Metabolic and Molecular Imaging of Atherosclerosis

and Venous Thromboembolism

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## **ABSTRACT**

Metabolic and molecular imaging continues to advance our understanding of vascular disease pathophysiology. At present, <sup>18</sup>F-fluorodeoxyglucose (<sup>18</sup>F-FDG) positron emission tomography (PET) imaging is the most widely utilized clinical tool for metabolic and molecular imaging of atherosclerosis. However, novel nuclear tracers and intravascular optical near-infrared fluorescence (NIRF) imaging catheters are emerging to assess new biological targets in vivo and in coronary arteries. This review highlights current metabolic and molecular imaging clinical and near-clinical applications within atherosclerosis and venous thromboembolism (VTE), and explores the potential for metabolic and molecular imaging to impact patient-level risk prediction and disease treatment.

# **INTRODUCTION**

"Prediction is very difficult, especially if it's about the future."

-Niels Bohr

In this focused review, we showcase state-of-the-art molecular imaging applications to atherosclerosis and VTE. Clinical or near-clinical applications will be highlighted, illuminating how molecular imaging can provide insights into disease pathophysiology, risk prediction and management.

# I. ATHEROSCLEROSIS

### **Background**

Atherosclerosis is the primary cause of heart attack, stroke, and limb ischemia, and remains a leading cause of death worldwide. Clinical atherosclerosis imaging traditionally assesses anatomical measures such as luminal stenosis. However, imaging of structural features provides limited insights into the pathobiology central to atherosclerosis disease progression, which is a biological consequence of accumulated inflammatory cells and oxidized lipids within the vessel wall. Molecular imaging is a complementary approach that provides new insights into mechanisms of atherosclerosis

progression and complications. For larger arteries (carotid, iliac, aorta), <sup>18</sup>F-FDG-PET imaging currently predominates to detect plaque inflammatory cells (macrophages). In the smaller-sized coronary arteries, <sup>18</sup>F-sodium fluoride (<sup>18</sup>F-NaF)-PET and high-resolution intravascular NIRF molecular imaging are emerging new approaches to image plaque mineralization and inflammation (e.g. protease activity), respectively.

## <sup>18</sup>F-Fluorodeoxyglucose Positron Emission Tomography

In atherosclerosis, the most widely utilized PET tracer is <sup>18</sup>F-FDG, a glucose analogue consumed by metabolically active cells. <sup>18</sup>F-FDG possesses a 110-minute half-life and maximum 2.4 mm positron range. Following phosphorylation, trapped intracellular <sup>18</sup>F-FDG-6-phosphate cannot proceed down glycolytic pathways and accumulates in direct relation to the degree of cellular glycolysis, substantially reflecting plaque macrophage content.

Association with cardiovascular risk factors and prediction of cardiovascular events. Atherosclerosis <sup>18</sup>F-FDG-PET metabolic imaging is positioned to improve risk prediction beyond structural imaging measures, by predicting atheroma progression and subsequent clinical events, and to tailor atheroma pharmacotherapies.

Risk factors (e.g. smoking, diabetes mellitus, hyperlipidemia, hypertension) are established predictors of cardiovascular events on a population-based level. To assess relationships between cardiac risk factors and  $^{18}\text{F-FDG-PET}$ , Noh et al. measured  $^{19}\text{F-FDG}$  carotid plaque uptake in 1,181 asymptomatic subjects, and correlated the results with 10-year FRS (mean  $12.3\pm8.7\%$ , indicating intermediate risk) (1). The authors determined that an elevated carotid plaque  $^{18}\text{F-FDG}$  uptake (mean target-to-background ratio (TBR) $\geq$ 1.7) increased the chance of having an elevated FRS  $\geq$ 10% (odds ratio 1.9).  $^{18}\text{F-FDG}$  uptake has also been associated with other risk factors. One study explored the relationship between plaque inflammation (by  $^{18}\text{F-PET}$ ) and atherogenic lipoprotein(a) (Lp(a)), a pro-inflammatory oxidized phospholipid transporter associated with accelerated arterial inflammation. Compared to 30 matched subjects with normal Lp(a) levels, those with elevated Lp(a) manifested greater arterial inflammation (2).

