18F-FDG PET/CT, 99mTc-MIBI, and MRI in Evaluation of Patients with Multiple Myeloma

Rosa Fonti1, Barbara Salvatore2, Mario Quarantelli1, Cesare Sirignano1, Sabrina Segreto3, Fara Petruzziello4, Lucio Catalano4, Raffaele Liuzzi1, Bruno Rotoli4, Silvana Del Vecchio3, Leonardo Pace3, and Marco Salvatore3

1Istituto di Biostrutture e Biomimagini-CNR, Napoli, Italy; 2Fondazione SDN-IRCCS, Naples, Italy; 3Diagnostic Imaging Department, University Federico II, Naples, Italy; and 4Hematology Department, University Federico II, Naples, Italy

New imaging techniques have been introduced to assess the extent and severity of disease in multiple myeloma (MM) patients. The aim of our study was to compare newer imaging modalities—such as 18F-FDG PET/CT, 99mTc-methoxyisobutylisonitrile (99mTc-MIBI) scintigraphy, and MRI—to assess their relative contribution in the evaluation of MM patients at diagnosis. Methods: Thirty-three newly diagnosed patients with MM were prospectively studied. Diagnosis and staging were made according to standard criteria. All patients underwent whole-body 18F-FDG PET/CT, whole-body 99mTc-MIBI, and MRI of the spine and pelvis within 10 d, and imaging findings were compared. Results: 18F-FDG PET/CT was positive in 32 patients (16 focal uptake, 3 diffuse uptake, 13 focal and diffuse uptake), 99mTc-MIBI was positive in 30 patients (6 focal, 11 diffuse, 13 focal and diffuse uptake), and MRI of the spine and pelvis was positive in 27 patients (6 focal, 13 diffuse, 8 focal and diffuse uptake). 18F-FDG PET/CT showed a total of 196 focal lesions (178 in bones and 18 in soft tissues), of which 121 were in districts other than the spine and pelvis, whereas 99mTc-MIBI visualized 63 focal lesions (60 in bones and 3 in soft tissues), of which 53 were in districts other than the spine and pelvis. In the spinal and pelvic regions, 18F-FDG PET/CT detected 75 focal lesions (35 in spine and 40 in pelvis), 99mTc-MIBI visualized 10 focal lesions (1 in spine and 9 in pelvis), and MRI detected 51 focal lesions (40 in spine and 11 in pelvis). Conclusion: In whole-body analysis, 18F-FDG PET/CT performed better than 99mTc-MIBI in the detection of focal lesions, whereas 99mTc-MIBI was superior in the visualization of diffuse disease. In the spine and pelvis, MRI was comparable to 18F-FDG PET/CT and 99mTc-MIBI in the detection of focal and diffuse disease, respectively. Because myelomatous lesions may often occur out of spinal and pelvic regions, MRI should be reserved to the evaluation of bone marrow involvement of these districts, whereas 18F-FDG PET/CT can significantly contribute to an accurate whole-body evaluation of MM patients. Finally, whole-body 99mTc-MIBI, despite its limited capacity in detecting focal lesions, may be an alternative option when a PET facility is not available.

