

Evaluation of Indium-111-2-Mercaptopyridine-*N*-Oxide for Labeling Leukocytes in Plasma: A Kit Preparation

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Pure neutrophils, lymphocytes, and mixed leukocytes have been labeled *in vitro* with ^{111}In chelated to a nontoxic, water soluble agent 2-mercaptopyridine-*N*-oxide (Merc). Cells were labeled in isotonic salt-balanced medium with preformed [^{111}In]Merc (yield >95%), or in 0.5 ml autologous plasma by incubation with dry Merc first and then with ^{111}In (yield 75%). The latter method facilitated a kit procedure that required 2 μg dry Merc when acid citrate dextrose was used as anticoagulant or 20 μg when heparin was used. Labeling efficiency was dependent on cell concentration and pH. Labeled cells accumulated avidly in experimental abscesses and provided abscess/blood ratios of >75 at 24 hr postinjection. In dogs, the liver uptake of labeled cells was only $18.8 \pm 7.1\%$ compared to that of 48.5% when cells were labeled with [^{111}In]oxine.

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During the past few years we have witnessed a dramatic increase in the use of indium-111- (^{111}In) labeled leukocytes for detecting abscesses and other inflammatory processes induced experimentally or occurring clinically deep in the body (1-10). The technique of labeling neutrophils with a gamma-emitting radionuclide, first evaluated in 1976 and further studied for its feasibility in patients since 1977, was based upon the passive diffusion of ^{111}In chelated with 8-hydroxyquinoline (oxine) (11,12). In the presence of plasma however, ^{111}In chelated with oxine binds to transferrin and necessitates the removal of blood plasma requiring the cells to be suspended in a suitable balanced salt media for efficient incorporation of radioactivity. Since this is undesirable, newer lipophilic agents such as [^{111}In]acetylacetone (13) and tropolone (14,15) have been developed. While some investigators have used them efficiently (16,17) others have found them to be less attractive than [^{111}In]oxine (18-21).

We have recently developed a new agent, namely [^{111}In]-2-Mercaptopyridine-*N*-oxide ([^{111}In]Merc), which allows efficient labeling of human platelets in plasma by a kit procedure (22). The purpose of this investigation was to evaluate the use of [^{111}In]Merc to label leukocytes in plasma, also by a kit procedure. Various parameters that may optimize labeling yields have been studied and the efficacy of the new agent has been compared with those of oxine and tropolone. The ability of labeled leukocytes to accumulate in experimental abscesses has been compared with gallium-67 (^{67}Ga) citrate in dogs.

MATERIALS AND METHODS

The new agent: Properties, preparation, and stability

The chemical characteristics of Merc, its toxicity and the methods of preparing [^{111}In]Merc are described elsewhere (22). It has been shown that Merc with ^{111}In forms a lipid soluble (1:3) complex at a wide range of pH and is stable under normal laboratory conditions (23,24).

Studies of the influence of some cationic impurities such as Zn^{2+} , Cd^{2+} , Fe^{2+} , and Fe^{3+} that may exist in [^{111}In]chloride

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solution on the formation of [^{111}In]Merc complex, have shown that the presence of Fe^{3+} interferes most (22).

For investigational use, [^{111}In]Merc was prepared in either 0.9% NaCl, 0.05%M phosphate buffer pH 7.4, 0.1M acetate buffer pH 7.4 or 3.8% sodium citrate. To 1 ml of these solutions were added a known quantity of Merc (1 mg/ml prepared freshly in corresponding medium) and [^{111}In]chloride (50 mCi/ml). Five hundred microliters of this preparation were diluted to 1 ml with a corresponding buffer solution and subjected to chloroform extraction. Percentage extraction efficiency was determined. The other 0.5 ml of [^{111}In]Merc aqueous solution was used for cell labeling.

Alternatively 1 to 50 μl of 1 mg/ml Merc solution in 0.05M phosphate buffer pH 7 were dispensed in sterile polystyrene test tubes, air-dried in a laminar flow hood, and stored for subsequent use. A required quantity of [^{111}In]chloride was also dried to eliminate the acid or buffered with citrate buffer pH 6.5 so that the final strength of the citrate buffer solution was 0.25M and the final total volume of [^{111}In]citrate was not more than 50 μl (0.0125 mM).

