etc. and bone marrow failure (iatrogenic or spontaneous) resulting in loss of cellularity and increase in fat. Some investigators (3) have even suggested that particular patterns of cellular distribution in hypocellular marrows (homogenous versus heterogeneous) may be helpful in distinguishing, for example, aplastic anemia from hypoplastic myelodysplastic syndrome. MRI offers the advantage of being sensitive, though nonspecific for pathology, and it can assess a much larger sample than can be studied by the usual invasive techniques. MRI has become the technique of choice for imaging selected regions of the bone marrow.

NMR spectroscopy can be used as an adjunct to MRI to obtain information, noninvasively, about the intracellular metabolites of a biologic sample. Although it has not been well utilized in studies of the bone marrow, and is still considered investigational, it can potentially provide information about the *biochemistry* and *physiology* of the marrow. Such spectroscopic studies have been performed in vivo on the brain and breast and in vitro using leukemic cell lines to determine differences in normal and malignant tissue, as well as between mature and immature cells, respectively (4). Jansen et al. (5) even reported differences in T1 relaxation times of the water spectrum in vivo for leukemic versus normal marrow. Both the imaging and spectroscopic techniques require specialized equipment and training.

Radionuclide imaging of the bone marrow targets specific cellular components of the normal bone marrow. It can be divided into three categories: (a) erythroid, (b) macrophage/histiocytic (RES) and (c) myeloid. The earliest studies of bone marrow utilized ^{52}Fe , a positron-emitting isotope, and ^{59}Fe , a long-lived, high-energy photon emitter. Both are incorporated into the erythroid precursors. Their utility has been limited by the equipment required to generate or analyze the isotope, the cost, and, in the case

of ^{59}Fe , the radiation exposure to the marrow. Although PET is becoming more widely available, production of the appropriate isotope is still difficult. The RES has been visualized previously by ^{198}Au and more recently with $^{99\text{m}}\text{Tc}$ -colloid. The colloid particles attach to the membrane of the cell, are then endocytosed and degraded by the lysosomes within the cell. Because these particles are distributed predominantly to the Kupffer cells of the liver and the phagocytic cells of the spleen and in much smaller amounts to the RES of the marrow, uptake in the marrow is relatively reduced. In addition, visualization of the lumbar and thoracic spine is impaired because of the high hepatosplenic uptake. Anatomic patterns change significantly with underlying systemic hematologic conditions, neoplastic hematologic disorders and tumor infiltration (6). The development of $^{99\text{m}}\text{Tc}$ -labeled nanocolloid has resulted in higher concentrations of particles localizing to the bone marrow compared to the conventional colloids, but limitations to visualization are similar.

Technetium-99m-labeled monoclonal antibodies, such as the NCA-95 antibody described by Chung et al., have been developed recently to target the myeloid elements of the bone marrow and peripheral blood. The NCA-95 antibody, under clinical investigation, binds to the target cells by interacting with the nonspecific cross-reacting antigen 95 (NCA-95) (7). This antigen is expressed on the membrane of granulocytes and other myeloid precursors. Other myeloid antibodies such as M195, p67 and a genetically engineered humanized version, HuM195 (all directed against the CD33 antigen), bind to myeloblasts and early myeloid precursors, but not to mature granulocytes. The anti-CD33 antibodies rapidly target leukemia cells throughout the marrow, liver and spleen (8,9); when labeled with ^{131}I these antibodies can be used to characterize biodistribution of leukemia cells and to quantitate target cells (10). When labeled with modest amounts of ^{131}I (80–140mCi), this targeting may reduce residual leukemia cells in patients in clinical remissions. Dosimetry modeling has revealed significant heterogeneity of uptake within the marrow (11). When labeled with larger amounts of ^{131}I (200–360mCi), the entire marrow, normal and neoplastic cells as well, can be ablated (8,12). Such cytoreduction may be applicable to pre-bone marrow transplantation preparation.

A major advantage to using the anti-

body as a carrier for the $^{99\text{m}}\text{Tc}$ is its specificity for hematopoietic elements. Like MRI, classic scintigraphy, using radioactive nuclides or nuclides attached to carriers, antibody targeting is most useful in providing information about the *anatomy* of the marrow. Its limitations lie in the distribution of the antigen to which the antibody has been developed and its value will most likely be as a tool for monitoring a disease or localizing a site for an invasive procedure. For example, marrow replaced by acute myelogenous leukemia may appear “falsely” hypocellular if the radiolabeled antibody used is expressed only on maturing myeloid cells; a hypoplastic bone marrow due to aplastic anemia may appear the same as that due to a hypoplastic myelodysplastic syndrome, or a hypoplastic phase preceding the development of full blown hairy cell leukemia or acute lymphocytic leukemia. On the other hand, an antibody targeting myeloblasts may prove useful in following patients in remission and in diagnosing early relapse. Conversely, bone marrow involvement by solid tumors allows detection by demonstrating photopenic areas.