Key Words: multiple myeloma; 18F-FDG-PET/CT; 99mTc-MIBI; MRI

DOI: 10.2967/jnumed.107.045641

Multiple myeloma (MM) is a malignant hematologic disorder characterized by proliferation of clonal plasma cells and overproduction of monoclonal immunoglobulins (1). Diagnosis and staging of MM is based on standardized criteria, including plasma cell infiltration of bone marrow, osteolytic bone lesions, and a monoclonal component in serum or urine (2,3). At present, the most used system for staging MM is that introduced by Durie and Salmon several years ago (3). In this staging system myelomatous bone lesions are traditionally detected by a whole-body radiographic survey; however, radiographs can significantly underestimate the extent of bone and bone marrow involvement, especially in early phases of the disease (4). Therefore, more advanced imaging modalities—including whole-body 18F-FDG PET/CT, whole-body 99mTc-methoxyisobutylisonitrile (99mTc-MIBI) scintigraphy, and MRI—have been proposed in the effort to improve the management of MM patients in a noninvasive manner (5–7). 18F-FDG PET/CT is a whole-body imaging technique capable of furnishing merged functional and morphologic information and is now routinely used in the staging and follow-up of lymphoma and various solid tumors. Moreover, previous studies have shown its usefulness in the detection of both osseous and extrasosseous myeloma lesions (8–10). The lipophilic cation 99mTc-MIBI has been successfully used for the detection of a variety of neoplastic diseases, including multiple myeloma, where it is reported to be useful in the assessment of disease extension both at diagnosis and during follow-up (11–22). MRI allows a direct high-contrast and sensitive visualization of the bone marrow and its components and, therefore, has become the method of choice for bone marrow imaging (23,24). Recently, the Scientific Advisors of the International Myeloma Foundation proposed a new staging system called “Durie and Salmon PLUS” based on the traditional Durie and Salmon system integrated by 18F-FDG PET or MRI of the
spine (25). This system attributes an equal relevance to both $^{18}$F-FDG PET and MRI of the spine, which can be used, as suggested by the guidelines, in a flexible fashion. However, the relative contribution of each imaging technique, the specific clinical contexts in which one technique should be preferred over the other, or, eventually, the need to perform both imaging studies have not been fully elucidated. In addition, $^{99m}$Tc-MIBI scans showed a high sensitivity and specificity in detecting sites of active disease and bone lesions (13). Despite several reports on the clinical usefulness of this imaging modality (11–22), it is still unclear whether $^{99m}$Tc-MIBI can be fully replaced by $^{18}$F-FDG PET/CT.

The aim of our study was to compare whole-body $^{18}$F-FDG PET/CT with whole-body $^{99m}$Tc-MIBI scintigraphy and MRI of the spine and pelvis to assess which of these imaging modalities would be more appropriate for detecting the presence of focal or diffuse disease and should, therefore, be included in the evaluation of patients with newly diagnosed MM.

MATERIALS AND METHODS

Thirty-three patients (11 females, 22 males; mean age ± SD, 64 ± 12 y) with newly diagnosed MM according to standard criteria were enrolled in this prospective study, which had undergone institutional approval before its inception. After informed consent had been obtained, all patients underwent whole-body $^{18}$F-FDG PET/CT, whole-body $^{99m}$Tc-MIBI, and MRI of the spine and pelvis in a random order within a maximum interval of 10 d. None of the patients had undergone chemotherapy or radiotherapy before the study.

$^{18}$F-FDG PET/CT scans were acquired after fasting for 8 h and 60–90 min after intravenous administration of $^{18}$F-FDG (350–370 MBq). The blood glucose level, measured just before tracer administration, was <120 mg/dL in all patients. $^{18}$F-FDG PET/CT images were obtained using a PET/CT Discovery LS8 scanner (GE Healthcare). All scans were performed in 2-dimensional mode. An emission scan was performed in the caudocranial direction, from the upper thigh to the base of the skull (4 min/each bed position) and from the feet to the base of the thigh (2 min/each bed position). Iterative image reconstruction was completed with an ordered-subset expectation maximization (OSEM) algorithm (2 iterations, 28 subsets). CT with a 4-slice multidetector helical scanner was used (detector row configuration, 4 × 5 mm; pitch, 1.5; gantry rotation speed, 0.8 s per revolution; table speed, 30 mm per gantry rotation; 140 kV and 80 mA). Attenuation-corrected emission data were obtained using filtered backprojection CT reconstructed images (gaussian filter with 8-mm full width at half maximum) to match the PET resolution. Transaxial, sagittal, and coronal images and coregistered images were examined using Xeleris software (GE Healthcare). Focal areas visible on at least 2 contiguous PET slices—showing a maximum standardized uptake value (SUVmax) ≥ 2.5 and corresponding to CT abnormalities not attributable to benign bone pathologies—were considered to be sites of active disease. In particular, hypermetabolic sites corresponding to spondylopathy, osteoarthrosis, joint disease, or traumas were carefully excluded from the analysis, whereas those corresponding to CT abnormalities—such as lytic lesions, minor lytic changes, osteopenic areas, morphologic changes not clearly attributable to degenerative disease, and minimal asymmetry of bone marrow attenuation likely due to plasma cell infiltration—were included.

