Impaired Lung $^{123}$I-MIBG Uptake on SPECT in Pulmonary Emphysema

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The aim of this study was to evaluate impaired lung uptake of $^{123}$I-metaiodobenzylguanidine ($^{123}$I-MIBG) on SPECT, compared with perfusion SPECT and morphologic CT, in patients with pulmonary emphysema (PE). **Methods:** $^{123}$I-MIBG SPECT was performed at 15 min and 4 h after intravenous injection of $^{123}$I-MIBG in 36 PE patients with a history of smoking and variable-extent low-attenuation areas on CT, indicative of emphysematous changes, and in 16 controls with no history of smoking and no noticeable low-attenuation areas. The distribution of $^{123}$I-MIBG was compared with that of low-attenuation areas on CT and perfusion on SPECT at the base of the 180 lung lobes of the PE patients. Total-lung $^{123}$I-MIBG kinetics were calculated, including early and delayed lung-to-mediasinum uptake ratios and washout rate. **Results:** The controls showed a fairly uniform lung $^{123}$I-MIBG distribution nearly consistent with perfusion. PE patients had heterogeneous $^{123}$I-MIBG defects showing frequent discordance with low-attenuation areas or perfusion distribution; $^{123}$I-MIBG defects were more extensive than low-attenuation areas in 76 lobes (42.2%) of 31 patients (86%) and more extensive than perfusion defects in 44 lobes (24.4%) of 22 patients (61%). $^{123}$I-MIBG defects were seen regardless of the absence of noticeable low-attenuation areas and perfusion defects in 19 lobes (10.5%) of 16 patients (44%). All total-lung $^{123}$I-MIBG kinetic parameters in PE patients were significantly lower than the control values ($P < 0.0001$), with significant correlation with alveolar–arterial oxygen tension gradient but without correlation with the extent of perfusion defects or low-attenuation areas.

**Conclusion:** $^{123}$I-MIBG SPECT allows evaluation of lung pathophysiology in PE independently of perfusion SPECT or morphologic CT, and impairment of lung $^{123}$I-MIBG uptake may be more extensive than perfusion or morphologic abnormalities in PE.

**Key Words:** metaiodobenzylguanidine (MIBG); pulmonary emphysema; single-photon emission computed tomography (SPECT); computed tomography (CT)

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Pulmonary emphysema (PE) is pathologically characterized by progressive disappearance of alveolar structures. Injury of alveolar endothelial cells (AECs) is of great concern and has been considered the primary pathogenesis of PE (1–11). Several histopathologic studies have shown early damage of these cells in smokers and mild-PE patients (2–4,8–10). Recently, evidence that functional impairment of AECs primarily induces alveolar septal cell apoptosis, leading to emphysematous changes, has been accumulating (5,8,10,11).

AECs in the lung microvasculature have the metabolic function of circulating vasoactive norepinephrine (12–15). $^{123}$I-metaiodobenzylguanidine ($^{123}$I-MIBG) shares the same uptake as norepinephrine in AECs (12–15). $^{123}$I-MIBG scintigraphic studies have been used to detect and assess the functional injury or integrity of AECs in various lung diseases, including PE (16–23). SPECT provides better assessment of lung $^{123}$I-MIBG uptake than planar scanning and allows cross-sectional comparisons with lung morphologic CT scans and perfusion SPECT scans.

In the present study, impaired uptake of $^{123}$I-MIBG on cross-sectional SPECT images of the lungs of PE patients was compared with lung morphologic changes on CT and perfusion distribution on SPECT.

