Journal of Nuclear Medicine, published on March 26, 2015 as doi:10.2967/jnumed.114.152215

Development of a Widely Usable Amino Acid Tracer: ^{76}Br-α-Methyl-Phenylalanine for Tumor PET Imaging

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Word count: 4,992 words

Financial support: This work was supported by a Grant-in-Aid for Young Scientists (A) (22689035) to H.H. from the Ministry of Health, Labor and Welfare.

Short running title: ^{76}Br-α-Me-Phe for tumor imaging

ABSTRACT

Radiolabeled amino acids are superior PET tracers for the imaging of malignant tumors, and amino acids labeled with ^{76}Br, an attractive positron emitter due to its relatively long half-life ($t_{1/2}$ = 16.2 h), could potentially be a widely usable tumor imaging tracer. In this study, in consideration of its stability and tumor specificity, we designed two ^{76}Br-labeled amino acid derivatives, 2-^{76}Br-bromo-α-methyl-L-phenylalanine (2-^{76}Br-BAMP) and 4-^{76}Br-bromo-α-methyl-L-phenylalanine (4-^{76}Br-BAMP), and we investigated their potential as tumor-imaging agents. **Methods:** Both ^{76}Br- and ^{77}Br-labeled amino acid derivatives were prepared. We performed in vitro and in vivo stability studies and cellular uptake studies using the LS180 colon adenocarcinoma cell line. Biodistribution studies in normal mice and in LS180 tumor-bearing mice were performed, and the tumors were imaged with a small-animal PET scanner. **Results:** Both ^{77}Br-BAMPs were stable in the plasma and in the murine body. While both ^{77}Br-BAMPs were taken up by LS180 cells and the uptake was inhibited by L-type amino acid transporter 1 inhibitors, 2-^{77}Br-BAMP exhibited higher uptake than 4-^{77}Br-BAMP. In the biodistribution studies, 2-^{77}Br-BAMP showed more rapid blood clearance and lower renal accumulation compared to 4-^{77}Br-BAMP. More than 90% of the injected radioactivity was excreted in the urine by 6 h after the injection of 2-^{77}Br-BAMP. High tumor accumulation of 2-^{77}Br-BAMP was observed in tumor-bearing mice, and PET imaging with 2-^{76}Br-BAMP enabled clear visualization of the tumors. **Conclusions:** 2-^{77}Br-BAMP exhibited preferred pharmacokinetics and high LS180 tumor accumulation, and 2-^{76}Br-BAMP enabled clear visualization of the tumors by PET imaging. These

findings suggest that 2-^{76}Br-BAMP could constitute a potential new PET tracer for tumor imaging and may eventually enable the wider use of amino acid tracers.

Key words: ^{76}Br; α-methyl-L-phenylalanine; tumor imaging; PET

INTRODUCTION

It is well recognized that ^{18}F-FDG-PET has had a great impact in tumor imaging and monitoring the response of tumors to chemotherapy. However, the high accumulations of ^{18}F-FDG that can occur in non-target tissues such as the brain and inflammatory sites invoke the need for other PET tracers that could complement or replace ^{18}F-FDG (*1, 2*). Among them, amino acid tracers such as ^{11}C-methionine, *O*-^{18}F-fluoromethyl-L-tyrosine, *O*-^{18}F-fluoroethyl-L-tyrosine and 3-^{18}F-fluoro-α-methyl-L-tyrosine (^{18}F-FAMT) have already been introduced into clinical practice (*1, 3, 4*). However, their widespread application in clinical studies is limited by the short half-lives of ^{11}C and ^{18}F. It may be possible to deliver an ^{18}F-labeled amino acid tracer as is done with ^{18}F-FDG, but the development of PET tracers using radionuclides with longer half-lives may constitute a way to circumvent the problem.

Among the positron emission radionuclides, ^{76}Br has been proposed as an attractive candidate for using PET ($\beta^+ = 57\%$, EC = 43%). ^{76}Br can be produced with a low-energy cyclotron by the nuclear reaction of ^{76}Se(p,n)^{76}Br (*5*). The relatively long half-life ($t_{1/2} = 16.2$ h) of ^{76}Br allows the delivery of ^{76}Br-labeled PET tracers from private companies and/or large facilities to other facilities. Several studies have demonstrated that PET imaging with ^{76}Br-labeled tracers is feasible not only in laboratory experiments but also for clinical diagnostics (*6-8*). Thus, the development of ^{76}Br-labeled amino acids that could complement or replace ^{18}F-FDG would provide significant benefit to tumor diagnoses in many PET facilities.

We previously designed and evaluated 3-^{76}Br-bromo-α-methyl-L-tyrosine (^{76}Br-BAMT), a ^{76}Br-substituted derivative of ^{18}F-FAMT, and we found that ^{76}Br-BAMT was transported to tumor cells via L-type amino acid transporter type 1 (LAT1) and provided the clear visualization of murine tumors by PET imaging (*9*). However, high background radioactivity levels caused by the debrominated free bromine were observed. Since radiobromine is a tracer of extracellular space and is retained in the blood and organs (*8, 10*), improved stability against in vivo debromination is needed before ^{76}Br-labeled amino acid can be used in clinical practice. In the present study, we considered the involvement of dehalogenase in the debromination of ^{76}Br-BAMT, and we designed and synthesized two ^{76}Br-labeled amino acid derivatives without phenolic hydroxyl groups, 2-^{76}Br-α-methyl-L-phenylalanine (2-^{76}Br-BAMP) and 4-^{76}Br-α-methyl-L-phenylalanine (4-^{76}Br-BAMP). Their stability against in vivo debromination, physicochemical properties, tumor cell uptake, and biodistribution were then evaluated. PET imaging was also conducted in nude mice bearing LS180 tumor cells. The potential of 2-^{76}Br-BAMP and 4-^{76}Br-BAMP as tumor-imaging agents were evaluated.