$^{99m}$Tc-MIBI imaging studies were performed by acquiring planar anterior and posterior whole-body scans (lasting about 10 min) 10 min after intravenous injection of 555 MBq of $^{99m}$Tc-MIBI using a dual-head γ-camera (ECAM; Siemens), equipped with a low-energy, high-resolution collimator.

MRI studies were performed at 1.5 T (Achieva; Philips) along sagittal planes covering the whole spine with 3 partially overlapping slabs and along coronal planes for the study of the pelvis. MRI sequences included T1- and T2-weighted turbo-spin-echo images (with and without fat suppression by a preparatory pulse with spectral inversion [SPIR]) and postcontrast T1-weighted fat-suppressed turbo-spin-echo images (5 min after intravenous administration of 0.1 mmol/g gadopentetate dimeglumine [Magnevist; Schering]). The sequence parameters (repetition time/echo time/echo train length) used for the spine were 477/13/4 for T1-weighted images and 3,500/120/43 for T2-weighted images. The sequence parameters used for the pelvis were 550/14/5 for T1-weighted images and 3,500/120/43 for T2-weighted images with SPIR fat suppression. The whole study lasted approximately 35 min, including patient positioning.

$^{18}$F-FDG PET/CT, $^{99m}$Tc-MIBI, and MRI were read and interpreted by 2 independent nuclear medicine physicians and 2 independent radiologists who were unaware of the imaging results. The data obtained were compared by using a χ² test or a Fisher exact test as appropriate. A probability value ≤ 0.05 was considered statistically significant. When a focal pattern was detected, the number and site of focal bone or soft-tissue lesions were reported. The number of focal lesions detected in each patient by each one of the 3 imaging techniques was compared by using the nonparametric paired-data Kendall’s coefficient-of-concordance (W) test. A probability value ≤ 0.01 was considered statistically significant.

RESULTS

The results of whole-body $^{18}$F-FDG PET/CT, whole-body $^{99m}$Tc-MIBI, and MRI of the spine and pelvis performed on the 33 MM patients were compared according to the presence of a normal, diffuse, or focal (combination with or without diffuse) pattern of bone marrow involvement as shown in Table 1. Whole-body $^{18}$F-FDG PET/CT was positive in 32 patients (97%), 3 (9%) of whom had a pure diffuse pattern of

<table>
<thead>
<tr>
<th>Imaging modality</th>
<th>N</th>
<th>D</th>
<th>F-FD</th>
</tr>
</thead>
<tbody>
<tr>
<td>Whole-body $^{18}$F-FDG PET/CT</td>
<td>1</td>
<td>3</td>
<td>29</td>
</tr>
<tr>
<td>Whole-body $^{99m}$Tc-MIBI</td>
<td>3</td>
<td>11</td>
<td>19</td>
</tr>
<tr>
<td>MRI of spine and pelvis</td>
<td>6</td>
<td>13</td>
<td>14</td>
</tr>
</tbody>
</table>

N = normal; D = diffuse; F-FD = focal and focal + diffuse. Values in parentheses are percentages (2-sided Fisher exact test; P < 0.005).
bone marrow uptake, whereas 29 (88%) showed focal lesions in the presence (13 patients, 39%) or absence (16 patients, 48%) of diffuse uptake. Whole-body $^{99m}$Tc-MIBI was positive in 30 patients (91%), of whom 11 (33%) presented a diffuse pattern of uptake and 19 (57%) showed a focal pattern with 13 patients (39%) or without (6 patients, 18%) the association of diffuse uptake. MRI of the spine and pelvis was positive in 27 patients (81%), of whom 13 (39%) had a diffuse pattern and 14 (42%) showed a focal pattern, in combination with a diffuse pattern (8 patients, 24%) or alone (6 patients, 18%).