Beyond risk factors, imaging arterial inflammation may provide direct insights into atherosclerosis progression. Cho et al. recently observed that aortic <sup>18</sup>F-FDG-PET uptake predicted the progression of coronary calcification at 1 year (3). In 96 subjects without known coronary disease or statin use, elevated aortic <sup>18</sup>F-FDG uptake significantly associated with incident coronary calcification (OR: 4.39, p=0.007). Similarly, Abdelbaky et al.

demonstrated that local <sup>18</sup>F-FDG uptake predicts incident calcium deposition in the underlying atheroma (4).

More importantly, several retrospective studies have shown that aortic <sup>18</sup>F-FDG uptake independently predicts cardiovascular disease (CVD) risk above the FRS (*5*), and evolving data supports prospective <sup>18</sup>F-FDG-PET imaging. <sup>18</sup>F-FDG-PET carotid arterial inflammation independently predicted recurrent ipsilateral cerebrovascular events in 60 patients with recent stroke (*6*). Accordingly, <sup>18</sup>F-FDG-PET / computed tomography (CT) arterial imaging may provide additive prognostic information beyond risk factor assessment and structural imaging data.

<sup>18</sup>F-FDG-PET imaging has yielded insights into how adipose tissue, particularly visceral adiposity, associates with heightened cardiovascular risk. Figueroa et al. evaluated CT adipose tissue <sup>18</sup>F-FDG-PET arterial inflammation and cardiovascular events in 415 asymptomatic patients (mean body mass index: 26.4 kg/m²) (7). Visceral fat volume correlated positively with <sup>18</sup>F-FDG inflammation (r=0.290, p<0.001). Over 4 years, the visceral fat volume associated with increased cardiovascular event risk (HR: 1.15, p<0.001; HR: 3.60, p<0.001, respectively). In a separate 443 patient study, <sup>18</sup>F-FDG-PET signal in plaques and brown adipose tissue, a metabolically active tissue present in childhood that regresses with age, demonstrated that

brown fat  $^{18}\text{F-FDG}$  activity correlated negatively with  $^{18}\text{F-FDG}$  arterial inflammation (r=-0.147, P<0.01) (8). Brown fat  $^{18}\text{F-FDG}$  uptake was further associated with improved cardiac event free survival (p=0.048). These data support the notion that visceral fat spurs arterial inflammation and subsequent events, and that brown fat may be protective.

Patients with acute coronary syndrome (ACS) harbor a heightened risk of repeat cardiovascular events. Pathophysiologically, recent preclinical mechanistic studies support splenic and bone marrow (the cardiospenic axis) activation as mediators of activated leukocyte trafficking and subsequent atheroma progression. Emami et al. imaged 22 ACS patients demonstrating increased <sup>18</sup>F-FDG spleen uptake compared to non-ACS controls (Fig. 1; standardized uptake value: 2.6±0.6 vs. 2.1±0.3, p=0.03) (9). A 464 patient substudy revealed that subjects with increased <sup>18</sup>F-FDG splenic activity experienced more cardiac events (HR: 3.3, p=0.003), even after adjustment for CVD risk factors. These results support the clinical importance of the cardiosplenic axis in humans, and motivate CVD preventative strategies against pro-inflammatory leukocyte emigration.

New clinical disease insights in atherosclerosis. Plaque inflammation drives atherosclerosis progression and clinical events, as evidenced by heightened CVD in patients with inflammatory rheumatological diseases. To examine this

association, Naik et al. performed  $^{18}\text{F-FDG-PET}$  in 60 psoriasis patients without known CVD, and found that aortic  $^{18}\text{F-FDG}$  uptake increased proportionately to psoriasis disease severity, even after adjustment for age, sex, and calculated FRS ( $\beta$ =0.41, p=0.001) (10). A separate study of 38 familial hypercholesterolemia subjects underwent serial  $^{18}\text{F-FDG-PET}$  imaging at baseline (Fig. 2), and then 3 days later after lipoprotein apheresis (11). Apheresis-based low-density lipoprotein reduction (284±118 vs. 127±50 mg/dl, p<0.001) rapidly lowered arterial  $^{18}\text{F-FDG}$  activity (TBR: 2.05±0.31 pre vs. 1.91±0.33 post, p<0.02). This intriguing data informs that atherogenic lipoprotein-induced arterial inflammation may be quickly reversible, supporting potent lipid therapy use in ACS.