MATERIALS AND METHODS

We purchased 2- and 4-iodo-α-methyl-L-phenylalanine from NAGASE & Co. ^{18}F was produced using a biomedical cyclotron, CYPRIS HM-18 (Sumitomo Heavy Industries), and then we synthesized ^{18}F-FAMT according to the method developed by Tomiyoshi et al. (*11*). A reversed-phase HPLC (RP-HPLC) analysis was performed with a C-18 column (Capcell Pak C18 AQ, 4.6 × 250 mm,

Shiseido Co.) at flow rate of 1 mL/min eluted with a linear gradient of water containing 0.1% trifluoroacetic acid (TFA) and acetonitrile containing 0.1% TFA from 90:10 to 75:25 in 30 min (system 1) or from 90:10 to 10:90 in 40 min (system 2). All other chemicals used were of the highest purity available.

Preparation of Radiobrominated BAMPs

We synthesized 2- and 4-trimethylstannyl-*N*-trifluoroacetyl-α-methyl-L-phenylalanine methyl ester (4a and 4b, respectively) as the radiolabeling precursor of 2- and 4-radiobrominated BAMPs (Fig. 1). The detailed synthesis procedures of each precursor are described in the Supplemental Information. No-carrier-added ^{76}Br and ^{77}Br, the latter of which is a suitable radiobromine for basic studies due to its longer half-life ($t_{1/2}$ = 57.1 h), were produced according to a process reported by Tolmachev et al. (*5*), with some modifications as described (*12*). For radiobromination, 100 μL of each stannyl precursor (1 mg/mL) dissolved in methanol containing 1% acetic acid was mixed with 15–100 μL of aqueous radiobromine solution in a small vial. Then, 10 μL of *N*-chlorosuccinimide (10 mg/mL) in methanol was added to the vial, and the reactant was incubated at room temperature for 30 min. After the reaction was quenched with aqueous sodium bisulfite (10 μL, 10 mg/mL), 6 M aqueous NaOH at the same amount as the reaction mixture was added, then heated to 70°C for 1 h. After the pH of reaction

mixture was neutralized, purification was performed by RP-HPLC (system 1), and the solvent was removed in vacuo. The radiochemical purity of BAMPs was determined by RP-HPLC (system 2).

Stability and characterization of BAMPs

Mice for these analyses were cared for and treated in accordance with the guidelines of the Animal Care and Experimentation Committee at Gunma University. For the evaluation of in vitro stability, each ^{77}Br-BAMP was incubated in the murine plasma for 48 h. For the evaluation of in vivo stability, urine and blood were collected at 6 h after injection of each ^{77}Br-BAMP into normal ddY mice (Japan SLC). The radioactivity of the sample was analyzed by TLC and RP-HPLC.

We estimated the lipophilicity of BAMPs by measuring the coefficients of partition between 1-octanol and 0.1 M of phosphate buffer (pH 7.4). The plasma protein binding of the BAMPs was measured according to the procedure of Kuga et al. (*13*) with slight modification. The detailed methods are described in the Supplemental Information.

Cellular Uptake and Protein Incorporation Studies

A human colon adenocarcinoma cell line, LS180, was purchased from the American Type Culture Collection. LAT1- or LAT2-expressing HEK293-hLAT1 or HEK293-hLAT2 cells were

established previously (*14*). These cell lines were incubated with ^{18}F-FAMT, 2-^{77}Br-BAMP or 4-^{77}Br-BAMP at 37°C for 1 min. After the incubation, the cells were lysed and the radioactivity was measured by a well-type gamma counter (ARC-7001; Hitachi Aloka Medical). For the inhibition assay, various inhibitors were added to the well.

The protein incorporation of BAMPs was evaluated using the cell line LS180 and dissected tumors of tumor-bearing mice. The detailed methods are described in the Supplemental Information.

Biodistribution Studies

Tumor-bearing mice were prepared by the implantation of LS180 cells (5×10^6 cells/head) into the flanks of BALB/c nude mice (CLEA Japan). When palpable tumors had developed, the mice were used for biodistribution experiments. For the biodistribution studies, each ^{77}Br-BAMP (15 kBq, <5 pmol in 100 μL of saline) was injected into the tail vein of 6-wk-old ddY mice (weight, 27–30 g) or tumor-bearing mice (weight, 22–25 g). At selected time points after the injection, mice were sacrificed, and the tissues of interest were dissected out and weighed. The radioactivity was measured by a well-type gamma counter. The uptake of the tracers is expressed as a percentage of the injected dose per gram of organ. Radiation-effective doses for humans were calculated from the biodistribution data of normal mice using the software program OLINDA/EXM version 1.1 (Vanderbilt University). Urine

and feces samples were collected using metabolic cages (Metabolica TYPE MM-ST; Sugiyama-Gen Iriki Co.) at 6 h after administration.