Cell separation procedures

Studies, with the exception of three abscess-bearing dogs, were carried out using venous blood obtained from healthy human volunteers. Blood was drawn in a 30-ml syringe containing ~300 units of heparin* or 4 ml of acid citrate dextrose solution. For studies requiring a larger number of cells, multiples of these blood volumes were used. Leukocyte-rich plasma was obtained using our routine procedure in which erythrocytes were allowed to sediment by hanging the syringe upright supported by an U-shaped 19 G needle in a laminar flow hood (24). The sedimentation was aided by adding to the blood 3% (v/v) of 2% (w/v) methylcellulose (Erythrocytes in patients' blood were allowed to sediment spontaneously). Leukocyte-rich plasma was then separated and centrifuged at 450 g for 5 min. A cell button thus obtained was then suspended either in 0.5 ml plasma, or washed once with phosphate buffered saline (PBS, pH 7) and suspended in 1.5 ml PBS. On most occasions mixed leukocytes were used. However, in some studies, pure neutrophils or lymphocytes were employed. These were separated using either Boyum's Lymphoprep (25) or noncontinuous density gradient media of 50, 60, and 65% Percoll.†

Labeling leukocytes with [^{111}In]Merc

Using [^{111}In]Merc, leukocytes could be labeled either in phosphate buffered saline or in plasma. Since being able to label cells efficiently in plasma was our primary objective, a major proportion of evaluation studies was carried out with cells labeled in plasma. For labeling cells in PBS, preprepared [^{111}In]Merc was used and cells were incubated at room temperature for 15 min. Cells were then centrifuged at 450 g \times 5 min and the cell button was washed by carefully layering over 0.5 ml leukocyte-poor plasma. Labeled leukocytes were then resuspended in plasma.

In plasma labeling, cells were suspended in 0.5 ml plasma, incubated with dry Merc for 5 min in a polystyrene tube (not polypropylene) and then with [^{111}In] either dry or in 0.25M citrate buffer pH 6. The mixture was incubated for 20 min at room temperature, and centrifuged at 450 g for 5 min. The

supernatant was removed, fresh leukocyte-poor plasma was gently layered over the cell button and removed. Finally cells were suspended in 5 ml plasma. A sterility test was performed by adding a 100 μl aliquot to a Trypticase soy broth tissue culture[‡] and incubating at 37°C for 8 days. A smear was made for observing structural integrity and differential cell counting. The specific conditions evolved from the results of experiments described as follows.

Influence of pH

Since it is difficult to maintain pH of plasma, PBS was used as a suspending medium and pH (3.8–7) was then adjusted using isotonic solution of sodium citrate or citric acid. Pure neutrophils at a concentration of 1.3 to 4.4 million cells/ml and pure lymphocytes at a concentration of 21 million/ml were used. To each test tube was then added [^{111}In]Merc, and the cells were incubated at 22°C for 15 min, centrifuged and labeling efficiency was determined.

Effect of anticoagulant: Heparin compared with acid citrate dextrose (ACD-A)

Ninety milliliters of blood were drawn using either 900 I.U. of heparin or 12 ml ACD-A as an anticoagulant and leukocytes were separated as described before. They were then suspended in 3.5 ml plasma. Half a milliliter of this suspension was incubated with an accurately known quantity of dry Merc which ranged between 1 to 100 μg . Cells were then incubated with [^{111}In] and labeling efficiency was determined in the usual manner.

Effect of cell concentration

Leukocytes separated from 90 ml of blood drawn using heparin as an anticoagulant were employed. These were suspended in 1 ml plasma and cell concentration was determined using a Coulter counter. Contaminating erythrocytes were eliminated by hypotonic lysis.

One hundred to 500 μl aliquot of this suspension was then added to test tubes containing dry Merc. This was followed by the addition of autologous plasma so that the final volume in each test tube was 500 μl . The cells were then incubated with [^{111}In] and labeling efficiency was determined.

Comparative use of Merc, oxine, and tropolone

Test tubes containing known quantities of either Merc, oxine, or tropolone were incubated with ~60 million leukocytes suspended in 0.5 ml plasma and then with [^{111}In]. The percentage of labeling efficiencies were then calculated for each chelating agent.