**MATERIALS AND METHODS**

**Study Population**

The population included 36 PE patients with variable-extent low-attenuation areas on high-resolution chest CT, indicative of emphysematous lungs, and 16 control subjects with no history of smoking and no noticeable low-attenuation areas on CT, who underwent $^{123}$I-MIBG SPECT during June 2004 to August 2010 (Table 1). All PE patients had a history of smoking, and PE was diagnosed according to the criteria of the American Thoracic Society (24,25). Another 13 PE patients also underwent $^{123}$I-MIBG SPECT during the same period, but these patients were excluded because of the presence of concomitant diseases such as hypertension, diabetes mellitus, congestive heart failure, or thyroid disease and drug therapy (such as sympathomimetics, antihypertensive drugs, or tricyclic antidepressants) that may interfere with $^{123}$I-MIBG uptake (2,16,21). All subjects underwent high-resolution chest CT within 3 wk before or after $^{123}$I-MIBG SPECT, as well as $^{99m}$Tc-macroaggregated albumin perfusion SPECT within 5–10 d before or after $^{123}$I-MIBG SPECT. Alveo-
TABLE 1
Study Population

<table>
<thead>
<tr>
<th>Characteristic</th>
<th>Data</th>
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</thead>
<tbody>
<tr>
<td><strong>PE patients</strong></td>
<td></td>
</tr>
<tr>
<td>Sex</td>
<td>29 men and 7 women</td>
</tr>
<tr>
<td>Age</td>
<td>62.8 ± 8.6 y (range, 49–83 y)</td>
</tr>
<tr>
<td>Smoking history</td>
<td>27 ± 13 pack-years (range, 10–91 pack-years)</td>
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<tr>
<td>%FEV1</td>
<td>75.4% ± 12.4% (range, 42.7%–95.7%)</td>
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<tr>
<td>FEV1</td>
<td>2,328 ± 287 cm³ (range, 1,284–3,685 cm³)</td>
</tr>
<tr>
<td>%VC</td>
<td>87.6% ± 11.7% (range, 81.7%–115.4%)</td>
</tr>
<tr>
<td>A-aDO₂</td>
<td>14.6 ± 9.7 torr (range, 2–36 torr)</td>
</tr>
<tr>
<td>Low-attenuation areas*</td>
<td>15.4% ± 7.9% (range, 4.3%–34%)</td>
</tr>
<tr>
<td>Perfusion defects†</td>
<td>20.8% ± 7.4% (range, 8.9%–37%)</td>
</tr>
</tbody>
</table>

**Controls**

| Sex                       | 9 men and 7 women                        |
| Age                       | 54 ± 31.1 y (range, 51–62 y)             |
| %FEV1                     | 99.4% ± 2.9% (range, 97.4%–111.7%)       |
| FEV1                      | 3,417 ± 208 cm³ (range, 2,951–3,882 cm³) |
| %VC                       | 95.4% ± 5.7% (range, 95.8%–109.5%)       |

*A Percentage of total-lung voxels with attenuation < −960 HU on CT.
†Percentage of total-lung voxels with radioactivity < 10% of maximum on perfusion SPECT.
%FEV1 = predicted forced expiratory volume in 1 s; FEV1 = forced expiratory volume in 1 s; %VC = predicted vital capacity.

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123I-MIBG SPECT

All subjects received 200 mg of potassium perchlorate per day orally, starting the day before SPECT and continuing for 2 d, to block uptake by the thyroid. 123I-MIBG (111 MBq) was injected intravenously with the subject resting supine after overnight fasting. SPECT was performed using a dual-head system (E-cam; Toshiba Medical) with a low-energy, high-resolution collimator at 15 min (early scan) and 4 h (delayed scan) after injection of 123I-MIBG. This timing was applied according to previous investigations of lung 123I-MIBG kinetics using planar images obtained 15–20 min and 3–4 h after injection (23). Each detector was moved at 6° increments and recorded data from 60 angular directions (360° arc) using a step-and-shoot technique, and projection data (128 × 128 pixels, 3.2 mm/pixel) were acquired. Images were acquired for 20 s per projection for a total imaging time of approximately 20 min, with 20% energy windows centered at a photopoint of 159 keV. SPECT data were reconstructed into multislice images in 3 orthogonal planes throughout the entire lung, using a Butterworth prefiltrer (cutoff frequency of 0.11 cycles/cm, order of 8) and a ramp backprojection filter, with a slice thickness of 2 pixels (6.4 mm), gapless. The lung contour on 123I-MIBG SPECT images was drawn at a threshold of 10% of the maximum radioactivity of the lungs in each subject.

