to estimate the number of projections required gives $N = \pi .200/(16/2)$, approximately 78 projections over 360° or half that number over 180°. This suggests that the number of projections should be greater than the 32 commonly used, although use of 64 projections over 180° is overkill (48 angles might be considered ideal). Note that the number of angles has no direct relationship to the matrix size chosen or zoom factor used for either acquisition or reconstruction, contrary to some authors' discussions (2-5).

2. For brain studies, the region of diagnostic interest tends to be located centrally. Therefore, in this case, the value for D does correspond to the dimension of the brain, typically 160 mm. Reconstructed resolution for brain studies is significantly better than that for cardiac studies and can be as low as 8 mm. Therefore, with a camera of 400-mm field size, a 128 × 128 matrix size is required to preserve resolution. The number of angles required is N = π.160/(8/2), approximately 125 angles over 360°. This is consistent with common practice. Note again that this is independent of the matrix size chosen; a zoomed acquisition using a smaller matrix size still requires the same number of projection angles.

The choice of angular sampling is frequently misunderstood and rarely appreciated. The discussion and illustration presented here, although intuitive, appears consistent with more rigorous descriptions and should assist readers in deciding what protocols are appropriate for any applications.

REFERENCES

- Rosenthal MS, Cullom J, Hawkins W, Moore SC, Tsui BMW, Yester M. Quantitative SPECT imaging: a review and recommendations by the focus committee of the Society of Nuclear Medicine Computer and Instrumentation Council. J Nucl Med 1995;36: 1489-1513.
- Bracewell RN, Riddle AC. Inversion of fan-beam scans in radio astronomy. Astrophys J 1967;150:427.
- Snyder DL, Cox JR. An overview of reconstruction tomography and limitations imposed by a finite number of projections. In: Reconstruction tomography in diagnostic radiology and nuclear medicine. University Park Press; 1977:3.
- Huesman RH. The effects of a finite number of projection angles and finite lateral sampling of projections on the propogation of statistical errors in transverse section reconstruction. Phys Med Biol 1977;22:511-521.
- 5. Larsson SA. Gamma camera emission tomography. Acta Radiol 1980;363(suppl):21-
- Bailey DL, Parker JA. Single-photon emission computerized tomography. In: Murray IPC, Ell PJ, eds. Nuclear medicine in clinical diagnosis and treatment, vol. 2. Edinburgh: Churchill Livingstone; 1994:1315-1326.

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Carbon-14-Urea Breath Test: A Cautionary Note

TO THE EDITOR: We currently perform about 75 ¹⁴C-urea breath tests annually based on the method of Marshall and Surveyor (1). Our experience with this test has highlighted the significance of fasting before the study. The paper by Marshall et al. (2) discusses the different results obtained between patients who fasted and those who ate a test meal. Our concern relates to clinicians using a reference range based on fasting patients, who may not be rigorous in their application of this fasting criterion.

Although our procedure for ¹⁴C-urea breath testing involves informing the patient to fast (at least 6 hr) and confirming that the patient did indeed fast before the test commences, there are instances when this routine is not followed. On two occasions, patients started the test without fasting. These patients underwent a repeat study after fasting; the results from the second study are shown in Table 1.

We measure the $^{14}\text{CO}_2$ at 5-min intervals for 30 min and calculate the peak value after 10 min as: % dose/mmole $\text{CO}_2 \times \text{body}$ weight. We also measure the area under the curve after 10 min.

Both patients would have had equivocal or normal results because the test values were affected by the presence of food in their stomachs. Their

TABLE 1
Results for Carbon-14-Urea Breath Test before and after Fasting

Patient no.	Nonfasting		Fasting	
	Peak value	Area under curve	Peak	Area under curve
1	1.26	20.4	3.29	55.2
2	0.84	13.8	2.5	42.0

Our fasting reference ranges were: <0.5 normal; 0.5–1.5 equivocal: >1.5 positive for peak value; and 0–16 normal; 16–25 equivocal: >25 positive for the area under curve.

fasting values, however, were both positive for *Helicobacter pylori*. Unfortunately, there were no other follow-up tests performed to verify our results and, hence, the presence of *H. pylori*. The significant elevation of the fasting values warrants careful examination of the fasting state of each patient.

REFERENCES

- Marshall BJ, Surveyor I. Carbon-14-urea breath test for the diagnosis of Campylobacter pylori associated gastritis. J Nucl Med 1988;29:11-16.
- Marshall BJ, et al. A 20-minute breath test for Helicobacter pylori. Am J Gastroenterol 1991;86:4:438-445.

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Which Is Better for Inferior Wall Evaluation: A Full or Empty Stomach?

TO THE EDITOR: Technetium-99m-tetrofosmin, recently introduced as an agent for myocardial perfusion imaging, is excreted mainly by the biliary system (I). High intestinal activity may be seen in a one-day imaging protocol. This intestinal activity may create a major problem in the visual interpretation of the inferior myocardial wall, especially in the rest imaging.

In the study of Braat et al. (2), the inferior wall of myocardium was considered ischemic in three patients by at least two of the three different observers in the one-day protocol while in the two-day protocol, the same region was defined as scar tissue by the observers. The explanation for this discrepancy was proposed to be scatter from the abdominal and hepatic background to the inferior wall of the myocardium.

