BONE SCINTIGRAPHY WITH ⁴⁷Sc AND THE SCINTILLATION CAMERA

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The direct measurement of radioactivity in bone after the administration of a tracer has chiefly been done with ${}^{47}Ca$ and ${}^{85}Sr$. ${}^{18}F$ has also been used recently (1). This isotope has numerous advantages: its half-life of 111 min is short, letting one record high counts while the radiation dose remains low. Moreover, the fluorine accumulates rapidly in the skeleton, and scintigrams can be made 1 hr after administration of the tracer. The isotope is a positron emitter, and when it is used with a positron camera, one obtains scintigraphic images rapidly and with great clarity (2).

Nevertheless, there are limitations to the use of 18 F. Because of its short period, one must be close to the site of production, and its price is quite high. We have therefore considered and tested a new procedure for bone scintigraphy. It consists of using the photoelectric peak of 47 Sc produced by the decay of 47 Ca. We report here the principle of the method, its advantages and applications.

MATERIALS AND METHODS

⁴⁷Ca is a difficult nuclide for scintigraphy because it emits beta and gamma rays with a half-life of 4.8 days. The energy of its photoelectric peak is 1.28 Mev. It decays into ⁴⁷Sc with a half-life of 3.43 days. ⁴⁷Sc yields stable titanium by emitting 166-kev gamma rays. The decay scheme is seen in Fig. 1.

The metabolism of the mixture of ${}^{47}Sc$ and ${}^{47}Ca$ injected intravenously has been studied by Taylor (3). This author has demonstrated that ${}^{47}Sc$ in solution follows an independent path and is fixed mostly in liver, kidneys, spleen and bones while the ${}^{47}Ca$ goes mostly to the bone. The reasons we chose ${}^{47}Sc$ to obtain bone images are the following:

1. ⁴⁷Sc produced from the decay of the ⁴⁷Ca fixed on the bone does not have the same metabolism as ⁴⁷Sc and remains fixed on the organic matrix of the bone. 2. The 166-kev energy of the scandium photoelectric peak fits very well with the optimum performance of a scintillation camera, which is very efficient in detecting gamma rays with energies between 100 and 400 kev.

3. The equilibrium of the ${}^{47}Ca$ and ${}^{47}Sc$ mixture is quickly reached. After 8 days in the skeleton the intensity of the photoelectric peak of ${}^{47}Sc$ is much higher than that of ${}^{47}Ca$, giving far clearer images with higher contrast than the calcium does. The ratio between the two peaks ${}^{47}Ca/{}^{47}Sc$ is 2.5 \times 10^{-2} (Fig. 2).

We carried out our first bone studies with ⁴⁷Sc on rats weighing about 200 gm and medium-size rabbits by intravenous injection of 20-50 μ c of a ⁴⁷Ca-⁴⁷Sc mixture. In man, ⁴⁷Ca was injected intravenously in doses not exceeding 1 μ c/kg of body weight, doses lower than CIPR norms (100 μ c). The bone scintigraphy was done with the Anger scintillation camera equipped with a collimator whose efficiency extended from 100-300 kev. The preliminary studies of the ⁴⁷Ca-⁴⁷Sc mixture was done using a sodium iodide crystal in conjunction with a photomultiplier. We have also been using lithium-drifted germanium junction, manufactured by SAIP (Société Applications Industrielles de la Physique), with the high resolving power of 5 kev for 60Co. All the spectra were registered with a 400-channel selector.

RESULTS

The first scintigraphic image which was made 2 days after administration of the tracer, shows a highly active zone at the level of the liver and the kidneys (Fig. 3). The localization is due to the 47 Sc present in the solution at the time of injection when

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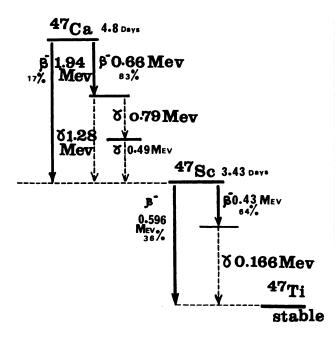


FIG. 1. Disintegrated scheme for ⁴⁷Ca.

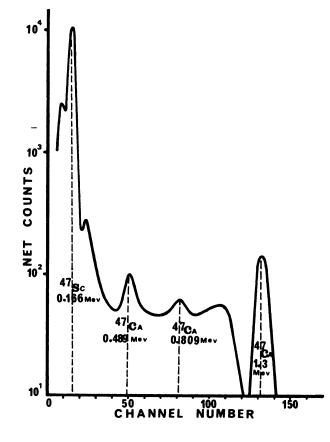


FIG. 2. Spectrum of ${}^{47}Ca-{}^{47}Sc$ mixture in vivo 8 days after injection into rats.

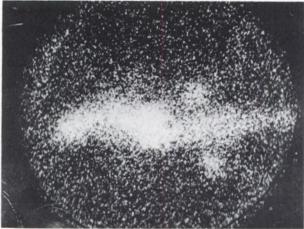


FIG. 3. Distribution of ⁴⁷Sc 2 days after injection of mixture of ⁴⁷Ca and ⁴⁷Sc in rat.

the ${}^{47}Ca - {}^{47}Sc$ mixture is practically at equilibrium; at this time the image of the skeleton begins to appear on the scintigram.

On the fourth, sixth and eighth days after the injection, the scintigraphic images show a progressive diminution of the active liver zone, whereas the radioactivity due to 4^{7} Sc fixed on the skeleton is rising steeply. One can see a very intense fixation in the skull, the iliac region and the joints (Fig. 4). The scintigrams shown are of rats only because we have not so far obtained as good images of the whole animal with the larger rabbits.

DISCUSSION

We have compared several images of bone scintigraphy obtained with ⁴⁷Ca, ⁴⁷Sc and ⁸⁵Sr with the peak of our spectrometer at 490 kev for ⁴⁷Ca, 166 kev for ⁴⁷Sc and 514 kev for ⁸⁵Sr. The images ob-



FIG. 4. Distribution of ⁴⁷Sc in rat 8 days after injection of ⁴⁷Ca-⁴⁷Sc mixture.

tained with ⁴⁷Ca cannot be interpreted because the number of counts is very low and the background radiation is very high. For ⁸⁵Sr the resolving power of our camera remains low. The images obtained with ⁴⁷Sc are much better and show a high contrast (Fig. 4). One can see the lower limits of the rat with intense fixation zones at the joints.

A single study has been made with a visualization unit (Intertechnique) that lets one eliminate the background counts and thus improve the quality of the scintigrams. Unfortunately this short study with ⁸⁵Sr is the only one we were able to do while the unit was available, but we expect to improve the quality of our ⁴⁷Sc scintigrams equally in our later work.

In conclusion, it is interesting to note that ⁴⁷Sc for bone scintigraphy represents an excellent tracer for calcium because it lets one follow the progressive fixation of calcium in the bone since the physical character of ⁴⁷Sc is well suited to scintigraphic examinations. We feel this technique of bone scintigraphy with ⁴⁷Sc promises to be of great usefulness in man for studying many osteopathic disorders.

SUMMARY

After presenting some physical and metabolic characteristics of ⁴⁷Ca and ⁴⁷Sc, we propose a new technique for bone scintigraphy using the scintillation camera and ⁴⁷Sc as a tracer. The images obtained on rats and rabbits show a much better definition and contrast than those usually obtained with ⁴⁷Ca or ⁸⁵Sr.

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