Perfusion SPECT

After injection of approximately 185 MBq (5 mCi) of 99mTc-macroaggregated albumin with the subject supine, SPECT was performed using the same system as for the 123I-MIBG scan but with an energy window centered at a photopoint of 140 keV. Three orthogonal-plane images throughout the entire lung were reconstructed using a Butterworth prefilter (cutoff frequency of 0.13 cycles/cm, order of 8) and a ramp backprojection filter, with the same slice thickness of 2 pixels (6.4 mm), gapless. The lung contour on 123I-MIBG SPECT images was drawn at a threshold of 20% of the maximum radioactivity of the lungs in each subject. The extent of perfusion defects in the lung was automatically quantified as the percentage of voxels with radioactivity less than 10% of the maximum radioactivity.

Chest CT

Chest CT was performed using a 16- or 64-detector-row scanner (Somatom Emotion or Sensation; Siemens-Asahi Medical Ltd.). With the subject supine, contiguous 3-mm-interval and 1.5- or 3-mm-thick CT images were obtained in a 512 × 512 matrix during a deep inspiratory breath-hold, with a tube rotation time of 0.8 s, at 120–135 kVp and 200–230 mA. A total of 78–129 transaxial CT images covering the entire lung were reconstructed with the lung algorithm (high-spatial-frequency reconstruction). The lung images were displayed using standard lung window settings (window level, 700 Hounsfield units [HU]; window width, 1,000–1,500 HU). To display the lung distribution of low-attenuation areas indicative of emphysematous lungs, density-mask CT images were created using M900 Quadra imaging software (Zio Soft K.K.). For segmentation of low-attenuation areas on density-mask CT, a threshold of -960 HU was applied, according to previous studies (26,27). The density-mask CT used red to indicate low-attenuation areas in the lung. The extent of the low-attenuation area in the lung was automatically quantified as the percentage of voxels with attenuation less than -960 HU.
Image Interpretation and Data Analysis

Two experienced observers working in consensus compared the distribution of $^{123}$I-MIBG with that of perfusion on SPECT and low-attenuation areas on density-mask CT at the base of the lobe in each subject. On visual inspection, the severity of lung $^{123}$I-MIBG or perfusion defects and low-attenuation areas was classified as limited if the extent was less than 50% of each lobe or as extensive if greater than 50%–60%. In this assessment, the matched transaxial slices of the respective SPECT and CT scans were determined by referring to the scout-view images and the distances from the diaphragm and lung apex. Then, the series of SPECT and CT slices were simultaneously displayed side by side, and adequate correspondence of each lobe was confirmed by comparing the contours of the heart, aorta, and hilar vessels. Any slight mismatching was considered inconsequential because each $^{123}$I-MIBG and perfusion defect and low-attenuation area was relatively extensive in size and spread, appearing similar in at least 2 adjacent planes.

For quantitative analysis of lung $^{123}$I-MIBG uptake, a summed coronal image of every $^{123}$I-MIBG SPECT section in the entire lung was created for each subject. As an index of total-lung $^{123}$I-MIBG uptake, early and delayed ratios of lung uptake relative to mediastinal uptake (L/M ratios) were estimated using averaged counts per pixel obtained from regions of interest covering the entire lung on the early and delayed summed coronal SPECT images (23). In this assessment, the delayed counts were corrected for $^{123}$I decay. In the 11 PE patients with concomitant lesions other than emphysema, the local areas with these lesions were excluded in setting regions of interest. $^{123}$I-MIBG washout rate, defined as (early L/M ratio – delayed L/M ratio)/early L/M ratio, was also calculated according to the previous study (23). These measurements were independently performed by the 2 observers, and the data were averaged. The number of total-lung radioactivity counts for all subjects ranged from 3,872 to 29,387 (average, 2,853 ± 2,971) on early SPECT and from 2,885 to 29,162 (average, 20,863 ± 2,847) on delayed SPECT.

In PE patients, the correlations of total-lung early and delayed L/M ratios and washout rate with the extent of perfusion defects or low-attenuation areas and with A-aDo$_2$ were evaluated.