In our early studies with ^{99m}Tc-tetrofosmin, we told patients to have their normal meal 45–60 min before rest imaging. Imaging starts 20–30 min after injection and patients are advised to drink 200–300 cc water

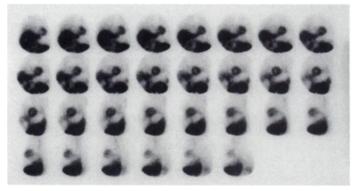
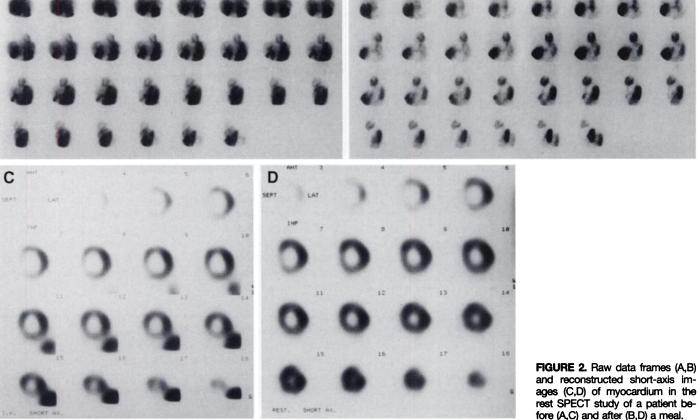


FIGURE 1. Raw data of rest myocardial SPECT image 20 min after an intravenous dose of 20 mCi of ^{99m}Tc-tetrofosmin. The patient was allowed to have his daily meal 1 hr before injection. Filled stomach appears as a photopenic area between myocardium and intestines in the frames.



ages (C,D) of myocardium in the rest SPECT study of a patient before (A,C) and after (B,D) a meal.

10-15 min before imaging. The filled stomach pushes the intestines caudal, removing intestinal activity from the myocardium (Fig. 1). A full stomach between myocardial and intestinal activity prevents scatter to the inferior wall of the myocardium (Fig. 2). This method may also be useful to reduce the additional undesired effect of duodenogastric reflux (3,4).

This method provides a high target-to-background ratio for myocardial imaging during a same day stress-rest protocol.

REFERENCES

- 1. Higley B, Smith FW, Smith T. Technetium-99m-1,2-bis {bis(2-ethoxyethyl) phosphino ethane: human biodistribution, dosimetry and safety of a myocardial perfusion agent. J Nucl Med 1993;34:30-38
- 2. Braat SH, Leclercq B, Itti R, Lahiri A, Sridhara B, Rigo P. Myocardial imaging with technetium-99m-tetrofosmin: comparison of one-day and two-day protocols. J Nucl Med 1994:35:1581-1585.
- Hassan IM, Mohammad MMJ, Constatinides C, Nair M, Belani N, Abdel-Dayem HM. Problems of duodenogastric reflux in ^{99m}Tc-Hexa MIBI planar, tomographic and bull's-eye display. Clin Nucl Med 1989;14:286-289.
- 4. Middleton GW, Williams JH. Significant gastric reflux of technetium-99m-MIBI in SPECT myocardial imaging. J Nucl Med 1994;35:619-620.

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The Transition from Technegas to Pertechnegas

TO THE EDITOR: The set of experiments described in the article by Scalzetti et al. (1) fills an important gap in the published science of technegas and its derivatives and rather neatly demonstrates some of the gas phase chemistry which occurs in the micro-aerosol generator. We performed only a few spot measurements looking for the transition point and worked down from our standard clinical figure of 3% oxygen in large steps.

At an oxygen concentration of $0.101 \pm 0.002\%$, we observed that 57% of the activity existed as pertechnetate. We used thin-layer paper chromatography using methyl ethyl ketone (MEK) as the solvent to separate mobile and nonmobile products.

Inspection of Scalzetti and Gagne's graphical data highlights an important parameter which also affects the technegas/pertechnegas ratio: the operating temperature of the machine.

We have examined the gas phase reaction which leads to the formation of technegas particles and uncovered an operating temperature/technegas yield profile which arises naturally from the mechanism of coating the technetium with graphite to form the micro-aerosol we call technegas. For example, in one set of measurements, the percentage of pertechnegas formed fell from 65% to 3% when the operating temperature of the machine was changed from 2475°C to 2550°C, i.e., an increase of only 75°C.

When the original design parameters for the micro-aerosol generator were set, a temperature of 2500°C was selected as a suitable operating temperature, at least 100°C below that at which the production of high levels of soot becomes significant. Scalzetti and Gagne's data would indicate that their machine might be operating at somewhat lower than the 2500°C, the servo response on the built-in optical pyrometer may not have been correct, and thus they could be generating a base level of pertechnegas caused by incomplete coating of the radionuclide by carbon.

Pertechnegas arose originally from the discovery of a wrongly labeled argon bottle being used in a micro-aerosol generator. The reproducibility of this phenomenon was tested with controlled oxygen loadings of argon gas cylinders at 2% and 5% (the original contaminated bottle was 3%), and then the Prince of Wales Hospital in Sydney was approached to test pertechnegas as an agent for examining the integrity of the alveolarcapillary membrane (2).

It was Mackey from that hospital who first coined the term pertechnegas to underline its pertechnetate properties in vivo, in contra distinction to its parent product technegas, which remains static in the lung once inhaled.