Comparing the pattern of bone marrow involvement obtained by $^{18}$F-FDG PET/CT, $^{99m}$Tc-MIBI, and MRI, using the Fisher exact test, a significant statistical difference ($P < 0.005$) between the 3 imaging methods was found. In particular, $^{18}$F-FDG PET/CT detected a focal pattern, alone or combined with a diffuse pattern, with a higher frequency than $^{99m}$Tc-MIBI ($P < 0.05$) and MRI ($P < 0.001$). On the other hand, $^{99m}$Tc-MIBI and MRI were comparable and performed better than $^{18}$F-FDG PET/CT in the detection of a pure diffuse pattern. By analyzing the number and sites of focal lesions detected, we found that $^{18}$F-FDG PET/CT showed a total of 196 focal lesions, of which 75 were in the spine and pelvis (35 and 40, respectively) and 121 were in other districts, whereas $^{99m}$Tc-MIBI visualized a total of 63 focal lesions, of which only 1 was in the spine, 9 were in the pelvis, and 53 were in other districts. Eighteen of the total focal lesions visualized by $^{18}$F-FDG PET/CT and only 3 of the lesions detected by $^{99m}$Tc-MIBI were localized in soft tissues. Finally, MRI detected a total of 51 focal lesions—40 in the spine and 11 in the pelvis. Comparing the number of focal lesions per patient detected by each imaging method on the whole dataset, using the nonparametric paired-data Kendall’s $W$ test, we showed that $^{18}$F-FDG PET/CT visualized more focal lesions ($5.94 \pm 9.29$) than $^{99m}$Tc-MIBI and MRI ($1.91 \pm 4.45$ and $1.54 \pm 2.45$, respectively), with a significant statistical difference ($P < 0.001$) as shown in Table 2. We also performed a post hoc analysis using the Kendall’s $W$ test with Bonferroni correction and found a significant statistical difference between the number of focal lesions per patient detected by $^{18}$F-FDG PET/CT and both $^{99m}$Tc-MIBI ($P < 0.001$) and MRI ($P < 0.005$).

To compare homogeneously the 3 imaging methods used, we focused our analysis exclusively on the data obtained in the spinal and pelvic district as shown in Table 3. Comparing these data, using the Fisher exact test, we also found a significant statistical difference ($P < 0.05$) between the 3 imaging techniques. In particular, $^{18}$F-FDG PET/CT and MRI were comparable and performed better than $^{99m}$Tc-MIBI in the detection of a focal pattern, alone or combined with a diffuse pattern. On the other hand, $^{99m}$Tc-MIBI and MRI were comparable and performed better than $^{18}$F-FDG PET/CT in the detection of a diffuse pattern. However, these differences were statistically significant only between $^{18}$F-FDG PET/CT and $^{99m}$Tc-MIBI ($P < 0.01$). Comparing the number of focal lesions per patient visualized by each imaging technique exclusively in the spinal and pelvic district, using the nonparametric paired-data Kendall’s $W$ test, we found that $^{18}$F-FDG PET/CT and MRI showed more focal lesions ($2.27 \pm 4.64$ and $1.54 \pm 2.45$, respectively) compared with $^{99m}$Tc-MIBI ($0.30 \pm 0.68$), with a significant statistical difference ($P < 0.005$) as shown in Table 4. Moreover, the post hoc analysis performed by using the Kendall’s $W$ test with Bonferroni correction showed a significant statistical difference between the number of focal lesions per patient detected by $^{18}$F-FDG PET/CT and MRI ($P < 0.001$ and

### Table 2

**Comparison of Number of Focal Lesions per Patient Detected by Whole-Body $^{18}$F-FDG PET/CT, Whole-Body $^{99m}$Tc-MIBI, and MRI of Spine and Pelvis**