Differential radioactivity distribution

The aim of this exercise was to determine the percentage of radioactivity associated with neutrophils, lymphocytes, erythrocytes, and contaminating platelets when leukocytes were labeled with [^{111}In]Merc in plasma using the dry Merc kit procedure carried out for clinical studies. This was accomplished by diluting an aliquot of ~100 μl labeled cells

(ready for injection) to 3 ml leukocyte-poor plasma and centrifuging over Ficoll-Hypaque (1.077 g/cm³) density gradient at 450 g for 30 min, as per Boyum (25).

For quantitative distribution of radioactivity, platelets in the upper plasma layer and lymphocytes at the interphase were separated. Erythrocytes in the cell button were lysed with 1 ml water for 60 sec, centrifuged and the supernatant separated from neutrophils at the bottom of the test tube. Radioactivity in the supernatant and neutrophils was measured in an ionization chamber and percentage radioactivity in each fraction was calculated.

In vivo evaluation

Studies were carried out in three dogs in which abscesses were induced by an intramuscular injection of 0.1 ml turpentine (2). Twenty-four hours following this procedure, animals received ~500 μ Ci of [¹¹¹In]Merc labeled autologous leukocytes as well as 1.5 mCi [⁶⁷Ga]citrate. The next day, the animals were killed with an overdose of pentobarbital and tissues were dissected. These were weighed and concomitant ¹¹¹In and ⁶⁷Ga radioactivity was determined using a 15 cc Ge (Li) detector[†] coupled to a multi-channel analyzer. ** Suitable ¹¹¹In and ⁶⁷Ga standards were made and counted similarly to enable us to determine percentage radioactivity of each radionuclide associated with each type of tissue. Abscess to blood, fat, muscle, liver, and spleen ratios were also calculated and compared to those with ¹¹¹In]oxine labeled leukocytes studied previously (2).

RESULTS

Using Merc as a chelating agent, neutrophils or lymphocytes can be labeled when suspended either in PBS (average of 95% labeling efficiency) or in plasma (average of 75% labeling efficiency).

In PBS labeling a preprepared [¹¹¹In]Merc was used. Such preprepared [¹¹¹In]Merc can also be used when plasma is employed as a suspending medium. However, incubating cells in plasma with dry Merc for 5 min at 22°C, followed by a 15-min incubation also at 22°C, with ¹¹¹In either dry or in 0.25M citrate buffer pH 6 (total volume less than 50 μ l), made the procedure simple, attractive, and easy to adapt for the preparation of a kit.

Table 1 indicates that the highest incorporation of radioactivity was achieved at neutral pH and that it decreased rapidly as pH of the medium decreased. Labeling efficiency was also dependent on cell concentration and decreased as the

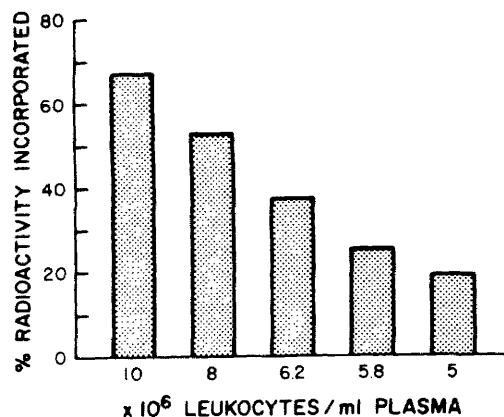


FIGURE 1
Influence of leukocyte concentration on labeling yields (Merc 50 μ g/ml, 22°C incubation for 15 min)

number of cells per ml increased (Fig. 1).

Studies on the effect of Merc concentration when labeling cells in plasma indicated that for optimal labeling efficiency 20 μ g dry Merc were required when heparin was used as an anticoagulant (Fig. 2). In these preparations radioactivity associated with platelets was less than 3% and that with erythrocytes averaged less than 2%. When ACD-A was used as an anticoagulant, only 2 μ g Merc were sufficient for optimal labeling efficiency. This decreased sharply up to 20 μ g Merc and then plateaued. At these concentrations, however, both oxine and tropolone in the dry form, used under identical conditions of pH and cell concentration, allowed only ~10% labeling efficiency (Table 2).