Evaluation of anti-atherosclerosis pharmacotherapies. As arterial inflammation remains an important pharmacotherapeutic target, several studies have recently harnessed <sup>18</sup>F-FDG-PET to assess the in vivo anti-inflammatory effects of novel atherosclerosis pharmacotherapies. Thus far there exist 5 compound classes where both clinical endpoint and PET imaging data are available. For two of these five drug classes (statins and thiazolidinediones), imaging and clinical endpoint trial results have been concordantly positive (12,13). On the other hand, for three of five drug classes (cholesteryl ester transfer protein inhibitor, lipoprotein-associated

phospholipase A2 inhibitor, and P38 MAP Kinase inhibitors), imaging and clinical endpoint trials have been concordantly neutral (14-18). Hence, thus far there appears to be concordance between directional changes in arterial imaging and clinical efficacy. Furthermore, <sup>18</sup>F-FDG-PET/CT trials are typically small (roughly 35 to 60 subjects per group) and fast (3-6 month treatment intervals), and thus have the potential to presage pharmacotherapeutic efficacy in considerably longer and more expensive outcomes trials of several thousand individuals.

### Intravascular near-infrared fluorescence molecular imaging

Intravascular NIRF is an emerging optical molecular imaging approach designed for high-resolution coronary arterial imaging. NIRF imaging employs injectable fluorescent imaging agents that target key cellular and molecular processes in vivo. NIR light (~700-900 nm excitation) not only offers greater tissue penetration and reduced autofluorescence compared to visible light, but NIRF imaging can be performed via coronary arterial-compatible catheters, and through blood without flushing. These attributes support intravascular NIRF as a viable coronary arterial molecular imaging method.

Jaffer et al. engineered and tested a fully-automated rotational 2D NIRF imaging catheter in rabbit atheroma to detect NIRF inflammatory cysteine

protease activity with nanomolar sensitivity (19). Stent-induced inflammatory vascular injury was also demonstrated, suggesting the potential to understand how inflammation may predict restenosis in living subjects. Translationally, indocyanine green (ICG), an FDA-approved NIRF imaging agent, has shown promise for intravascular NIRF imaging (20). A clinical ICG study very recently reported that ICG serves as a human in vivo plaque imaging agent in carotid endarterectomy specimens (21). ICG was reliably detected by ex vivo NIRF imaging and NIR fluorescence microscopy, and was found to report on endothelial barrier compromise, and deposited in adjacent areas macrophage infiltration and plaque hemorrhage (Fig. 3).

As standalone NIRF imaging is limited by a lack of anatomical information, a next-generation intravascular NIRF imaging system incorporating co-registered optical coherence tomography (OCT) structural imaging was constructed (22). Integrated NIRF-OCT imaging combines high-sensitivity NIRF detection with exquisite 10-20 µm OCT spatial resolution, and can illuminate inflammatory plaque protease activity in experimental atherosclerosis, as well as fibrin deposition on clinical-grade coronary stents (23). Recently, first-in-human intracoronary NIRF-OCT imaging was successfully performed to image NIR autofluorescence in 12 patients (24). With additional development, including integrating NIRF with intravascular

ultrasound (25), intravascular NIRF imaging is positioned to transform clinical molecular imaging of coronary atherosclerosis and stents.

#### II. VENOUS THROMBOEMBOLISM

## **Background**

Deep venous thrombosis (DVT) and pulmonary embolism (PE), collectively known as VTE, remain leading causes of morbidity and mortality worldwide. Diagnostically, compression ultrasonography and CT pulmonary angiography are the primary clinical imaging modalities for assessing DVT and PE, respectively. While ultrasound and CT pulmonary angiography are well-validated for diagnosing VTE, they have limited ability to diagnose recurrent VTE, predict the efficacy of fibrinolytic therapy for PE, or predict debilitating complications such as the DVT-induced post-thrombotic syndrome, or PE-induced chronic thromboembolic pulmonary hypertension.