PET Imaging

PET imaging was performed using an animal PET scanner (Inveon, Siemens). Tumor-bearing mice were prepared by the implantation of LS180 cells (5×10^6 cells/head) into the shoulder of mice. ^{18}F-FAMT (10 MBq, approx. 100 nmol) or 2-^{76}Br-BAMP (5 MBq, <1 nmol) was injected intravenously into LS180 tumor-bearing mice, and imaging was performed 1, 3 and 4 h later or 1, 3, 6 and 12 h later, respectively. The PET scans with ^{18}F-FAMT and 2-^{76}Br-BAMP were obtained from mice under isoflurane anesthesia for 10 min and 30 min (1, 3 and 6 h) or 60 min (12 h), respectively. Mean-SUV (SUV(m)) was determined by placing the region of interest (ROI) on the whole tumor or kidney.

Statistical Analyses

The statistical analyses were performed using the SYSTAT 13 software (Systat). Results are expressed as mean ± standard deviation (SD). The results were analyzed using the unpaired *t*-test for comparing differences between two groups, and by performing a one-way analysis of variance (ANOVA) followed by Tukey's honestly significant difference (HSD) test for comparing differences among multiple groups. Differences were considered significant when the *p*-value was less than 0.05.

RESULTS

Radiolabeling

The radiolabeling yield of the 2-^{76}Br-BAMP, 2-^{77}Br-BAMP and 4-^{77}Br-BAMP were 52.6 ± 11.9% (n=3), 64.5 ± 14.8% (n=5) and 57.1 ± 8.2% (n=4), respectively. The radiochemical purity of the BAMPs after purification by RP-HPLC was >95%. The stannyl precursor was removed by RP-HPLC purification, and the specific activity of 2-^{76}Br-BAMP was over 10 GBq/μmol.

Stability and Physicochemical Properties of 2-BAMP and 4-BAMP

Free bromine or other metabolites were not revealed by the RP-HPLC analysis of in vitro or the in vivo stability studies (Fig. 2). More than 95% of the 2-^{77}Br-BAMP and 4-^{77}Br-BAMP remained intact over 48 h after incubation in the plasma in vitro. At 6 h after the injection of 2-^{77}Br-BAMP, most of the radioactivity was eliminated, and no detectable peak was observed in the blood. More than 95% of the excreted radioactivity in the urine was intact at 6 h after the injection of 2-^{77}Br-BAMP, and >95% of the radioactivity in the blood and in the urine was intact at 6 h after the injection of 4-^{77}Br-BAMP. These results indicated that both ^{77}Br-BAMPs were stable in the murine body.

From the octanol/water partition coefficient measurement, the $logD_{7.4}$ values of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP were found to be −0.69 ± 0.00 and −0.21 ± 0.00, respectively (p<0.01), indicating that the lipophilicity of 2-BAMP was lower than that of 4-BAMP. This result was consistent with that of the RP-HPLC analysis of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP (Suppl. Fig. S1). The percentage binding of 2-^{77}Br-BAMP to murine plasma protein was significantly lower than that of 4-^{77}Br-BAMP (24.2 ± 2.2% vs. 44.5 ± 2.9%, respectively, p<0.01).

Cellular Uptake and Protein Incorporation Studies

The cellular uptake of 2-^{77}Br-BAMP to LS180 cells was significantly higher than that of ^{18}F-FAMT, whereas that of 4-^{77}Br-BAMP was similar to that of ^{18}F-FAMT (Fig. 3A). The uptake of both radiotracers was markedly reduced by co-incubation with some natural amino acids and LAT1 inhibitors (BCH [2-aminobicyclo-(2,2,1)-heptane-2-carboxylic acid] and AMT [α-methyl-L-tyrosine]), and it showed nearly the same reducing pattern as that of ^{18}F-FAMT (Fig. 3B), indicating that same amino acid transporters would be involved in the uptake of all three tracers. In addition, the uptake of 2-^{77}Br-BAMP was significantly enhanced by LAT1 transfection into HEK293 cells, whereas it was unaffected by LAT2 transfection (Fig. 3C).

Although a very small amount of radioactivity was observed in protein fraction after 6-h incubation with LS180 cells, more than 90% of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP remained intact

(Suppl. Fig. S3). No radioactivity in the tumor was observed in the protein fraction at 1 h after the injection of 2-^{77}Br-BAMP or 4-^{77}Br-BAMP.

Biodistribution Studies

In our biodistribution studies using normal mice, 2-^{77}Br-BAMP showed much more rapid blood clearance and lower renal accumulation compared to 4-^{77}Br-BAMP (Table 1). More than 90% of the injected radioactivity was excreted in the urine by 6 h after the injection of 2-^{77}Br-BAMP. In tumor-bearing mice, 2-^{77}Br-BAMP showed rapid blood clearance and high tumor accumulation, resulting in a high tumor-to-blood ratio and tumor-to-muscle ratio (Table 2). Moreover, since the renal clearance was also rapid, the tumor-to-kidney ratio became >1 at 1 h post-injection. In contrast, 4-^{77}Br-BAMP was retained in the blood and in many organs of the tumor-bearing mice, and consequently the tumor-to-blood ratio or tumor-to-organs ratio were low. The effective doses of 2-^{76}Br-BAMP and 4-^{76}Br-BAMP in human were calculated to be roughly 3.37×10^{-2} and 11.1 mSv/MBq, respectively.