<table>
<thead>
<tr>
<th>Focal lesions per patient (n)</th>
<th>$^{18}$F-FDG PET/CT</th>
<th>$^{99m}$Tc-MIBI</th>
<th>MRI</th>
<th>Kendall’s $W$ test</th>
</tr>
</thead>
<tbody>
<tr>
<td>Whole-body</td>
<td>5.94 ± 9.29</td>
<td>1.91 ± 4.45</td>
<td>1.54 ± 2.45</td>
<td>$P &lt; 0.001$</td>
</tr>
<tr>
<td>$^{99m}$Tc-MIBI</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>spine and pelvis</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

* $P < 0.001$, $^{18}$F-FDG PET/CT vs. $^{99m}$Tc-MIBI.

### Table 3

**Comparison of Number of Focal Lesions per Patient Detected by $^{18}$F-FDG PET/CT, $^{99m}$Tc-MIBI, and MRI of Spinal and Pelvic District**

<table>
<thead>
<tr>
<th>Imaging modality</th>
<th>N</th>
<th>D</th>
<th>F-FD</th>
</tr>
</thead>
<tbody>
<tr>
<td>Whole-body $^{18}$F-FDG PET/CT of spine and pelvis</td>
<td>12 (36)</td>
<td>6 (18)</td>
<td>15 (45)</td>
</tr>
<tr>
<td>Whole-body $^{99m}$Tc-MIBI of spine and pelvis</td>
<td>8 (24)</td>
<td>18 (54)</td>
<td>7 (21)</td>
</tr>
<tr>
<td>MRI of spine and pelvis</td>
<td>6 (18)</td>
<td>13 (39)</td>
<td>14 (42)</td>
</tr>
</tbody>
</table>

$N = \text{normal; } D = \text{diffuse; } F-FD = \text{focal and focal + diffuse.}$ Values in parentheses are percentages (2-sided Fisher exact test; $P < 0.005$).

### Table 4

**Comparison of Number of Focal Lesions per Patient Detected by $^{18}$F-FDG PET/CT, $^{99m}$Tc-MIBI, and MRI of Spinal and Pelvic District**

<table>
<thead>
<tr>
<th>Focal lesions per patient (n)</th>
<th>$^{18}$F-FDG PET/CT</th>
<th>$^{99m}$Tc-MIBI</th>
<th>MRI</th>
<th>Kendall’s $W$ test</th>
</tr>
</thead>
<tbody>
<tr>
<td>spine and pelvis</td>
<td>2.27 ± 4.64</td>
<td>0.30 ± 0.68</td>
<td>1.54 ± 2.45</td>
<td>$P &lt; 0.005$</td>
</tr>
<tr>
<td>$^{99m}$Tc-MIBI</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>spine and pelvis</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

* $P < 0.001$, $^{18}$F-FDG PET/CT vs. $^{99m}$Tc-MIBI.

1 $P < 0.005$, $^{18}$F-FDG PET/CT vs. MRI.

1 $P < 0.01$, MRI vs. $^{99m}$Tc-MIBI.
respectively) may be due to the mechanism of 18F-FDG uptake that reflects the increased glycolysis usually occurring in tumor cells and, thus, the rapid growth and invasive characteristics of focal lesions (4,16,26)—though the inflammation that can be associated with tumor proliferation may also contribute to increased 18F-FDG uptake (20). Moreover, the use of a hybrid system composed by PET and CT images allows the detection of small or slightly active lesions that were barely distinguishable from the surrounding normal tissue on the basis of PET images alone (28). The hybrid system also allows a more precise anatomic localization of hypermetabolic lesions and, therefore, a better discrimination between bone and soft-tissue lesions (8,10). In fact, 18F-FDG PET/CT detected a total of 18 soft-tissue lesions, whereas 99mTc-MIBI visualized only 3 of them. The resolution of 99mTc-MIBI could be improved by performing SPECT. This technique of acquisition, though, would be time-consuming and costly, taking from 99mTc-MIBI imaging some of its positive characteristics—technical ease, rapidity of execution (the study is performed 10 min after injection and lasts only 10 min), and low costs.