VTE is an intertwined thrombotic and inflammatory process, consisting of an initial neutrophil infiltrate followed by a monocyte-macrophage influx. These cells coordinate to promote endogenous fibrinolysis, thrombus stabilization, and ensuing VTE resolution. A number of thrombus-targeted imaging agents have developed for PET or SPECT imaging (see Table for selected agents), but have not yet demonstrated diagnostic advantages over

anatomical US or CT imaging. However, VTE inflammation as an imaging target has undergone limited evaluation. Recently, <sup>18</sup>FDG-PET/CT imaging of VTE has been used in humans to assess DVT age. Future studies are needed to assess this tool's role in diagnosing recurrent DVT, a vexing clinical problem.

## <sup>18</sup>FDG-PET Imaging of VTE

*Primary DVT.* Rondina et al. performed the first prospective study demonstrating that <sup>18</sup>F-FDG-PET/CT is a sensitive imaging tool for detecting symptomatic, proximal first-time (primary) DVT. The authors observed significantly higher <sup>18</sup>F-FDG uptake in thrombosed vein segments over matched contralateral segments without thrombosis. <sup>18</sup>F-FDG was accurate in diagnosing DVT with 87.5% sensitivity and 100% specificity. While limited by a small sample size, this study demonstrated that the <sup>18</sup>FDG DVT uptake diminished over time (*26*).

Recurrent DVT. Recurrent DVT occurs up to 10% per year after an unprovoked DVT, and increases the risk of post-thrombotic syndrome, pulmonary embolism and death (27). While accurate diagnosis of recurrent same-site VTE is critical for justifying reinitiation of anticoagulation therapy, its diagnosis is challenging for conventional ultrasound due to residual vein

wall scarring and/or thrombus from the initial DVT. Recognizing that <sup>18</sup>F-FDG-PET can report on DVT metabolic/inflammatory activity, and that a recurrent DVT should generate a new inflammatory response, Hara et al. leveraged <sup>18</sup>F-FDG-PET/CT to accurately diagnose recurrent DVT in mice (Fig. 4) (28). Analysis of thrombosed veins showed that the majority of <sup>18</sup>F-FDG uptake was in the thrombus (70%), with a minority signal in the vein wall (30%). Furthermore, they observed that inflammatory <sup>18</sup>F-FDG DVT signal was more closely associated with neutrophils than macrophages, and that <sup>18</sup>F-FDG uptake was neutrophil-dependent and accordingly higher in early-stage, neutrophil-rich DVT. Finally the authors demonstrated that clinical <sup>18</sup>F-FDG uptake in DVT diminishes with increasing DVT age, extending earlier results.

Pulmonary embolism. Case reports and retrospective studies have described <sup>18</sup>F-FDG uptake in PE, mostly as incidental findings in whole-body cancer staging <sup>18</sup>F-FDG-PET/CT imaging sessions (29-31). As suspected, metabolically active tumors may mimic VTE <sup>18</sup>F-FDG enhancement, increasing the chances of false-positive diagnosis (32,33). Interestingly, delayed <sup>18</sup>F-FDG imaging (2 hours post-injection) may be more specific for PE and should be considered in future studies (30). While CT pulmonary angiography is the gold standard for PE diagnosis, <sup>18</sup>F-FDG-PET might also be

useful for detecting recurrent PE (28). In addition, <sup>18</sup>F-FDG-PET assessment of thrombus age could help predict the success of fibrinolytic therapies, as suggested by recent preclinical molecular imaging investigations (34,35).

## **SUMMARY AND FUTURE DIRECTIONS**

Atherosclerosis. As showcased above, metabolic and molecular imaging approaches have the potential to better predict clinical events, tailor selection of pharmacotherapeutic and interventional therapies, and assessment of pharmaceutical efficacy.

Large arterial beds. Larger arteries, in particular the carotid artery, are well suited to noninvasive PET imaging. Therefore we anticipate that future studies of carotid <sup>18</sup>F-FDG-PET will extend the initial insights provided by Marnane et al. (6), and better determine which carotid lesions are high-risk and warrant a more intensive medical or interventional approach. This is an area of vital importance, as there remains controversy about when to intervene on asymptomatic severe interval carotid artery lesions, and whether biological data (beyond currently available stenosis information) might help guide that decision (36). Risk-benefit of radiation exposure and cost-effectiveness will need to be further analyzed.