PET Imaging

As shown in Figure 4, 2-^{76}Br-BAMP clearly enabled the imaging of tumors at 1, 3 h and 6 h post-administration, but most of radioactivity had disappeared from the body at 12 h. Although high levels of accumulation were observed in the kidney at 1 h after the administration, the levels decreased

in a time-dependent manner. ^{18}F-FAMT also accumulated in the tumors; however, the renal accumulation was much higher than that of the tumors at early time points, which could disrupt the detection of the tumors.

DISCUSSION

We considered the involvement of dehalogenase in the in vivo debromination of ^{76}Br-BAMT, and we designed new radiobrominated amino acids by replacing L-tyrosine with L-phenylalanine in order to remove the hydroxyl group vicinal to radiobromine. Since the chemical properties of bromine are close to those of iodine, radiobromine can be directly introduced on an aromatic group by a destannylation reaction with a positively charged radiobromine species generated by the presence of *N*-chlorosuccinimide as an oxidizing agent. Both compounds were obtained at fair to good radiochemical yields.

We also estimated the in vivo stability of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP in normal mice. 2-^{77}Br-BAMP exhibited rapid elimination from the whole body, and 90% of the injected dose was excreted intact in the urine by 6 h post-injection, indicating high in vivo stability of 2-^{77}Br-BAMP. 4-^{77}Br-BAMP showed a slow elimination rate from the whole body including blood, even compared to ^{77}Br-BAMT (*9*). However, the analysis of blood samples taken at 6 h post-injection showed a single peak identical to that of 4-^{77}Br-BAMP, suggesting that 4-^{77}Br-BAMP also possesses high resistance against in vivo debromination.

In our biodistribution studies, 2-^{77}Br-BAMP rapidly cleared from the blood and the body, whereas 4-^{77}Br-BAMP showed extremely slow blood clearance and high retention in the body. Similar phenomenon was also observed in ^{123}I-iodo-phenylalanine (*15*). The preferred pharmacokinetics of 2-^{77}Br-BAMP would be attributable to its low plasma protein binding and high hydrophilicity compared to 4-^{77}Br-BAMP. However, further studies are needed to fully elucidate the effect of the substitution position on the biodistribution. The tumor accumulation level and the tumor-to-blood ratio of 2-^{77}Br-BAMP were comparable to those of the ^{18}F-FAMT (*9*) (tumor accumulation: 4.45 ± 1.21 vs. 4.19 ± 0.65%ID/g, and tumor-to-blood ratio: 4.09 ± 1.08 vs. 4.80 ± 0.97 at 1 h post-injection, respectively). In addition, the tumor-to-kidney ratio of 2-^{77}Br-BAMP was much higher than that of ^{18}F-FAMT (1.14 ± 0.27 vs. 0.17 ± 0.04 at 1 h post-injection, respectively).

The high selectivity toward LAT1 over LAT2 is essential to tumor-imaging agents, since LAT1 is highly overexpressed in many types of tumor cells, whereas LAT2 is expressed in normal cells (*16-19*). The cell uptake of both 2-^{77}Br-BAMP and 4-^{77}Br-BAMP was competitively inhibited by amino acids known as the LAT1 substrates, similar to ^{18}F-FAMT used as a LAT1 selective tracer (*20*), indicating that both 2-^{77}Br-BAMP and 4-^{77}Br-BAMP would be taken up into tumor cells via LAT1 transporter. Both 2-^{77}Br-BAMP and 4-^{77}Br-BAMP were less incorporated into protein, similarly to ^{18}F-FAMT (*21*). The cell uptake of 2-^{77}Br-BAMP was significantly higher than those of 4-^{77}Br-BAMP and ^{18}F-FAMT. In addition, the cell uptake of 2-^{77}Br-BAMP was significantly increased by transfection with LAT1 but not by transfection with LAT2, indicating that 2-^{77}Br-BAMP was transported into cells

via LAT1 but not via LAT2. These findings indicated that while the presence of an α-methyl group would be favorable for the preferable recognition by the LAT1 transporter system, the position of bromine in α-methyl phenylalanine played a crucial role in the affinity for the LAT1 transporter system. The impact of the bromine position on the LAT1 affinity of BAMP isomers remains unsettled, and further studies are needed to elucidate the mechanism. However, similar phenomena were also observed in iodohippuric acid for the renal organic anion transporter (*22*) and iodo-benzylguanidine for the norepinephrine transporter (*23*). Overall, the present findings demonstrated that 2-^{77}Br-BAMP possesses high resistance against in vivo debromination, and higher affinity to LAT1 transporter than that of FAMT with high selectivity toward LAT1 over LAT2.

Such favorable properties of 2-Br-BAMP were well reflected in the PET images. The PET images with 2-^{76}Br-BAMP were well correlated with the biodistribution study. 2-^{76}Br-BAMP provided the visualization of tumorous lesions more clearly than did ^{18}F-FAMT, indicating the high potential of 2-^{76}Br-BAMP as a new tumor-imaging PET probe. Although human studies are needed, 2-^{76}Br-BAMP may detect various tumors such as lung and brain tumors, lymphomas, melanomas and maxillofacial tumors as well as ^{18}F-FAMT does (*24-27*). In addition to the relatively long half-life of ^{76}Br, 2-^{76}Br-BAMP exhibited slower elimination rates from the tumor than from the kidney, and thus a delayed-phase scan may visualize the tumor even if it is in the urinary tract. In the future, 2-^{76}Br-BAMP is expected to be widely used not only for the differential diagnosis of malignant tumors

in concert with ^{18}F-FDG but also for the diagnosis of brain, liver and urinary tract tumors which would be difficult to detect with ^{18}F-FDG.