Statistical Analysis

Results were expressed as the mean ± SD, and a Mann–Whitney U test for nonparametric data was used to analyze differences between controls and PE patients. A probability value of less than 0.05 indicated a significant difference. In PE patients, linear regression analysis was performed to assess the correlations of total-lung early and delayed L/M ratios and washout rate with the extent of perfusion defects or low-attenuation areas and with A-aDo$_2$, using the commercially available Statview Statistical Package (Abacus Concepts). A probability value of less than 0.05 was considered significant for each correlation coefficient.

RESULTS

All 16 controls showed a homogeneous and symmetric distribution of $^{123}$I-MIBG in the lungs on both early and delayed SPECT, but with a gravitational effect showing the most intensive $^{123}$I-MIBG uptake in the lower dorsal part of the lungs (Fig. 1). $^{123}$I-MIBG distribution appeared nearly consistent with perfusion distribution.

By contrast, all 36 PE patients showed partly or diffusely reduced lung $^{123}$I-MIBG uptake, predominantly in the upper lung zones (Figs. 2 and 3). Although variable-extent $^{123}$I-MIBG defects were seen in all the lung lobes with low-attenuation areas or perfusion defects, discordance was frequent (Table 2). Extensive $^{123}$I-MIBG defects were seen in 76 lobes (42.2%) with limited-extent low-attenuation areas in 31 patients (86%) and in 44 lobes (24.4%) with limited-extent perfusion defects in 22 patients (61%). $^{123}$I-MIBG defects were even seen in 19 lobes (10.5%) without noticeable low-attenuation areas or perfusion defects in 16 patients (44%). Although a total of 56 lobes (31.1%) with extensive perfusion defects showed consistently extensive $^{123}$I-MIBG defects, faint $^{123}$I-MIBG radioactivity was seen in 19 lobes (10.5%) with nearly complete perfusion defects in 19 patients (52%).

Quantitatively, the total-lung delayed L/M ratio was lower than the early ratio in all controls but was higher in 14 PE patients (38%) (Fig. 4). All total-lung early and delayed L/M ratios and washout rates were significantly lower in PE patients than in controls ($P < 0.0001$) (Table 3; Supplemental Fig. 1; supplemental materials are available online only at http://jnm.snmjournals.org). All these $^{123}$I-MIBG parameters in these patients had no correlation with the extent of total-lung perfusion defects or low-attenuation areas (not statistically significant). All these $^{123}$I-MIBG parameters and the extent of perfusion defects in PE patients were significantly correlated with A-aDo$_2$ (Table 4; Supplemental Fig. 2; Fig. 5), whereas the extent of low-attenuation areas had no correlation.

![Image](https://example.com/image.png)
The present study showed a significant reduction of lung 123I-MIBG uptake and washout rate in PE patients, compared with controls. Lung 123I-MIBG defects in these patients were frequently more extensive than perfusion defects or low-attenuation areas at the base of the lobe and were occasionally seen in lobes without noticeable perfusion defects or low-attenuation areas. The estimated 123I-MIBG kinetic parameters correlated with A-aD O2 but not with the extent of total-lung perfusion defects or low-attenuation areas. These results indicate that 123I-MIBG SPECT can be an investigative tool to evaluate lung pathophysiology in PE, independently of perfusion SPECT and morphologic CT.

The AECs of the lung extract and metabolize approximately 25%–50% of norepinephrine, that is, 123I-MIBG, during a single pass through pulmonary circulation (13–15). The fact that the homogeneous lung 123I-MIBG distribution was nearly consistent with perfusion in our controls appears to be attributable to this high extraction of 123I-MIBG in AECs. The slight variability in estimated lung 123I-MIBG kinetic parameters in our controls is consistent with previous observations on planar 123I-MIBG scintigraphic studies of healthy subjects (21–23).