In addition to assessing plaque inflammation in clinical subjects, as robustly demonstrated (4,5,7-9,11,12,14,18), noninvasive carotid FDG PET/CT will continue to play a role in evaluating novel pharmacotherapy anti-inflammatory effects. New tracers have an opportunity to improve the ability to sensitively and specifically detect plaque inflammation (37), but will need outcomes validation to serve as a compelling challenger to FDG.

Coronary arterial imaging. Background cardiomyocyte metabolic signal, cardiorespiratory motion, and partial volume effects greatly impact the reliability to detect FDG signal in coronary arteries, particularly distal to the proximal coronary segments. In contrast, <sup>18</sup>F-Na PET does not suffer from myocardial background uptake and appears to be a reliable noninvasive option for imaging coronary plaque osteogenic activity/calcification. Future studies are needed to determine <sup>18</sup>F-Na's clinical value beyond widely available calcium scoring and CT angiography. There is also promise for this tracer to understand the potential effects of bisphosphonates and statins on the pathophysiology of coronary calcification.

Intravascular NIRF molecular imaging shows promise for high-resolution molecular imaging, and can be integrated with IVUS (25) or OCT (22), strengthening the ability to provide comprehensive molecular-structural imaging of atherosclerosis and stent biology. However, NIRF

imaging is in its infancy for clinical translation, and will require clinical outcome studies to determine its value. Given its invasive requirement, NIRF imaging will likely be used to further stratify patients already undergoing percutaneous coronary intervention (PCI) for ACS or stable angina.

VTE. The ability of FDG-PET to image VTE inflammation may provide a new opportunity to detect recurrent DVT, and may provide a foundation for guiding anticoagulation decisions. However, outcome and safety studies are needed. In addition FDG-PET may soon provide insights into the post-thrombotic syndrome, a common complication of DVT that is partly inflammation driven. For pulmonary embolism, new imaging tracers may help identify which thrombi are amenable to fibrinolysis, a question of particular importance given recent neutral data of fibrinolysis in patients with intermediate-risk pulmonary embolism (38).

# **CONCLUSION**

Metabolic and molecular imaging with <sup>18</sup>F-FDG-PET and other modalities are providing valuable insights into atherosclerosis and VTE pathophysiology in human subjects. <sup>18</sup>FDG-PET and emerging metabolic/molecular imaging technologies are expected to evolve as

outcomes studies emerge, and are further analyzed for cost-effectiveness and safety. Overall, these advances are expected to shed important insight into atherosclerotic disease pathophysiology, help identify novel treatment strategies, and improve clinical evaluation and management of individual patients.

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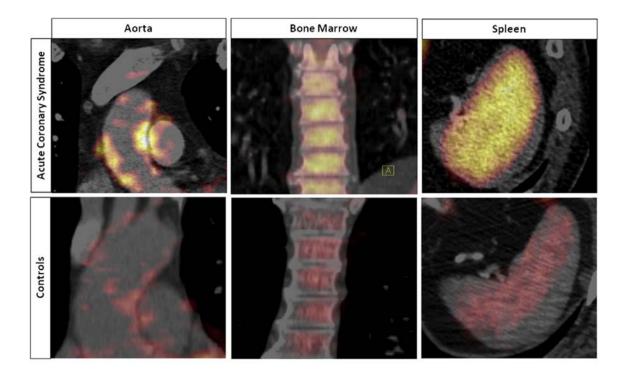


Figure 1. Evidence of a cardiosplenic axis in ACS patients. <sup>18</sup>F-FDG uptake is significantly increased in the aortic wall (left), bone marrow (middle), and spleen (right) in ACS patients compared to controls. Reprinted with permission from Emami et al. (9).

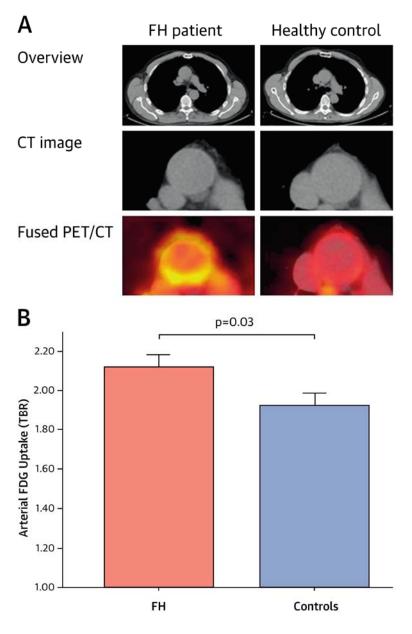


Figure 2.  $^{18}$ F-FDG-PET/CT inflammation imaging in familial hypercholesterolemia patients. (A)  $^{18}$ F-FDG uptake is elevated in the aorta of familial hypercholesterolemia subjects (left) compared to controls (right), as

quantified by (B) significantly higher mean arterial TBR. FH, familial hypercholesterolemia. Reprinted with permission from van Wijk et al. (11).