Since ^{76}Br has a relatively long half-life, the high radiation dose is of concern. 2-^{76}Br-BAMP was rapidly excreted into the urine, and free bromine was not observed in the body. Consequently, the effective dose of 2-^{76}Br-BAMP was estimated to be roughly 3.37×10^{-2} mSv/MBq, which is similar to that of ^{18}F-labeled PET tracers. This again suggests the potential use of 2-^{76}Br-BAMP in clinical practice. On the other hand, the estimated dose of 4-^{76}Br-BAMP was high (11.1 mSv/MBq). These results indicated that the high radiation dose is caused by the long retention of radioactivity in the body rather than the long half-life of ^{76}Br. Therefore, it is desirable to develop novel ^{76}Br-labeled tracers that can be rapidly cleared from the body.

CONCLUSION

In the present study, 2-^{77}Br-BAMP exhibited preferred pharmacokinetics and showed higher LS180 cell uptake via LAT1 compared to 4-^{77}Br-BAMP or ^{18}F-FAMT. 2-^{77}Br-BAMP also showed high levels of tumor accumulation and 2-^{76}Br-BAMP enabled clear visualization of the tumor by PET imaging. These findings suggest that 2-^{76}Br-BAMP could constitute a potential new PET tracer for tumor imaging and may eventually enable the wider use of amino acid tracers.

DISCLOSURE

The costs of publication of this article were defrayed in part by the payment of page charges. Therefore, and solely to indicate this fact, this article is hereby marked “advertisement” in accordance with 18 USC section 1734. This work was supported by a Grant-in-Aid for Young Scientists (A) (22689035) to H.H. from the Ministry of Health, Labor and Welfare. No other potential conflict of interest relevant to this article was reported.

ACKNOWLEDGEMENTS

For the operation of the AVF cyclotron, we thank Mr. Hiroyuki Suto and the staff of Takasaki Ion Accelerators for Advanced Radiation Applications. We thank Dr. Satoshi Watanabe for preparing the no-carrier-added radiobromine.

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Fig. 1

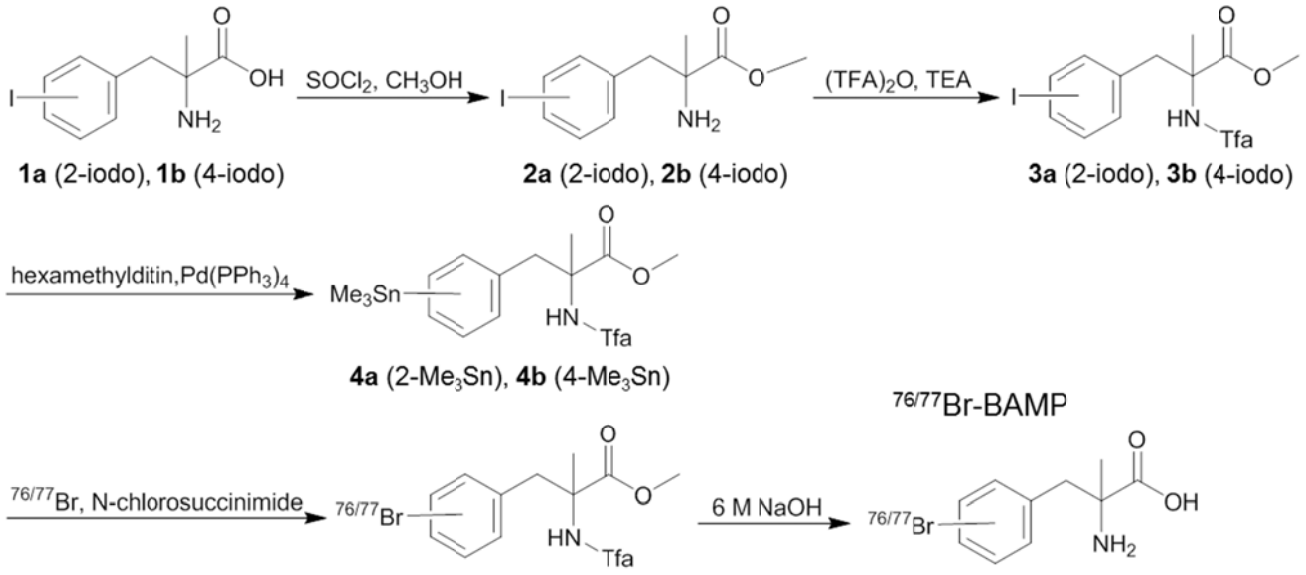

Fig. 1. Synthesis of 2-BAMP and 4-BAMP.