On the whole data analysis, 18F-FDG PET/CT detected more focal lesions than MRI (196 and 51 lesions, respectively) because of the presence of a consistent number of lesions outside the spine and pelvis (121 lesions detected by 18F-FDG PET/CT and 53 lesions detected by 99mTc-MIBI). In fact, focusing our analysis exclusively on the spinal and pelvic districts, the number of focal lesions visualized by 18F-FDG PET/CT and MRI became comparable (75 and 51 lesions, respectively). In this district, both 18F-FDG PET/CT and MRI performed better than 99mTc-MIBI, which detected 10 lesions only; this finding could be due to the physiologic uptake of 99mTc-MIBI in the liver and its excretion in the bowel, which may obscure local focal lesions (18).

99mTc-MIBI performed better than 18F-FDG PET/CT in the detection of a diffuse pattern of bone marrow uptake both in the whole data (33% of patients by 99mTc-MIBI and 9% by 18F-FDG PET/CT) and in the pelvic analysis (54% of patients by 99mTc-MIBI and 18% by 18F-FDG PET/CT). The meaning of 18F-FDG diffuse bone marrow uptake in MM patients must be further investigated, as a mild and diffuse 18F-FDG uptake in the spine could be also found in young or mildly anemic patients (28,29). On the other hand, previous studies showed that 99mTc-MIBI concentrates in malignant plasma cells and that diffuse tracer uptake correlates with the percentage of plasma cell infiltration and the amount of a monoclonal component (13,15). Moreover, it has been shown that 99mTc-MIBI bone marrow uptake is able to identify active myeloma and that the extension and intensity of tracer uptake correlates both with the clinical status and the stage of disease (13). In fact, a previous study showed that moderate-to-intense diffuse 99mTc-MIBI uptake or focal uptake with or without diffuse uptake, in the absence of inflammation or other pathologies, excludes the diagnosis of monoclonal gammopathy of unknown significance (MGUS) and correlates with poor prognosis (19). However, it should be noted that faint bone marrow uptake has been reported also in patients affected by pathologies other than MM (20). Nevertheless, when the intensity of diffuse 99mTc-MIBI uptake was analyzed according to the criteria used by Pace et al. (13), specificity improved significantly (20). False-negative cases by 99mTc-MIBI may be due, rather, to the overexpression of P-glycoprotein (Pgp) that can be associated with multidrug-resistant myeloma. 99mTc-MIBI, in fact, is a transport substrate of the energy-dependent efflux pump Pgp, and its washout increases over time from the bone marrow of MM patients overexpressing this protein (17,30). Therefore, to overcome the action of Pgp in our study, imaging was performed no later than 10 min after the injection of 99mTc-MIBI.

Similarly to 99mTc-MIBI, MRI also performed better than 18F-FDG PET/CT in the detection of a diffuse pattern both in the whole data and in the spinal and pelvic analysis (39% of patients by MRI of spine and pelvis, 9% by whole-body 18F-FDG PET/CT, and 18% by 18F-FDG PET/CT in the spinal
and pelvic regions, respectively). Previous studies, in fact, showed that a diffuse pattern of distribution detected by MRI in MM patients correlates with increased bone marrow cellularity, increased plasmacytosis (although <10% may be associated with false-negative cases), anemia, and poorer survival (31). Moreover, recent studies showed that MRI was more sensitive than 18F-FDG PET/CT in the detection of an infiltrative pattern, allowing direct visualization of the bone content with a high spatial resolution (8, 28). These features can be useful, especially in the spinal and pelvic regions that have a complex anatomy and are overlaid by bowel and ribs, respectively (32)—though, the field of view of MRI excludes regions such as skull, sternum, ribs, and long bones containing a high amount of red marrow and frequently infiltrated by malignant plasma cells (23, 24), as shown in Figure 1. In fact, it has been shown that in substituting a whole-body radiographic survey with MRI of spine and pelvis, 10% of MM patients would be understaged (33). In this respect, Zamagni et al. (8) reported that MRI was superior to 18F-FDG PET/CT in the assessment of bone marrow involvement of the spine and pelvis, whereas 18F-FDG PET/CT allowed the detection of myelomatous lesions that were out of the field of view of MRI. In agreement with these findings, our study showed that MRI performed better than 18F-FDG PET/CT in the evaluation of diffuse disease and performed equally well in the detection of focal disease in the spinal and pelvic regions. Also, our study showed a considerable number of focal lesions detected by 18F-FDG PET/CT that were out of the field of view of MRI. This limitation could be overcome by using whole-body MRI. Currently, though, this imaging technique is not widely available yet, and its imaging times are still too long despite the advances in MRI, such as the development of rapid data acquisition and high-performance gradient systems (9). Moreover, the spatial resolution of whole-body MRI is worse than that of focused surface-coil MRI, resulting in poorer imaging quality (34).