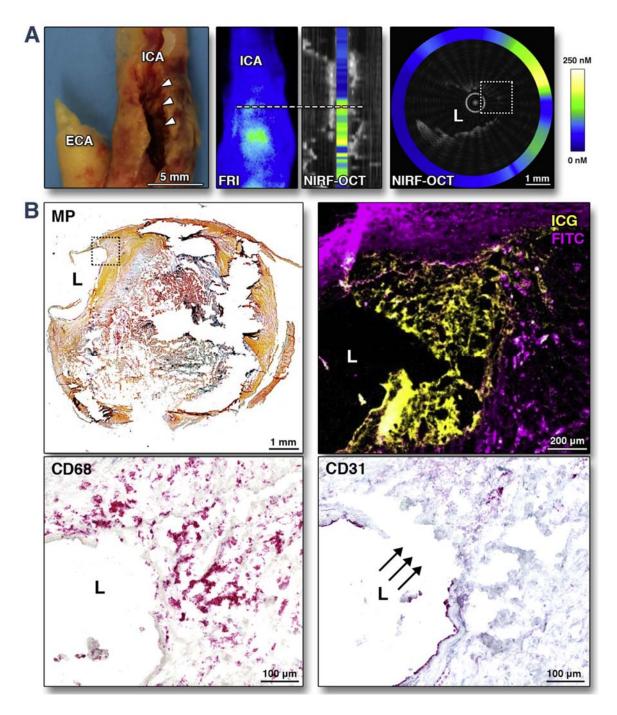


Figure 3. NIRF imaging of ICG deposition in human atheroma. (A) Aligned photo, fluorescence reflectance image (FRI), and long-view NIRF-OCT fusion

image of a resected human carotid atheroma. Ninety minutes after intravenous ICG administration, elevated ICG signal (green-yellow) presents the area of severe stenosis (arrowheads). NIRF-OCT cross-sectional image at the white dotted line shows a thinned/absent fibrous cap (white dotted box), with corresponding high NIRF ICG signal. (B) High-magnification histology reveals a complex plaque (top-left, Movat's Pentachrome (MP)) and surface ICG NIRF uptake (yellow, top-right). The ICG NIRF-positive areas demonstrate endothelial barrier disruption (CD31; arrows) and macrophage infiltration (CD68). ICA, internal carotid artery; L, lumen. Reprinted with permission from Verjans et al. (21).

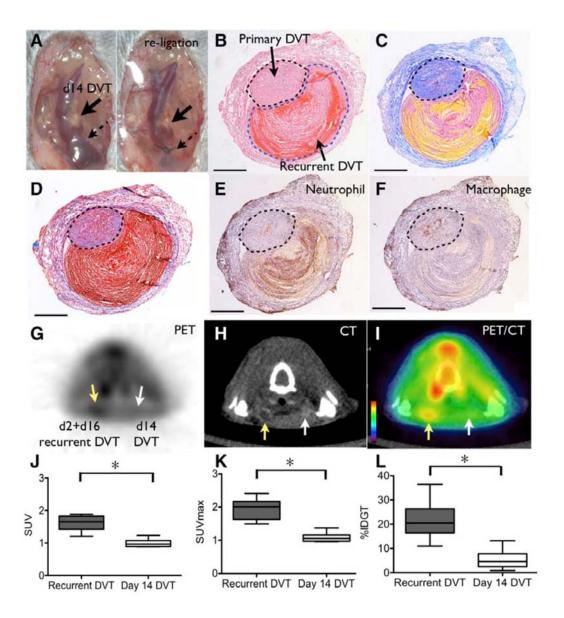


Figure 4. <sup>18</sup>F-FDG-PET/CT imaging of recurrent VTE. Mouse model illustrating day 14 DVT and the re-ligation of the jugular vein to create the recurrent DVT mouse model utilized in FDG-PET imaging (A). Histological staining with H&E (B), Carstairs (C), and Masson's Trichrome (D) of resected day 2 recurrent DVT (black dotted line) overlying the day 16 DVT (blue