Fig. 2

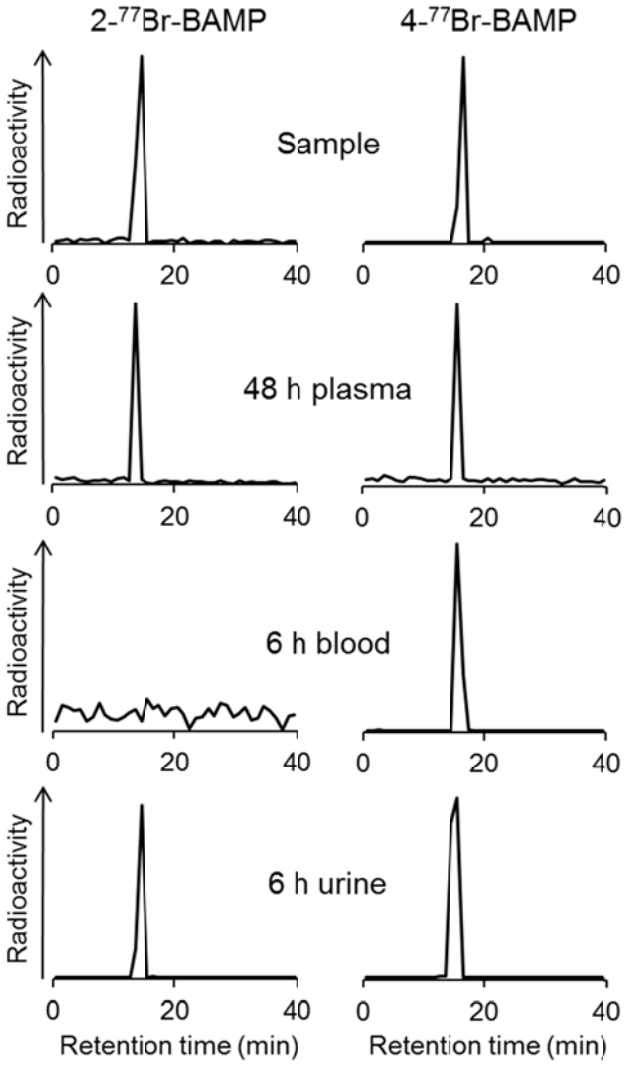

Fig. 2. Analytical RP-HPLC profiles of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP after incubation in murine plasma for 48 h and in a blood sample drawn from the heart of a mouse or a urine sample collected at 6 h after the administration of 2-^{77}Br-BAMP or 4-^{77}Br-BAMP. The retention time of free bromine was 2–3 min.