CONCLUSION

In whole-body analysis, 18F-FDG PET/CT and 99mTc-MIBI provided complementary information in the diagnostic evaluation of MM patients by detecting focal and diffuse disease, respectively. In the spinal and pelvic regions, MRI was comparable to 18F-FDG PET/CT and 99mTc-MIBI in the detection of focal and diffuse patterns, respectively. Therefore, in the diagnostic work-up of multiple myeloma, MRI—because of its ability in detecting both focal and diffuse disease in the spine and pelvis—should be reserved for the evaluation of bone marrow involvement in these regions. Until whole-body MRI with reasonably short imaging times, good spatial resolution, and standardized sequences for MM will be widely available, the main drawback of MRI of spine and pelvis will be the limited field of view that could underestimate newly diagnosed MM patients, by missing lesions located outside these regions. Therefore, in the whole-body evaluation of MM patients at diagnosis, 18F-FDG PET/CT can contribute to a more accurate assessment of disease—especially in a clinical context highly suggestive of focal involvement of the appendicular skeleton, such as the presence of bone pain or pathologic fractures in long bones or in the case of discrepancies between clinical status and hematologic parameters. On the other hand, despite the limited capacity in detecting focal lesions, 99mTc-MIBI still remains the most rapid and inexpensive technique for whole-body evaluation and may be an alternative option when a PET facility is not available.

ACKNOWLEDGMENTS

This work was partly supported by EU grant EMIL (European Molecular Imaging Laboratories Network) contract 503569, by the Ministry of Health, and by the Ministry of University and Research.
REFERENCES


24. Lucignani G. Bone and marrow imaging: do we know what we see and do we see what we want to know? Eur J Nucl Mol Imaging. 2007;34:1123–1126.


18F-FDG PET/CT, 99mTc-MIBI, and MRI in Evaluation of Patients with Multiple Myeloma

Rosa Fonti, Barbara Salvatore, Mario Quarantelli, Cesare Sirignano, Sabrina Segreto, Fara Petruzzello, Lucio Catalano, Raffaele Liuzzi, Bruno Rotoli, Silvana Del Vecchio, Leonardo Pace and Marco Salvatore

JNM
Published online: January 16, 2008.
Doi: 10.2967/jnumed.107.045641

This article and updated information are available at:
http://jnm.snmjournals.org/content/early/2008/01/16/jnumed.107.045641.citation

Information about reproducing figures, tables, or other portions of this article can be found online at:
http://jnm.snmjournals.org/site/misc/permission.xhtml

Information about subscriptions to can be found at:
http://jnm.snmjournals.org/site/subscriptions/online.xhtml

JNM ahead of print articles have been peer reviewed and accepted for publication in JNM. They have not been copyedited, nor have they appeared in a print or online issue of the journal. Once the accepted manuscripts appear in the JNM ahead of print area, they will be prepared for print and online publication, which includes copyediting, typesetting, proofreading, and author review. This process may lead to differences between the accepted version of the manuscript and the final, published version.