The significant reduction of lung 123I-MIBG uptake in our PE patients can be explained by lack of function and integ-

### TABLE 2

<table>
<thead>
<tr>
<th>Findings</th>
<th>No. of lobes</th>
<th>No. of patients</th>
</tr>
</thead>
<tbody>
<tr>
<td>Preserved 123I-MIBG uptake in lobe, without noticeable perfusion defect and low-attenuation areas</td>
<td>20 (11.1%)</td>
<td>18 (50%)</td>
</tr>
<tr>
<td>Limited 123I-MIBG defect in lobe, without noticeable perfusion defect and low-attenuation areas</td>
<td>19 (10.5%)</td>
<td>16 (44%)</td>
</tr>
<tr>
<td>Limited 123I-MIBG defect in lobe, with limited perfusion defect and low-attenuation areas</td>
<td>41 (22.7%)</td>
<td>36 (100%)</td>
</tr>
<tr>
<td>Extensive 123I-MIBG defects in lobe, with limited perfusion defect and low-attenuation areas</td>
<td>44 (24.4%)</td>
<td>22 (61%)</td>
</tr>
<tr>
<td>Extensive 123I-MIBG defects in lobe, with extensive perfusion defect but limited low-attenuation areas</td>
<td>32 (17.7%)*</td>
<td>28 (77%)</td>
</tr>
<tr>
<td>Extensive 123I-MIBG defects in lobe, with extensive perfusion defect and low-attenuation areas</td>
<td>24 (13.3%)*</td>
<td>17 (47%)</td>
</tr>
</tbody>
</table>

*All 56 lobes with extensive perfusion defects had extensive 123I-MIBG defects, but in 19 patients (52%) with nearly complete perfusion defects, some faint 123I-MIBG radioactivity was seen in 19 lobes (10.5%).
rity of the AECs and loss of the pulmonary vascular bed. Pulmonary arterial vasoconstriction due to oxidant or inflammation-induced mediators and regional hypoxia associated with smoking, and vascular compression in emphysematous lungs, induces ischemia and damage to AECs (12,15,16,23,28). Previous histologic studies showed frequent thinning or disappearance of AECs in PE patients (2–4,8–10,23,29–33). Damaged AECs cannot efficiently extract circulating 123I-MIBG (9,12,13,28). The previous animal model studies of pulmonary vascular damage showed a linear relationship between the degree of reduced 123I-MIBG uptake and loss of the pulmonary vascular bed (17,23). Poor delivery of 123I-MIBG due to decreased perfusion also may reduce 123I-MIBG uptake, as 123I-MIBG defects were persistently seen at the lung lobes with perfusion defects in our patients. The occasional 123I-MIBG defects seen in lobes without perfusion defects in our patients indicate that lung 123I-MIBG uptake may be more sensitively impaired than perfusion. Damaged sympathetic neurons widely distributed in pulmonary airways and vessels due to regional hypoxia associated with smoking (3,8,10,15,16,23) also may reduce 123I-MIBG uptake in PE, since part of the circulating 123I-MIBG is trapped in the presynapses of these neurons (12–14,16). The observed occasional faint 123I-MIBG radioactivity in lung lobes with nearly complete perfusion defects can be explained by the difference between nonparticulate 123I-MIBG and particulate 99mTc-macroaggregated albumin.

The decreased lung 123I-MIBG washout rate in our patients may be partly caused by reduced perfusion associated with vascular damage. Although extracellular 123I-MIBG increases because of decreased extraction of circulating 123I-MIBG to damaged AECs and sympathetic neurons, decreased perfusion disrupts back-diffusion of this component to systemic circulation (15,17,21). Lack of integrity or dysfunction of AECs in PE patients also decreases the 123I-MIBG washout rate, as various other lung disorders with injury of AECs persistently show a decreased 123I-MIBG washout rate (16,18,20–23,34).

The observed correlations of total-lung 123I-MIBG uptake and washout rate with A-aDO2 in our patients strengthen the value of 123I-MIBG SPECT in assessing lung pathophysiology in PE. A-aDO2 should be increased proportionally by the reduced surface and integrity of AECs. Recently, injury of AECs has been of great concern as the primary pathogenesis of smoking-induced PE (1–11,31,35,36). A recent ultrastructural study showed early disruption of AECs to be associated with smoking-induced chronic inflammatory processes and regional hypoxia (1,3,31). Decreased expression of vascular endothelial growth factor and its receptor is reported to enhance apoptosis of AECs, causing progressive disappearance of lung tissue in smoking-induced PE (5,8,10,11,29,30,35,36).