Fig. 3

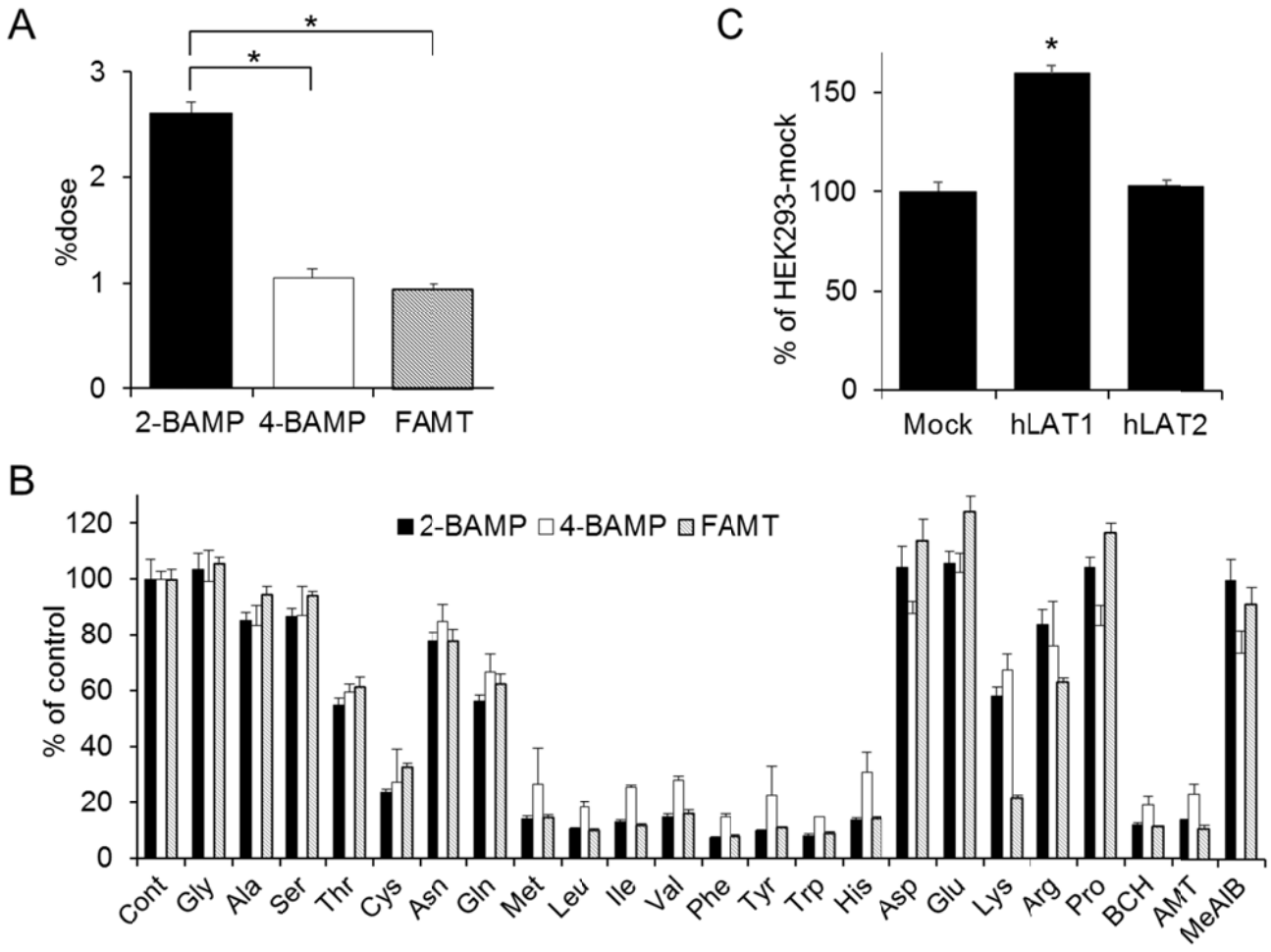

Fig. 3. Cellular uptake studies. (A) Cellular uptake of 2-^{77}Br-BAMP, 4-^{77}Br-BAMP and ^{18}F-FAMT into LS180 cells. Significant differences were determined (*p<0.01). (B) Inhibition of the cellular uptake of 2-^{77}Br-BAMP, 4-^{77}Br-BAMP or ^{18}F-FAMT into LS180 cells by L-amino acids or these analogs. BCH: 2-aminobicyclo-(2,2,1)-heptane-2-carboxylic acid; AMT: α-methyl-L-tyrosine; MeAIB: α-methyl-aminoisobutyric acid. (C) The cellular uptake of 2-^{77}Br-BAMP into HEK293-mock,

HEK293-hLAT1 or HEK293-hLAT2 cells. Significant differences compared with HEK293-mock group were determined (*p<0.01).

Fig. 4

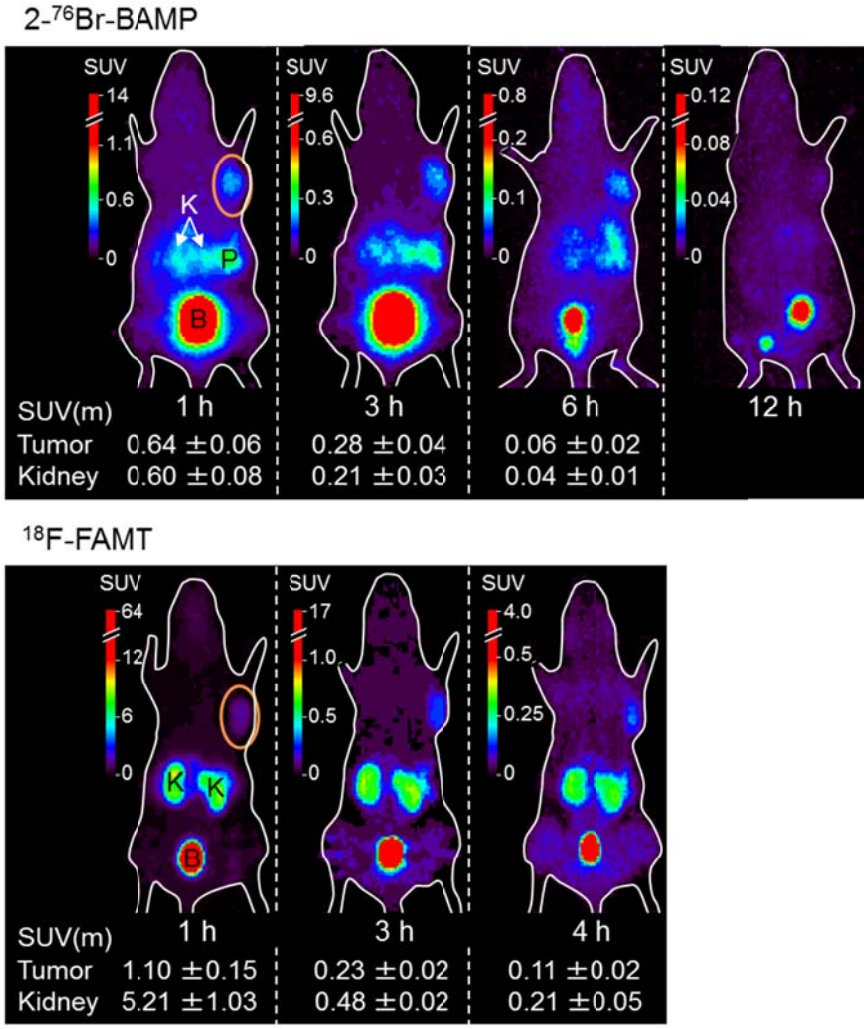

Fig. 4. A typical PET image and SUV(m) in the tumor and kidney of LS180-bearing mice injected with 2-^{76}Br-BAMP and ^{18}F-FAMT. Orange circles indicate the implanted tumors. K: kidney; P: pancreas; B: bladder. SUV(m) represents means ± SD of 3 mice.