Finally, PET, which also relies on selective accumulation of administered radiolabeled materials, has been developed to study functional and metabolic changes in normal and abnormal tissue. Because of the physics of positron emission and detection, its performance in diagnosing malignancy has been found superior to that of CT and MRI, with sensitivity *and* specificity greater than 90% in the detection of some tumors. Like NMR spectroscopy, it focuses on differences in the biochemistry and metabolism of normal and diseased tissue (13,14). Dahlbom et al. (15) have recently developed a whole-body PET method that permits evaluation of the entire body, and have opened the door to broader applications in hematology and assessment of bone marrow. Its application, unfortunately, has been limited by cost and the availability of equipment and labeled radiotracers.

Noninvasive imaging and spectroscopic techniques for the marrow are still in their infancy. Therefore, carefully conducted clinical studies that include correlation between the results of imaging and the reference standard—bone marrow aspiration and biopsy—are critical to the definition of their utility in hematology and oncology. As these noninvasive methods become more sophisticated, as they are used in combination and as

larger databases are developed, the need for the invasive procedures may lessen.

Ann Jakubowski
David A. Scheinberg

Leukemia and Clinical Immunology Services
Memorial Sloan-Kettering Cancer Center
New York, New York

REFERENCES

1. Chung JK, Yeo J, Lee DS, et al. Bone marrow immunoscintigraphy using ^{99m}Tc -labeled antigranulocyte antibody in hematologic disorders. *J Nucl Med* 1996;37:948-952.
2. Vogler JB, Murphy WA. Bone marrow imaging. *Radiology* 1988;168:679-693.
3. Negendank W, Weisman D, Bey TM, et al. Evidence for clonal disease by magnetic resonance imaging in patients with hypoplastic marrow disorders. *Blood* 1991;78:2872-2879.
4. Agris PF, Campbell ID. Proton nuclear magnetic resonance of intact friend leukemia cells; phosphorylcholine increase during differentiation. *Science* 1982;216:1325-1327.
5. Jensen KE, Jensen M, Grundtvig P, et al. Localized in vivo proton spectroscopy of the bone marrow in patients with leukemia. *Magnetic Resonance Imaging* 1990;8:779-789.
6. Larson SM, Nelp WB. The radiocolloid bone marrow scan in malignant disease. *J Surg Oncol* 1971;3:685-697.
7. Choi CW, Chung JK, Lee DS, et al. Development of bone marrow immunoscintigraphy using a ^{99m}Tc -labeled anti-NCA-95 monoclonal antibody. *Nucl Med Biol* 1995;22:117-123.
8. Appelbaum FR, Matthews DC, Eary JF, et al. The use of radiolabeled anti-CD33 antibody to augment marrow irradiation prior to marrow transplantation for acute myelogenous leukemia. *Transplantation* 1992;54:829.
9. Caron PC, Jurcic JG, Scott AM, et al. A Phase IB trial of humanized monoclonal antibody M195 (Anti-CD33) in myeloid leukemia: specific targeting without immunogenicity. *Blood* 1994;7:1760-1768.
10. Sgouros G, Graham MC, Divgi CR, et al. Modeling and dosimetry of monoclonal antibody M195 (Anti-CD33) in acute myelogenous leukemia. *J Nucl Med* 1993;34:422-430.
11. Jurcic JG, Caron PC, Miller WH Jr, et al. Sequential targeted therapy for relapsed acute promyelocytic leukemia with all-trans retinoic acid and anti-CD33 monoclonal antibody M195. *Leukemia* 1995;9:244-248.
12. Schwartz MA, Lovett DR, Redner A, et al. Dose escalation trial of ^{131}I -M195 (Anti-CD33) for cytoreduction and marrow ablation in relapsed or refractory myeloid leukemias. *J Clin Oncol* 1993;11:294-303.
13. Glaspy JA, Hawkins R, Hoh CK, et al. Use of positron emission tomography in oncology. *Oncology* 1993;7:41-50.
14. Larson SM. Positron emission tomography in oncology and allied diseases. In: Devita VT, Hellman S, Rosenberg SA, eds. *Cancer, principles and practice of oncology*, 2nd ed. Philadelphia: JB Lippincott; 1989:1-12.
15. Dahlbom M, Hoffman EJ, Hoh CK, et al. Evaluation of a positron emission tomography scanner for whole-body imaging. *J Nucl Med* 1992;33:1191-1199.