**TABLE 3**
Comparison of Lung 123I-MIBG Kinetic Parameters Between Controls and PE Patients

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Controls</th>
<th>PE patients</th>
<th>P</th>
</tr>
</thead>
<tbody>
<tr>
<td>Early L/M ratio</td>
<td>4.10 ± 1.00</td>
<td>1.55 ± 0.58</td>
<td>&lt;0.0001</td>
</tr>
<tr>
<td>Delayed L/M ratio</td>
<td>2.82 ± 0.90</td>
<td>1.51 ± 0.49</td>
<td>&lt;0.0001</td>
</tr>
<tr>
<td>Washout rate</td>
<td>30.7% ± 14.0%</td>
<td>1.0% ± 7.2%</td>
<td>&lt;0.0001</td>
</tr>
</tbody>
</table>

**TABLE 4**
Linear Dependency of Total-Lung Early and Delayed L/M Ratios, Washout Rate, and Extent of Perfusion Defects and Low-Attenuation Areas on A-aDo2 in PE Patients

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Formula</th>
<th>R</th>
<th>P</th>
</tr>
</thead>
<tbody>
<tr>
<td>Early L/M ratio</td>
<td>$y = 34.147 - 8.569x$</td>
<td>0.406</td>
<td>0.0027</td>
</tr>
<tr>
<td>Delayed L/M ratio</td>
<td>$y = 32.204 - 7.51x$</td>
<td>0.363</td>
<td>0.029</td>
</tr>
<tr>
<td>Washout rate</td>
<td>$y = 22.042 - 1.18x$</td>
<td>0.833</td>
<td>&lt;0.0001</td>
</tr>
<tr>
<td>Perfusion defects</td>
<td>$y = 11.265 + 459x$</td>
<td>0.333</td>
<td>0.0471</td>
</tr>
<tr>
<td>Low-attenuation areas†</td>
<td>$y = 20.345 + 031x$</td>
<td>0.024</td>
<td>NS</td>
</tr>
</tbody>
</table>

*Percentage of total-lung voxels with radioactivity < 10% of maximum on perfusion SPECT.
†Percentage of total-lung voxels with attenuation < −960 HU on CT.
NS = not statistically significant.
The present finding of decreased lung $^{123}$I-MIBG uptake and washout rate in PE patients is consistent with the recent pilot study of planar $^{123}$I-MIBG scintigraphy, but the study evaluated only the upper lung zones, without comparison with lung perfusion, and showed correlations of lung $^{123}$I-MIBG washout rate with the severity of emphysema on CT (25). Because $^{123}$I-MIBG defects were occasionally seen without noticeable low-attenuation areas in our patients, CT may not be sufficiently sensitive to identify mild alveolar pathophysiology in PE (27,37).

The altered lung $^{123}$I-MIBG uptake in our PE patients seems to be associated with smoking-induced pathologic changes in AECs, since smoking is a strong factor for injuring AECs (2–4). However, polluted air and some foods and drugs may also cause pathologic changes in AECs and altered $^{123}$I-MIBG uptake. Further evaluation is required.

CONCLUSION

Impaired $^{123}$I-MIBG uptake in the lungs of PE patients was evaluated in cross-sectional comparisons of $^{123}$I-MIBG SPECT scans with perfusion SPECT scans and CT scans. Lung $^{123}$I-MIBG uptake and washout rate were significantly lower in patients than in controls. Lung $^{123}$I-MIBG uptake in these patients was frequently discordant with perfusion or morphologic abnormalities, as $^{123}$I-MIBG defects were often more extensive than perfusion defects or low-attenuation areas and occasionally were seen even without noticeable perfusion defects or low-attenuation areas. The estimated total-lung $^{123}$I-MIBG kinetic parameters were correlated with A-aDO$_2$ but not with the extent of perfusion defects or low-attenuation areas. $^{123}$I-MIBG SPECT allows evaluation of lung pathophysiology in PE independently of perfusion SPECT or morphologic CT, and impairment of lung $^{123}$I-MIBG uptake may be more extensive than perfusion or morphologic abnormalities in PE.

DISCLOSURE STATEMENT

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No potential conflict of interest relevant to this article was reported.

REFERENCES


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