Table 1. Biodistribution of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP in normal mice

	Time after injection				
	10 min	30 min	1 h	3 h	6 h
2-^{77}Br-BAMP					
Blood	2.43 ± 0.17	1.28 ± 0.08	0.55 ± 0.19	0.05 ± 0.02	0.00 ± 0.00
Liver	2.93 ± 0.11	1.74 ± 0.59	0.89 ± 0.68	0.13 ± 0.12	0.02 ± 0.01
Kidney	9.89 ± 1.75	6.28 ± 2.44	3.15 ± 0.98	0.47 ± 0.17	0.04 ± 0.04
Intestine	1.64 ± 0.09	1.05 ± 0.13	0.56 ± 0.13	0.20 ± 0.24	0.01 ± 0.00
Spleen	2.98 ± 0.13	1.45 ± 0.11	0.60 ± 0.17	0.00 ± 0.00	0.01 ± 0.03
Pancreas	15.74 ± 1.68	7.03 ± 0.52	3.28 ± 1.32	0.23 ± 0.07	0.00 ± 0.01
Lung	2.33 ± 0.17	1.34 ± 0.36	0.77 ± 0.61	0.02 ± 0.03	0.00 ± 0.01
Heart	2.84 ± 0.15	1.41 ± 0.09	0.74 ± 0.22	0.02 ± 0.04	0.00 ± 0.00
Stomach[a]	0.80 ± 0.27	0.38 ± 0.03	0.21 ± 0.05	0.13 ± 0.19	0.01 ± 0.02
Urine[b]					90.86 ± 7.07
Feces[b]					0.07 ± 0.03
4-^{77}Br-BAMP					
Blood	4.04 ± 0.04	3.11 ± 0.27	2.96 ± 0.17	2.04 ± 0.31	0.68 ± 0.34
Liver	4.91 ± 0.27	3.92 ± 0.45	3.53 ± 0.23	2.50 ± 0.47	0.83 ± 0.39
Kidney	28.42 ± 6.57	23.98 ± 2.64	22.00 ± 2.67	15.24 ± 3.49	5.32 ± 1.95
Intestine	3.25 ± 1.05	2.32 ± 0.35	1.98 ± 0.10	1.41 ± 0.34	0.45 ± 0.21
Spleen	5.07 ± 0.36	4.29 ± 0.61	3.61 ± 0.23	2.49 ± 0.73	0.77 ± 0.31
Pancreas	30.20 ± 3.46	24.91 ± 4.23	19.37 ± 3.41	13.98 ± 3.67	5.43 ± 3.10
Lung	4.07 ± 0.12	3.39 ± 0.27	3.07 ± 0.10	2.17 ± 0.41	0.69 ± 0.32
Heart	4.36 ± 0.11	4.09 ± 0.42	3.63 ± 0.15	2.45 ± 0.53	0.82 ± 0.33
Stomach[a]	1.39 ± 0.28	1.14 ± 0.38	0.94 ± 0.13	0.83 ± 0.20	0.35 ± 0.22
Urine[b]					24.22 ± 6.91
Feces[b]					3.33 ± 3.26

Each value represents the mean % injected dose/g of organ ± SD (n=5).

Each value represents the mean % injected dose ± SD ([a]n=5, [b]n=3).

Table 2. Biodistribution of 2-^{77}Br-BAMP and 4-^{77}Br-BAMP in tumor-bearing mice

	Time after injection			
	30 min	1 h	3 h	6 h
2-[^{77}Br]-BAMP				
Blood	2.19 ± 0.22	1.09 ± 0.15	0.16 ± 0.07	0.04 ± 0.03
Liver	2.71 ± 0.30	1.20 ± 0.16	0.16 ± 0.10	0.03 ± 0.01
Kidney	9.09 ± 1.15	3.89 ± 0.54	0.39 ± 0.16	0.10 ± 0.02
Intestine	1.97 ± 0.50	0.97 ± 0.11	0.17 ± 0.13	0.04 ± 0.01
Pancreas	27.28 ± 7.46	10.21 ± 2.96	1.26 ± 0.89	0.11 ± 0.02
Muscle	3.55 ± 1.35	1.62 ± 0.07	0.28 ± 0.28	0.05 ± 0.05
Tumor	5.17 ± 0.53	4.45 ± 1.21	1.08 ± 0.40	0.32 ± 0.07
Tumor/blood ratio	2.36 ± 0.08	4.09 ± 1.08	7.03 ± 0.92	6.40 ± 2.48
Tumor/muscle ratio	1.57 ± 0.37	2.74 ± 0.62	6.46 ± 3.42	6.44 ± 5.48
Tumor/kidney ratio	0.57 ± 0.07	1.14 ± 0.27	2.89 ± 0.43	3.22 ± 0.65
4-[^{77}Br]-BAMP				
Blood	4.01 ± 0.41	3.89 ± 0.29	3.63 ± 0.27	2.88 ± 0.82
Liver	5.62 ± 0.66	5.31 ± 0.49	4.46 ± 0.36	3.43 ± 0.92
Kidney	34.49 ± 6.12	29.78 ± 2.69	31.42 ± 4.04	22.09 ± 6.42
Intestine	3.54 ± 0.58	3.45 ± 0.54	2.77 ± 0.64	2.15 ± 0.65
Pancreas	31.71 ± 2.25	34.97 ± 4.24	27.36 ± 3.43	20.54 ± 7.97
Muscle	3.19 ± 0.61	3.53 ± 0.26	3.53 ± 0.17	2.78 ± 0.76
Tumor	4.69 ± 1.31	7.61 ± 1.88	7.19 ± 1.50	5.62 ± 1.12
Tumor/blood ratio	1.17 ± 0.28	1.95 ± 0.45	1.97 ± 0.31	2.03 ± 0.45
Tumor/muscle ratio	1.51 ± 0.46	2.14 ± 0.40	2.03 ± 0.38	2.09 ± 0.43
Tumor/kidney ratio	0.13 ± 0.02	0.26 ± 0.06	0.23 ± 0.06	0.27 ± 0.07

Each value represents the mean % injected dose/g of organ ± SD ($n \geq 4$).