FDG-PET to Evaluate Response to Hyperthermic Isolated Limb Perfusion for Locally Advanced Soft-Tissue Sarcoma

Robert J. van Ginkel, Harald J. Hoekstra, Jan Pruijm, Omgo E. Nieweg, Willemina M. Molenaar, Anne M.J. Paans, Antoon T.M. Willemsen, Willem Vaalburg and Heimen Schraffordt Koops
Department of Surgical Oncology, PET Center and Department of Pathology, University Hospital Groningen, The Netherlands; and Department of Surgery, The Netherlands Cancer Institute, Amsterdam, The Netherlands

We investigated FDG-PET in patients undergoing hyperthermic isolated limb perfusion (HILP) with rTNF- α , rIFN- γ and melphalan for locally advanced soft-tissue sarcoma of the extremities. **Methods:** Twenty patients (11 women, 9 men; aged 18-80 yr, mean age 49 yr) were studied. FDG-PET studies were performed before, 2 and 8 wk after HILP. After the final PET study, the tumor was resected and pathologically graded. Patients with pathologically complete response (pCR) showed no viable tumor after treatment. Those with pathologically partial response (pPR) showed various amounts of viable tumor in the resected specimens. **Results:** Seven patients showed a pCR (35%) and 12 patients showed a pPR (60%). In one patient, pathological examination was not performed (5%). The pre-perfusion glucose consumption in the pCR group was significantly higher than in the pPR group ($p < 0.05$). Visual analysis of the PET images after perfusion showed a rim of increased FDG uptake around a core of absent FDG uptake in 12 patients. The rim signal contained a fibrous pseudocapsule with inflammatory tissue in the pCR group, viable tumor was seen in the pPR group. The glucose consumption in the pCR group at 2 and 8 wk after perfusion had decreased significantly ($p < 0.05$) in comparison to the glucose consumption in the pPR. **Conclusion:** Based on the pretreatment glucose consumption in soft-tissue sarcomas, one could predict the probability of a patient achieving complete pathological response after HILP. FDG-PET indicated the pathologic tumor response to HILP, although the lack of specificity of FDG, in terms of differentiation between an inflammatory response and viable tumor tissue, hampered the discrimination between pCR and pPR.

Received May 22, 1995; revision accepted Nov. 7, 1995.

For correspondence or reprints contact: Harald J. Hoekstra, MD, PhD, Division of Surgical Oncology, Department of Surgery, Groningen University Hospital, PO Box 30.001, 9700 RB Groningen, The Netherlands.

Key Words: fluorine-18-fluorodeoxyglucose; PET; hyperthermic isolated limb perfusion; tumor necrosis factor; sarcoma

J Nucl Med 1996; 37:984-990

Malignant soft-tissue sarcomas are a heterogeneous group of lesions that all arise from tissue of mesenchymal origin and are characterized by aggressive local growth and hematogenic metastases. They account for 1% of all malignant tumors and have an incidence rate of 2 per 100,000. About 60% of these tumors occur in the extremities and are often quite large at diagnosis (1). Limb-saving treatment of extremity soft-tissue sarcomas is a multidisciplinary matter, with surgery and radiotherapy as the usual treatment protocol (2,3). This combination therapy has avoided ablative surgical procedures in the majority of patients.

The majority of locally advanced extremity soft-tissue sarcomas are treated by amputation. Intra-arterial chemotherapy with adriamycin, combined with preoperative radiotherapy, surgery and postoperative radiotherapy is effective in the treatment of locally advanced soft-tissue sarcoma, but significant morbidity does occur (4). Recently Eilber et al. (5) reported a complete response rate of 49% and a limb-saving rate of 98% with neo-adjuvant chemotherapy and radiation for high-grade extremity soft-tissue sarcoma with low-treatment morbidity. Hyperthermic isolated limb perfusion (HILP) also proved to be of value in the treatment for locally advanced extremity soft-tissue sarcoma (6-8). With HILP, chemotherapeutic tissue concentrations may be up to 20 times higher than can be attained with systemic administration (9). The intro-