Autologous leukocytes labeled with [¹¹¹In]Merc and given along with [⁶⁷Ga]citrate to dogs bearing experimentally induced abscesses indicated that the abscess to tissue ratio with ¹¹¹In (Merc or oxine) were much higher (>75) than those obtained with [⁶⁷Ga]citrate (11.9). With [¹¹¹In]Merc-labeled cells the abscess to blood ratios (75.2) were close to those obtained with [¹¹¹In]oxine-labeled leukocytes (75.8) (24,2).

Interestingly, however, the abscess to liver and abscess to spleen ratios obtained with [¹¹¹In]Merc-labeled cells were much higher (14.6 and 4.2, respectively) than those obtained with [¹¹¹In]oxine-labeled leukocytes (4.2 and 1.8, respectively). The absolute quantity of [¹¹¹In]Merc leukocytes measured 18.8 \pm 7.1% in the liver and 11.2 \pm 8.9% in the spleen.

DISCUSSION

This work was undertaken to assess the feasibility of labeling leukocytes in plasma with [¹¹¹In]Merc which has been observed to label human platelets in plasma efficiently (22). Over the past few years, labeling leukocytes with [¹¹¹In]oxine in a nonplasma salt-balanced media has become an established technique and has been employed in thousands of patients for detecting infectious processes. It has been reported, however, that neutrophils labeled in plasma with [¹¹¹In]tropolone cleared from the lungs in a shorter period of time than

TABLE 1
Influence of pH on Labeling Efficiency (LE)

pH	Neutrophils		Lymphocytes		
	13 million/ml		21 million/ml		
	LE (%)	LE (%)	LE (%)	LE (%)	
3.8	14.4	4.5	44.3	4.8	35.8
5.2	45.9	5.8	90.7	5.5	76.5
6.4	91.9	6.5	96.9	6.2	94.6
6.9	94.4	6.6	98.2	6.4	96.0
7.0	93.0	6.8	98.0	6.9	96.7

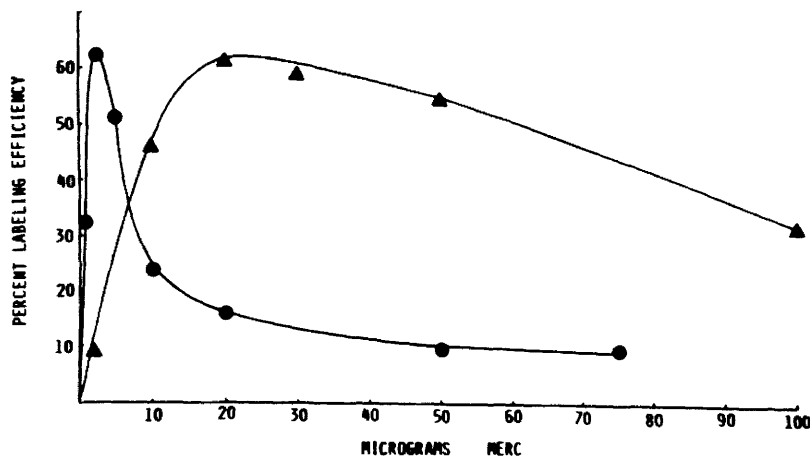


FIGURE 2
Effect of Merc concentration on incorporation of ^{111}In into (~ 50 million/0.5 ml plasma) leukocytes separated from blood anticoagulated either with heparin or ACD. (●) ACD; (▲) Heparin

did neutrophils labeled with [^{111}In]oxine in saline (16). Furthermore, tropolone-labeled cells enabled investigators to detect abscesses in less than 4 hr postinjection due to the rapid migration of the cells to the sites of inflammation (16).

Although these advantages are appreciable, many investigators have found disadvantages to these agents compared to the use of [^{111}In]oxine (18–21). Since platelets can be labeled in plasma using [^{111}In]Merc by a kit method, it was a natural progression that the use of this method be investigated for labeling leukocytes in mixture with lymphocytes. The dry Merc concentration required by the optimal platelet labeling is 2 μg (22). This concentration can also be used for the optimal labeling of leukocytes (Fig. 2) but only when ACD-A is used as an anticoagulant. As high as $29 \pm 15\%$ of ^{111}In activity associated with contaminating platelets in leukocytes separated from ACD anticoagulated blood has been reported previously (26). Contrary to this, when heparin was used as an anticoagulant, contamination of radioactive platelets in leukocytes was no more than 3%. In these preparations radioactivity associated with erythrocytes remained less than 2%. This minimizes the blood background and decreased interference in abscess localization. Unfortunately, when leukocytes are separated from heparin as an anticoagulant, 20 μg Merc is required for optimal labeling yields (Fig. 2). Having to

prepare test tubes with 20 μg dry Merc is just as easy as preparing them with 2 μg Merc for a platelet kit. We prefer the use of dry Merc because it eliminates the preparation of [^{111}In]Merc and avoids any problems related to its quality control and stability.

