and by drying and weighing previously weighed filters. It can be seen that not only are the calculated and measured weights in good agreement but also that the weights absorbed on the Millipore filters are relatively constant despite considerable change in the total weight of albumin being passed through the filter. Thus, it appears that the filtration of small amounts of high-specific-activity Tc-99m HSA through cellulose-type filters will result in the loss of a significant amount of the labeled albumin—approximately 0.8 mg on a 25-mmdiameter filter.

A similar binding of albumin to cellulose has been reported in the case of paper chromatography by Lin et al. (1), who found that pretreatment of the paper with unlabeled albumin avoided the problem. When the same approach was applied here, the radioactivity retained by the filter was reduced to approximately one third of the amount on the untreated filter. It should be noted, however, that such a procedure would result in a loss of specific activity, and is therefore less than optimum where material of high specific activity is desired.

M. W. BILLINGHURST B. A. WESTENDORF Health Sciences Centre Winnipeg, Manitoba, Canada

REFERENCE

I. LIN MS, KRUSE SL, GOODWIN DA, et al.: Albumin loading effect: A pitfall in saline paper analysis of ⁹⁰Tcalbumin. J Nucl Med 15: 1018-1020, 1974

Using the S Tables of MIRD Pamphlet 11

Through the recently published Pamphlet 11 (1), the Society of Nuclear Medicine's MIRD Committee has sought to simplify greatly the calculation of absorbed doses from internally administered radionuclides. In this pamphlet, tables of S, the mean absorbed dose per unit cumulated activity, have been published for 117 radionuclides, with promises of more in the future. The implication is that to estimate the dose to a target organ from a radionuclide uniformly distributed in a source organ, the user need only calculate the cumulated activity in the source organ and multiply it by the value of S from that source organ to the desired target organ. The pamphlet contains a brief summary of the derivation, assumptions, and limitations of the tables, as well as three examples of their use.

We feel that clarification of some of the notations and explanations, especially those of Example 3, may be helpful to those who have occasionally used previous MIRD pamphlets. First, let us emphasize that the tables of Pamphlet 11 combine into each value of S the contributions resulting from both penetrating and nonpenetrating emissions, and that nonpenetrating S values occur in the tables (A) whenever source and target regions are the same, and (B) in all entries pertaining to the total body. Separate entries for penetrating and nonpenetrating components of S for some radionuclides, as well as a more detailed explanation of S, are available in ORNL-5000 (2).

Second, in Example 3 the value of \bar{A}_{bone} is listed as 3.0 μ Ci-h; $\bar{A}_{blade} = 0.6 \mu$ Ci-h; and $\bar{A}_{TB} = 0.4 \mu$ Ci-h where "the latter represents activity uniformly distributed in the total body, in addition to the activity present in the other organs." In past MIRD publications, the symbol \bar{A}_r has im-

plied the total cumulated activity uniformly distributed in region r. Note that Example 3 defines the cumulated activity symbols differently. Recalling the notations of Cloutier et al. (3), the cumulated activity values given in Example 3 were previously called Abone, Ablade, and Aunif, where the latter is the cumulated activity uniformly distributed throughout the body, and the first two are the differences between A_{unif} and the total cumulated activities in the bone and bladder contents, respectively. (Note: \tilde{A}_r^* may be either positive or negative, depending on whether the concentration of activity in region r is greater or smaller than the concentration that is uniformly distributed in the body. Also $\tilde{A}_r^* = \tilde{A}_r$ if and only if $\tilde{A}_{unif} = 0$, as is the case in Examples 1 and 2 of Pamphlet 11.) As pointed out by Roedler et al. (4) these distinctions in cumulated activities affect the final dose estimates most significantly if a large portion of the activity in the body is unaccounted for in specific organs.

In summary, we wish to emphasize: (A) the S values of MIRD Pamphlet 11 contain a nonpenetrating component for all total-body entries as well as for those entries in which target and source are the same; and (B) the symbols for the cumulated activities \bar{A}_{bone} , \bar{A}_{blade} , and \bar{A}_{TB} as used in Example 3 of this pamphlet replace \bar{A}_{bone} , \bar{A}_{blade} , and \bar{A}_{wnif} , respectively, describe previously by Cloutier et al. (3).

> PAUL A. FELLER VINCENT J. SODD Nuclear Medicine Laboratory Bureau of Radiological Health, FDA Cincinnati, Ohio

JAMES G. KEREIAKES Radioisotope Laboratory University of Cincinnati College of Medicine Cincinnati, Ohio

REFERENCES

1. SNYDER WS, FORD MR, WARNER GG, et al.: "S," absorbed dose per unit cumulated activity for selected radionuclides and organs. MIRD Pamphlet No. 11, New York, Society of Nuclear Medicine, 1975, pp 1-257

2. SNYDER WS, FORD MR, WARNER GG, et al.: A tabulation of dose equivalent per microcurie-day for source and target organs of an adult for various radionuclides. Oak Ridge National Laboratory (ORNL-5000), Oak Ridge, Tenn., 1974, pp 1-70

3. CLOUTIER RJ, WATSON EE, ROHRER RH, et al.: Calculating the radiation dose to an organ. J Nucl Med 14: 53-55, 1973

4. ROEDLER HD, KAUL A: Dose to target organs from remaining body activity: Results of the formally exact and approximate solution. In *Radiopharmaceutical Dosimetry* Symposium, Proceedings of Conference Held at Oak Ridge, Tenn., April 26-29, 1976, Cloutier RJ, Coffey JL, Snyder WS, Watson EE, eds. HEW Publication (FDA) 76-8044, June 1976, pp 155-163

An Improved FORTRAN Program for Calculating Modulation Transfer Functions

In a recent concise communication by Benedetto and Nusynowitz (1) describing a FORTRAN program for cal-