dotted line) show red-blood cell and fibrin rich areas in recurrent DVT (red and yellow area in B-D) and collagen-rich zones in older primary DVT (blue areas in C and D). Immunostaining for neutrophils (E) and macrophages (F) highlight differences between recurrent DVT and older DVT. <sup>18</sup>F-FDG-PET/CT images (G-I) of recurrent and primary DVT show increased <sup>18</sup>F-FDG uptake in recurrent DVT (J-L). Yellow arrows, recurrent DVT. White arrows, primary day 16 DVT. Reprinted with permission from Hara et al. (28).

TABLE
Selected clinical and translational metabolic and molecular imaging agents for illuminating atherosclerosis and venous thromboembolism.

<u>Agent</u>	Applic ation	<u>Target</u>	Moda lity	Clinically tested?	<u>Reference</u>
<sup>18</sup> F-FDG	Athero	Macrophages, hypoxia	PET	Yes	Circulation. 2002;105:2708-2711 J Am Coll Cardiol. 2011;58:603-14
<sup>18</sup> F-sodium fluoride	Athero	Calcification	PET	Yes	J Nucl Med. 2015;56:1019-1023 Lancet. 2014;383:705-713
<sup>18</sup> F- fluorothymidine	Athero	Cell proliferation	PET	Yes	Circ Res. 2015;117:835-845
<sup>18</sup> F-fluorocholine	Athero	Cell proliferation	PET	Yes	Circ Cardiovasc Imaging. 2016;9:e004467
<sup>68</sup> Ga-dotatate	Athero	Somatostatin receptors	PET	Yes	J Am Coll Cardiol. 2013;62:2344-2345 J Am Coll Cardiol. 2017;69:1774-1791
<sup>68</sup> Ga-pentixafor	Athero	Macrophage CXC4 receptors	PET	Yes	J Nucl Med. 2016;Oct 27 epub
<sup>18</sup> F-galacto-RGD	Athero	ανβ3 integrins	PET	Yes	JACC Cardiovasc Imaging. 2014;7:178- 187
<sup>64</sup> Cu- ATSM	Athero	Macrophages	PET	Yes	J Nucl Med. 2016;57:2006-2011
<sup>64</sup> Cu-CANF-Comb	Athero	Macrophages	PET	Yes	J Nucl Med. 2010;51:85-91
USPIO	Athero	Macrophages	MRI	Yes	Circulation. 2003;107:2453-8
Indocyanine green	Athero	Endothelial permeability	NIRF	Yes	JACC Cardiovasc Imaging. 2016;9:1087-1095
<sup>99m</sup> Tc-apcitide	VTE	Platelet glycoprotein IIb/IIIa receptors	Scintig raphy	Yes	J Nucl Med. 1995;36:1384-1391 J Nucl Med. 2000;41:1214-1223
99mTc-DMP444	VTE	Platelet glycoprotein	Scintig raphy	Yes	Coron Artery Dis. 1998;9:131-141

<sup>111</sup> In-59D8	VTE	IIb/IIIa receptors Fibrin	Scintig raphy	Yes	J Nucl Cardiol. 2000;7:359-364 Science. 1983;222:1129-1132
					J Nucl Med. 1991;32:785-791
EP-2104R / FTP11	Athero, VTE	Fibrin	MRI SPECT NIRF	Yes / No	Eur Radiol. 2008;18:1995-2005 Contrast Medial Mol Imaging. 2013;8:229-237 JACC Cardiovasc Imaging. 2012;5:607-15 Circulation. 2014;130:1044-1052 Theranostics. 2015;5:1317-27
Prosense VM110	Athero	Cathepsin proteases	NIRF	No	J Am Coll Cardiol. 2011;57:2516-2526
MMR-Cy7	Athero	Macrophage mannose receptors	NIRF	No	Sci Rep. 2016;6:22608
<sup>18</sup> F- fluorodeoxyman nose	Athero	Macrophage mannose receptors	PET	No	Nat Med. 2014;20:215-219