The reasons for the necessity of the higher quantity of Merc for labeling leukocytes from heparin anticoagulated blood are not yet clearly understood. However, it is considered that some quantity of Merc, in the presence of a small quantity of heparin, probably forms disulphides, a class substance which cannot bind metal ions (27).

Experiments studying the influence of additional 1 to 50 units of heparin in 0.5 ml plasma indicated no further reduction in labeling efficiency. However, we do not use more than 10 IU heparin per ml of blood. Generally $>75\%$ labeling efficiency is achieved, but depending upon the cell concentration lower labeling yields have been obtained. Incubation at 37°C did not raise labeling efficiency or the rate of incorporation of radioactivity, but increased the risk of leukocytes aggregation.

Nevertheless, advantages of labeling leukocytes in plasma with [^{111}In]Merc were obvious. In humans, leukocytes labeled by this procedure cleared rapidly from normal lungs (24), migrated to abscesses sooner and helped reduce the quantity of radioactivity taken up by the liver. The exact quantification of radioactivity is yet to be determined, but qualitatively it appears from the scans that the radioactivity concentration in the liver is no more than that in the bone marrow. In a canine model, the hepatic uptake of [^{111}In]Merc-labeled leukocytes was only $18.8 \pm 7.1\%$ compared with that of 48.5% when cells were labeled with [^{111}In]oxine (28). This probably suggests a better preservation of cell viability and supports the in vitro observations that Merc does not alter the phagocytic ability of neutrophils.

The exact nature of the radioactivity that accumulates in the liver, spleen, and bone marrow activity is a subject of further investigations. Using sulfur-35-labeled Merc, we have attempted to study the mechanism by which 20

TABLE 2
Leukocytes Labeling Yields with ^{111}In Using Dry Merc, Oxine, and Tropolone

μg	Merc	Oxine	Tropolone
10	46 ± 4.5	6.9 ± 2.3	8.7 ± 4.2
25	96 ± 2.3	10.4 ± 2.2	7.8 ± 3.2
50	55 ± 5.7	5.6 ± 2.1	8.2 ± 3.9

* 60 million leukocytes in 0.5 ml plasma were first incubated with the agent and then with dry ^{111}In .

μg dry Merc allows ^{111}In to incorporate into the cells. The initial results of these experiments indicated that after cell incubation, greater than 90% of Merc remained in plasma and probably only indium bound Merc entered in cells. Indium-111 was bound to cytoplasmic components and Merc also appeared to remain in association with cytoplasmic components.

When 100 million leukocytes containing ~ 30 million lymphocytes are labeled with $\sim 500 \mu\text{Ci } ^{111}\text{In}$, each lymphocyte receives a radiation dose of >8000 rad. Consequently, they may no longer be viable and pose no further risk to the recipient (29). These are probably taken up by the spleen.

Our experiments in which we used technetium-99m ($^{99\text{m}}\text{Tc}$), ^{67}Ga , or thallium-201 as probable tracers for Merc incubated leukocytes produced lower labeling yields than ^{111}In . This eliminated the possibility of using [$^{99\text{m}}\text{Tc}$]Merc which could have been particularly useful since early abscess detection appeared feasible. In comparison with other agents such as oxine or tropolone Merc produced higher labeling efficiency (Table 2). We believe, therefore, that Merc is not only a nontoxic, water soluble, chelating agent, but also allows efficient cell labeling in plasma by a simple kit procedure that could be uniformly performed in any laboratory. It is hoped that investigators will find this agent easier to use and will be able to eliminate the laboratory to laboratory variations that exist in cell labeling procedures today (30).

FOOTNOTES

- * Elkin-Sinn, Inc., NJ.
- † Pharmacia.
- ‡ Becton Dickinson.
- § Capintec CRC-5, Capintec Inc., Ramsey, NJ.
- ¶ Canberra Industries, Meriden, CT.
- ** Tracor Northern, TN-1710.

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